



Master 2 Pharmacotechnie et Biopharmacie

Nanoscale drug delivery systems (UE 3)

The magic bullet

Paul Ehrlich (1854-1915)

Magic bullet

- 1906 : “Magic bullet” (magische Kugel)
- An ideal therapeutic agent, capable of targeting the causative element of the disease

(Nano)carrier

Targeting

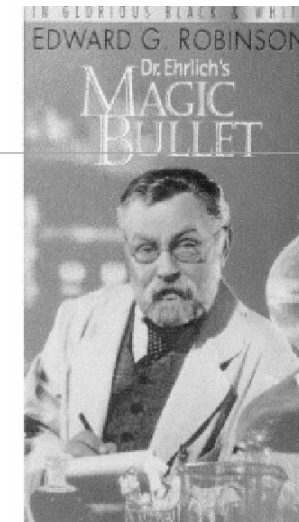


Dr. Ehrlich's Magic Bullet

Thursday ■ July 31 ■ 7:00 p.m.

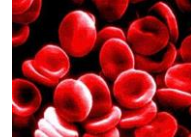
Starring

EDWARD G. ROBINSON (Dr. Paul Ehrlich)
RUTH GORDON (Mrs. Ehrlich)
OTTO KRUGER (Dr. Emil Von Behring)
DONALD CRISP (Minister Althoff)
MARIA OUSPENSKAYA (Franziska Speyer)
MONTAGU LOVE (Prof. Hartmann)
Directed by WILLIAM DIETERLE
Written by JOHN HUSTON, HEINZ
HERALD, and NORMAN BURNSIDE

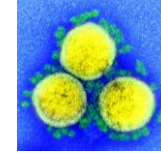


The scale of objects

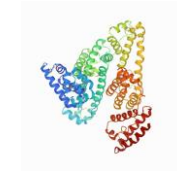
Red blood cells



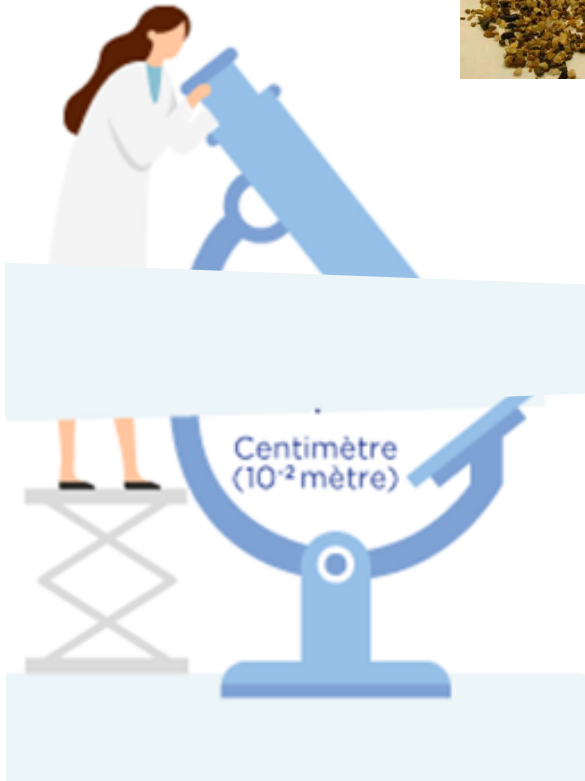
Virus
20 -400 nm



Protein 10 -20 nm



Molecule
< 10 nm



1000 nm

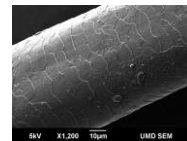
100 nm

1 nm

Millimeter
(10^{-3} meter)

Micrometer
(10^{-6} meter)

Nanometer
(10^{-9} meter)



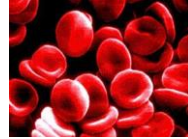
Hair
10 μ m



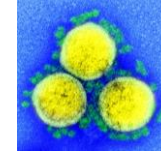
Bacteria
500 nm –10 μ m

The scale of objects

Red blood cells



Virus
20 -400 nm



Protein 10 -20 nm



Molecule
< 10 nm



1000 nm

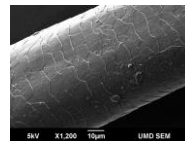
100 nm

1 nm

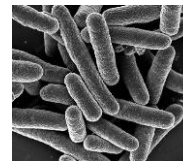
Millimeter
(10^{-3} meter)

Micrometer
(10^{-6} meter)

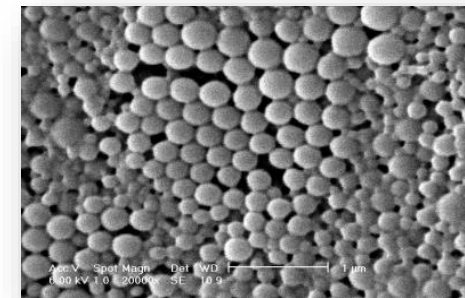
Nanometer
(10^{-9} meter)



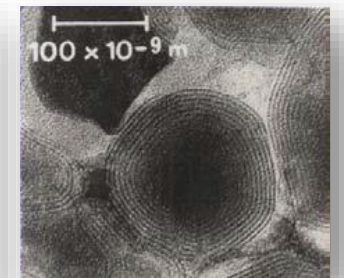
Hair
10 μ m



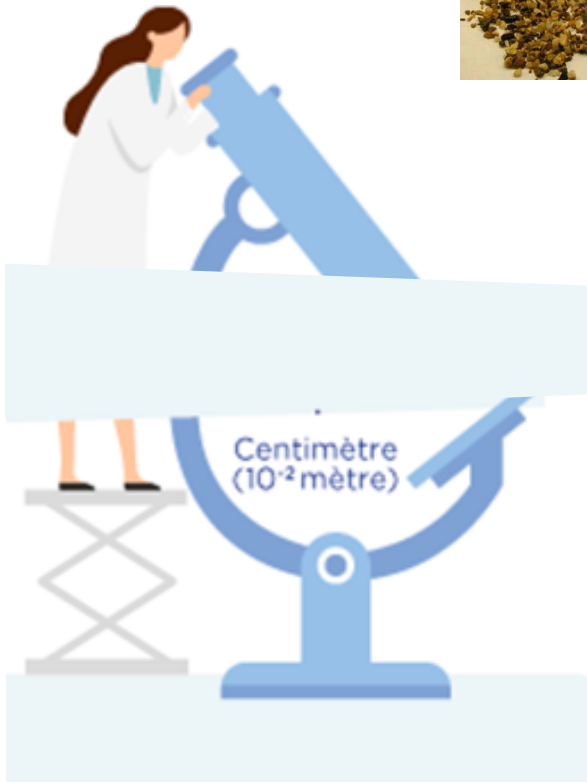
Bacteria
500 nm –10 μ m



Polymer nanoparticle



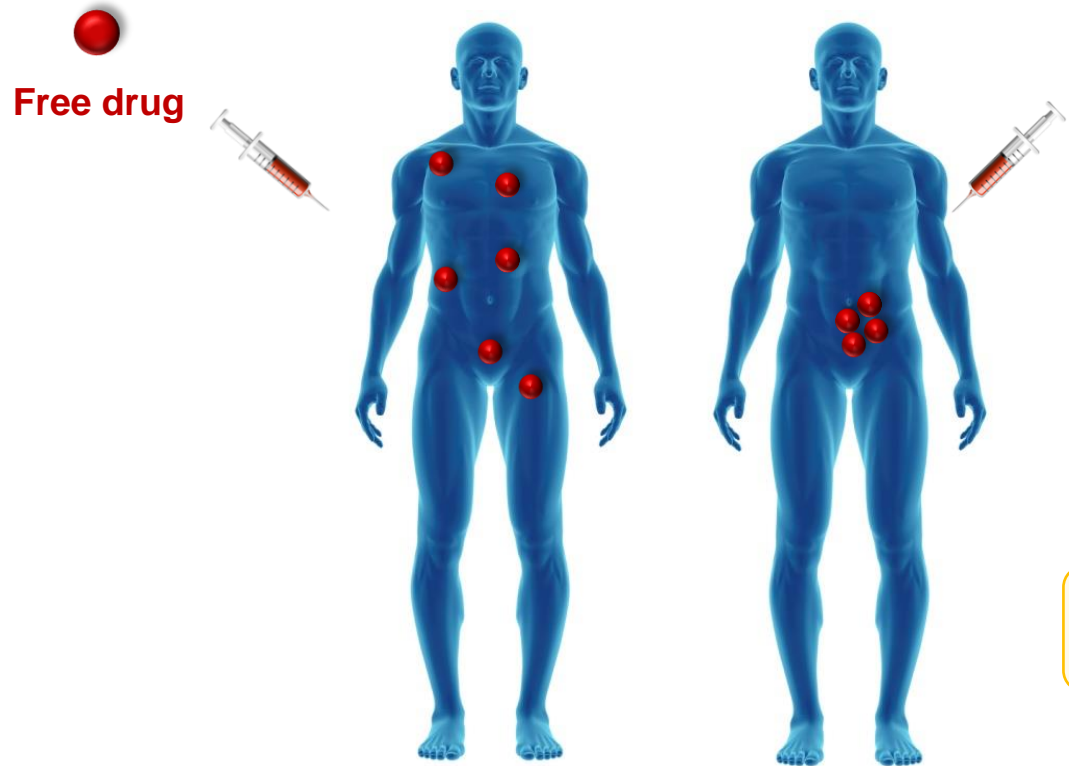
Liposome
s



The magic bullet

Make the fate of a drug dependent from a carrier

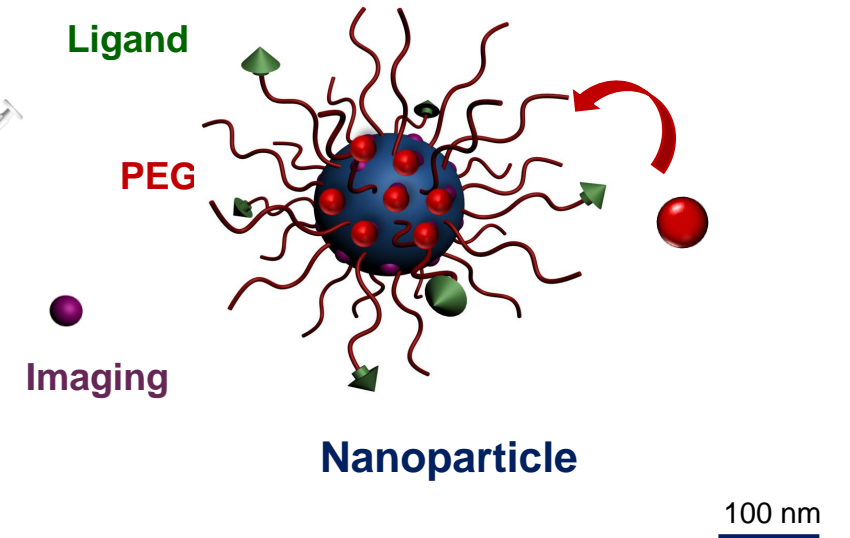
- Traditional chemotherapy



Distribution

- Size
- Pka
- Lipophilicity
- Binding to plasma proteins
- Biotransformations

- Nanomedicines

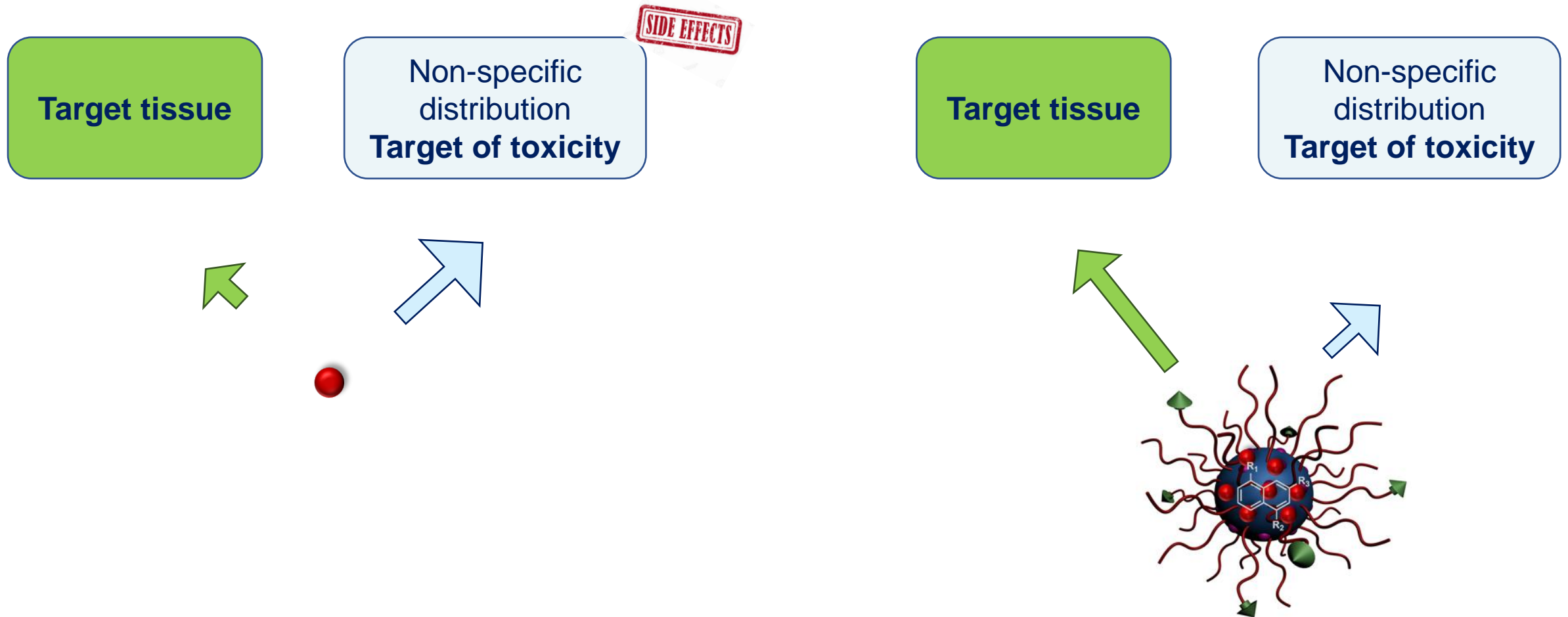


Alternative Distribution

- Vector size
- Lipophilicity
- Stability
- Cytotropism

Controlled delivery

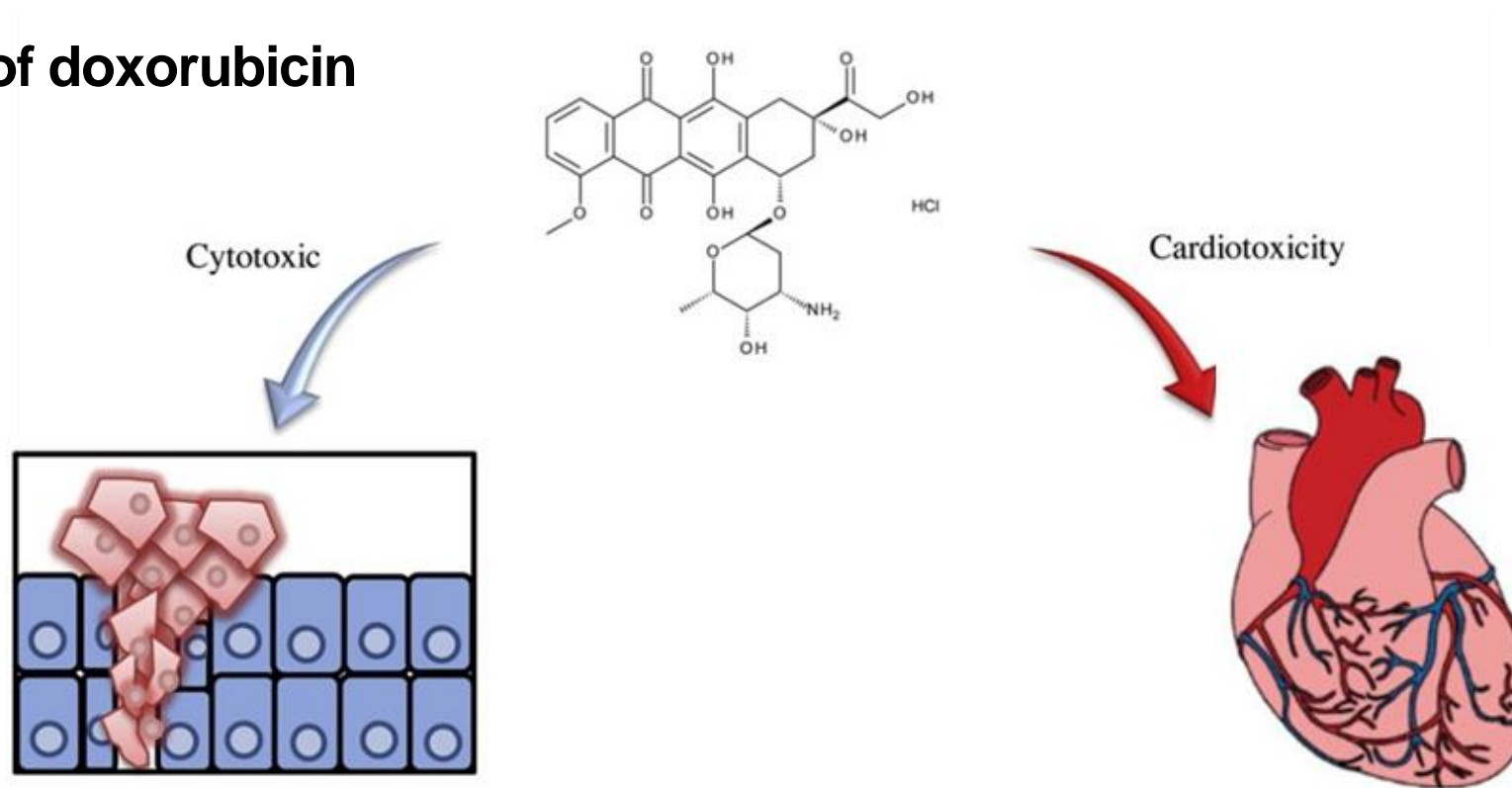
Targeting and reducing side effects



Controlled delivery

Targeting and reducing side effects

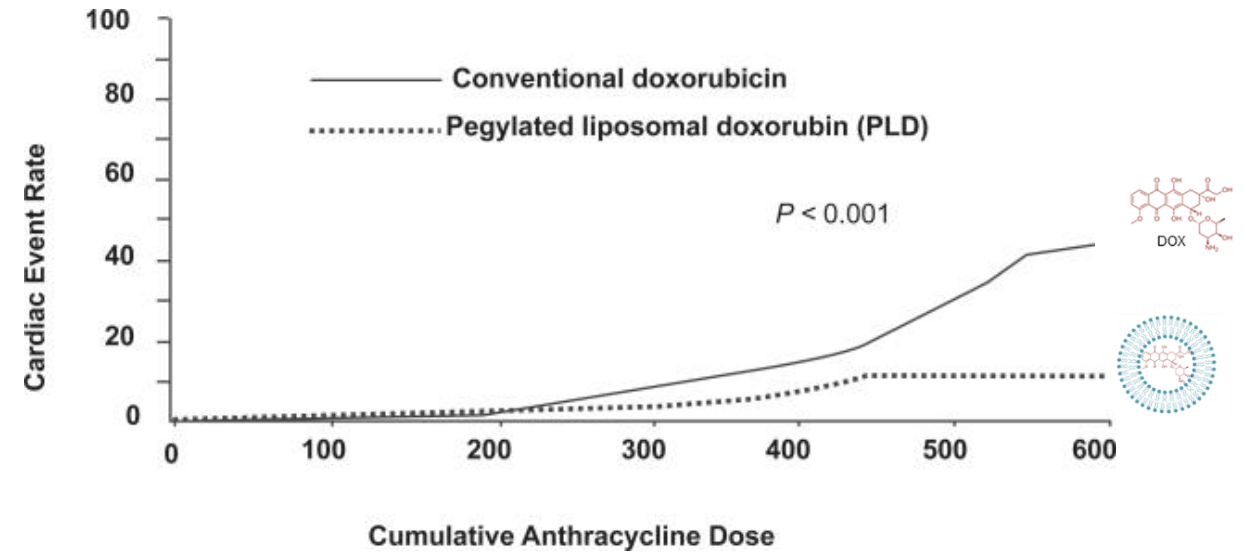
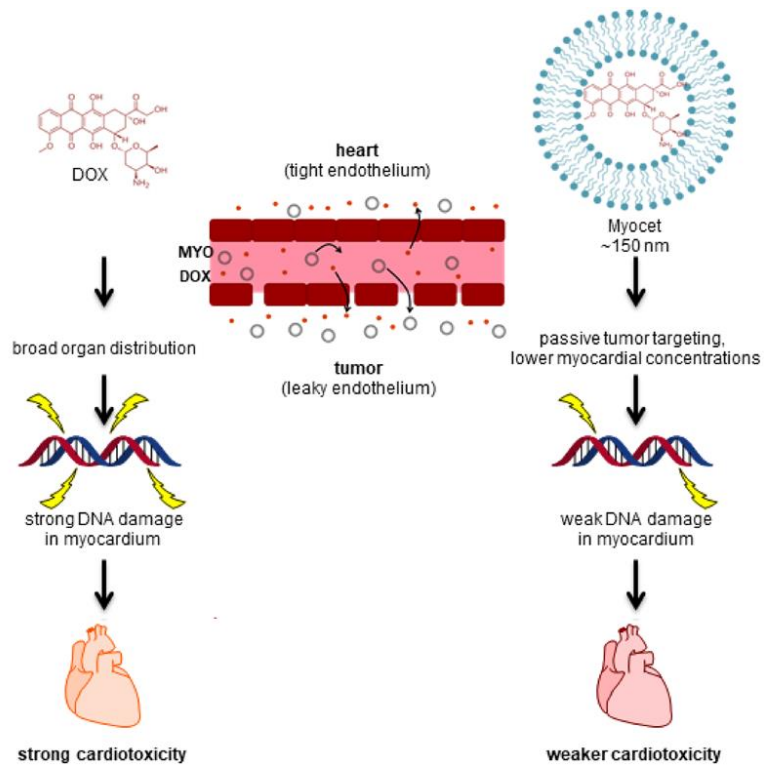
Cardiotoxicity of doxorubicin



Controlled delivery

Targeting and reducing side effects

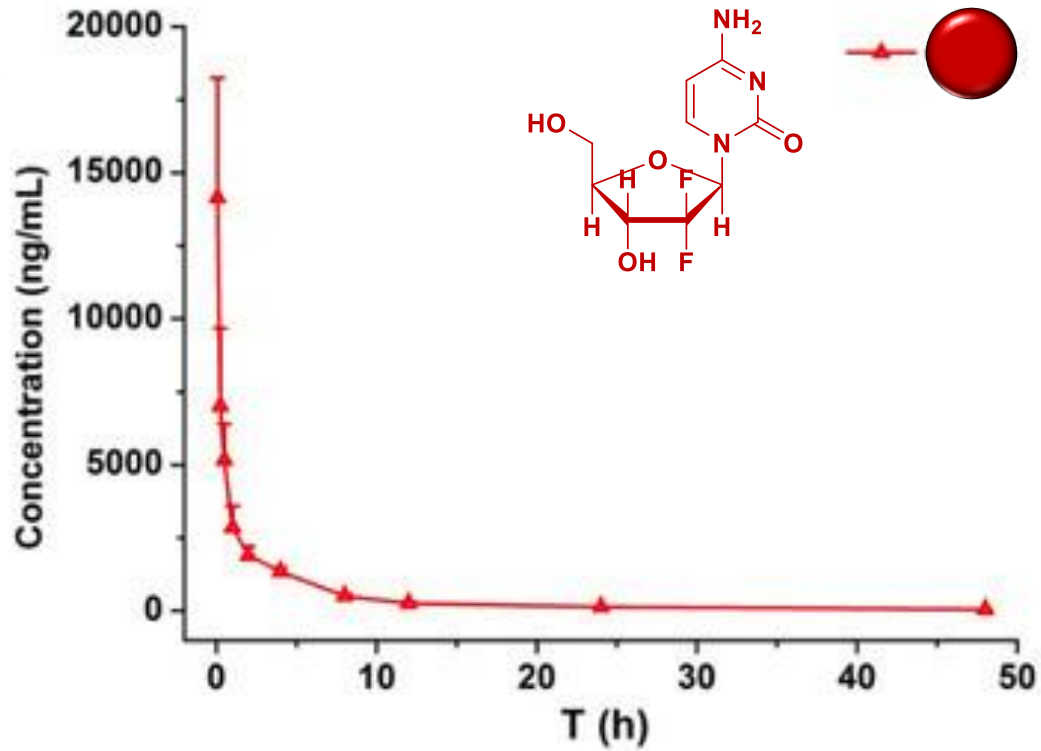
Cardiotoxicity of doxorubicin



- Efficacy of CAELYX not inferior to doxorubicin
- Significantly less cardiotoxicity in first-line treatment of women with metastatic breast cancer

Controlled delivery

Protection against degradation_prodrug strategy



Drug (inactive) Polymer/lipid



Metabolization

Drug (active)

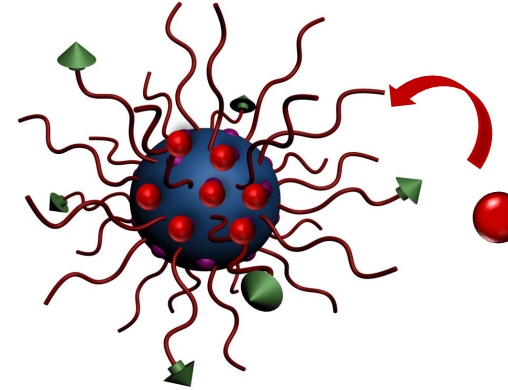


Advantages

- Sustained drug release
- Increase of the drug chemical stability
- Reduced toxicity before metabolization occurs

The magic bullet

Make the fate of a drug dependent from a carrier



Nanoparticle

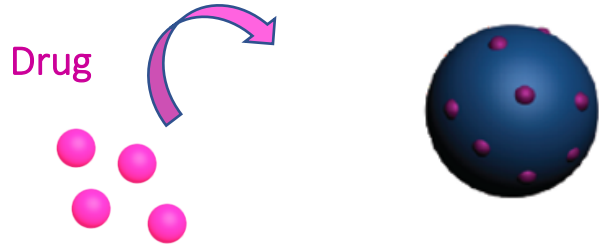
Traditional chemotherapy

- Instability/metabolization
- Limited intracellular accumulation
- Lack of cell/tissue specificity
- Induction of resistance phenomena

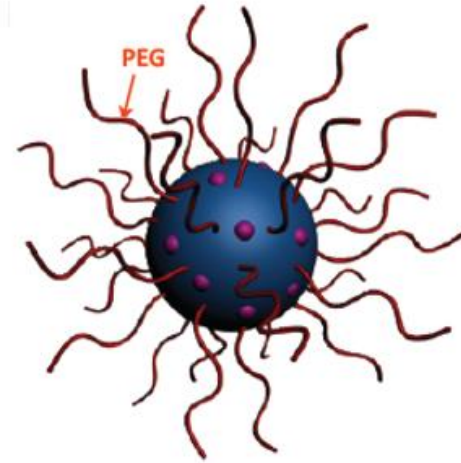
Nanomedicines

- Protection from degradation
- Increase intracellular penetration
- Cell/tissue targeting
- Overcome resistance

Nanomedicine generations

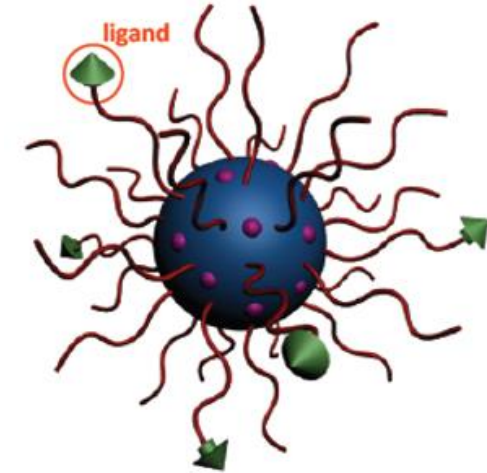


1st generation



2nd generation

Stealth/Long circulating

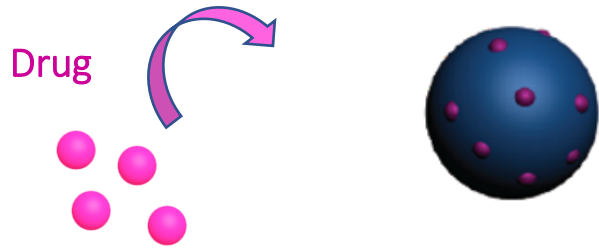


3rd generation

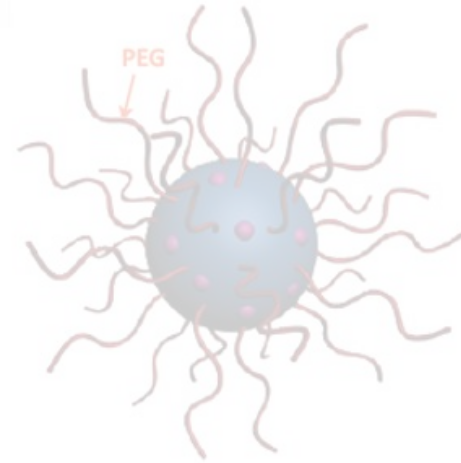
Stealth/Long circulating
Surface functionalized



Nanomedicine generations

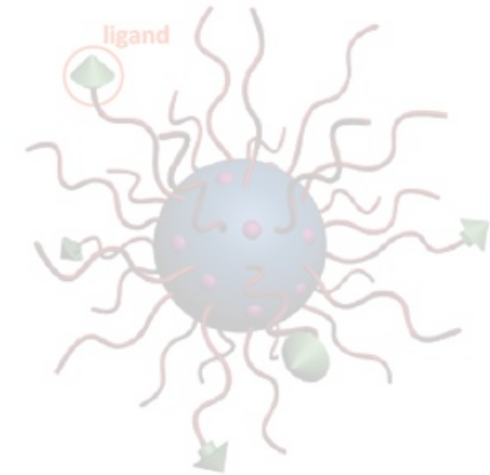
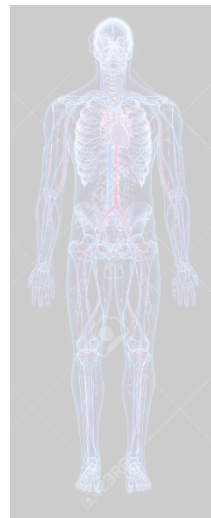


1st generation



2nd generation

Stealth/Long circulating



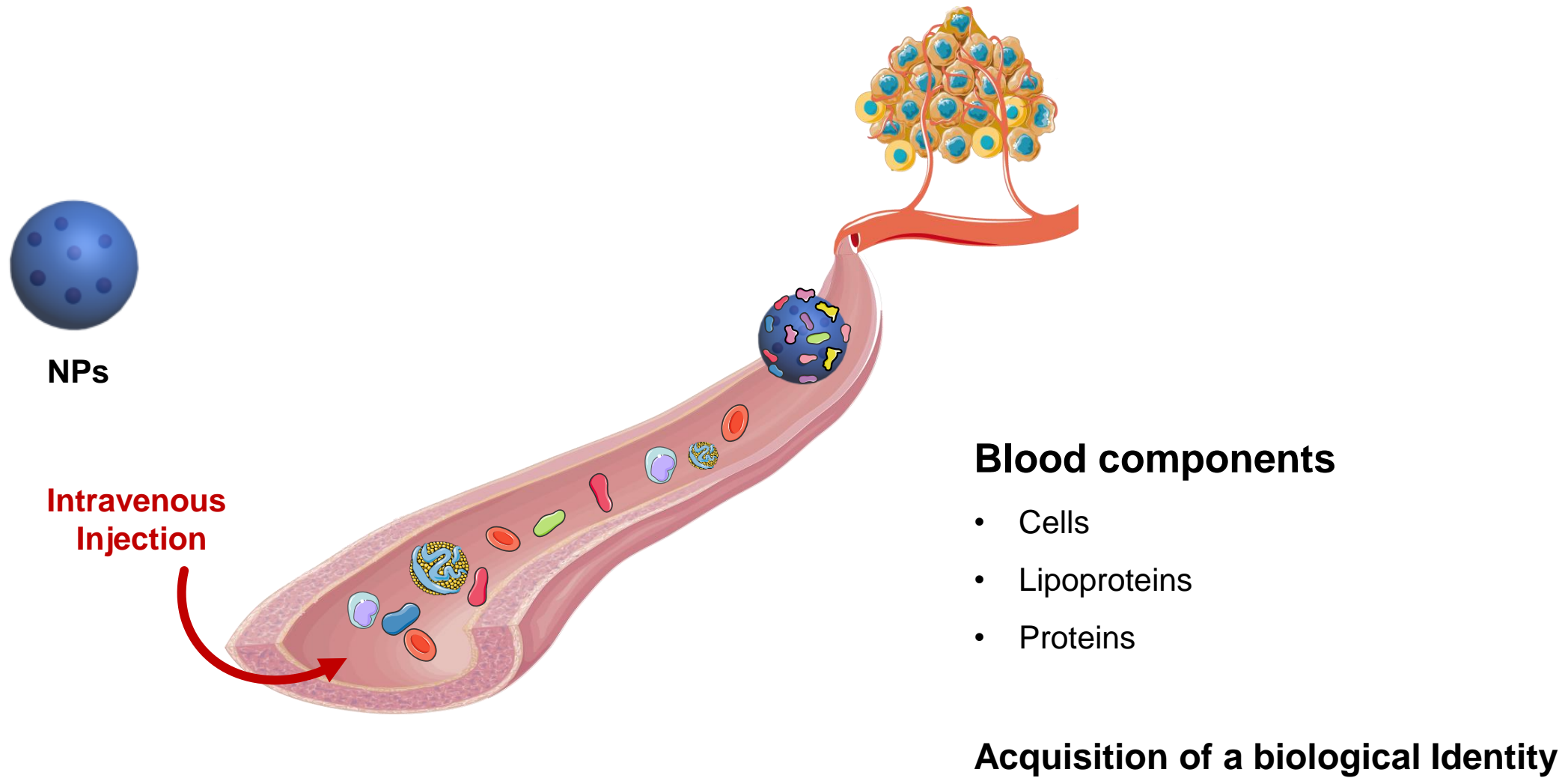
3rd generation

Stealth/Long circulating
Surface functionalized



In vivo fate

Interactions in the biological medium



In vivo fate

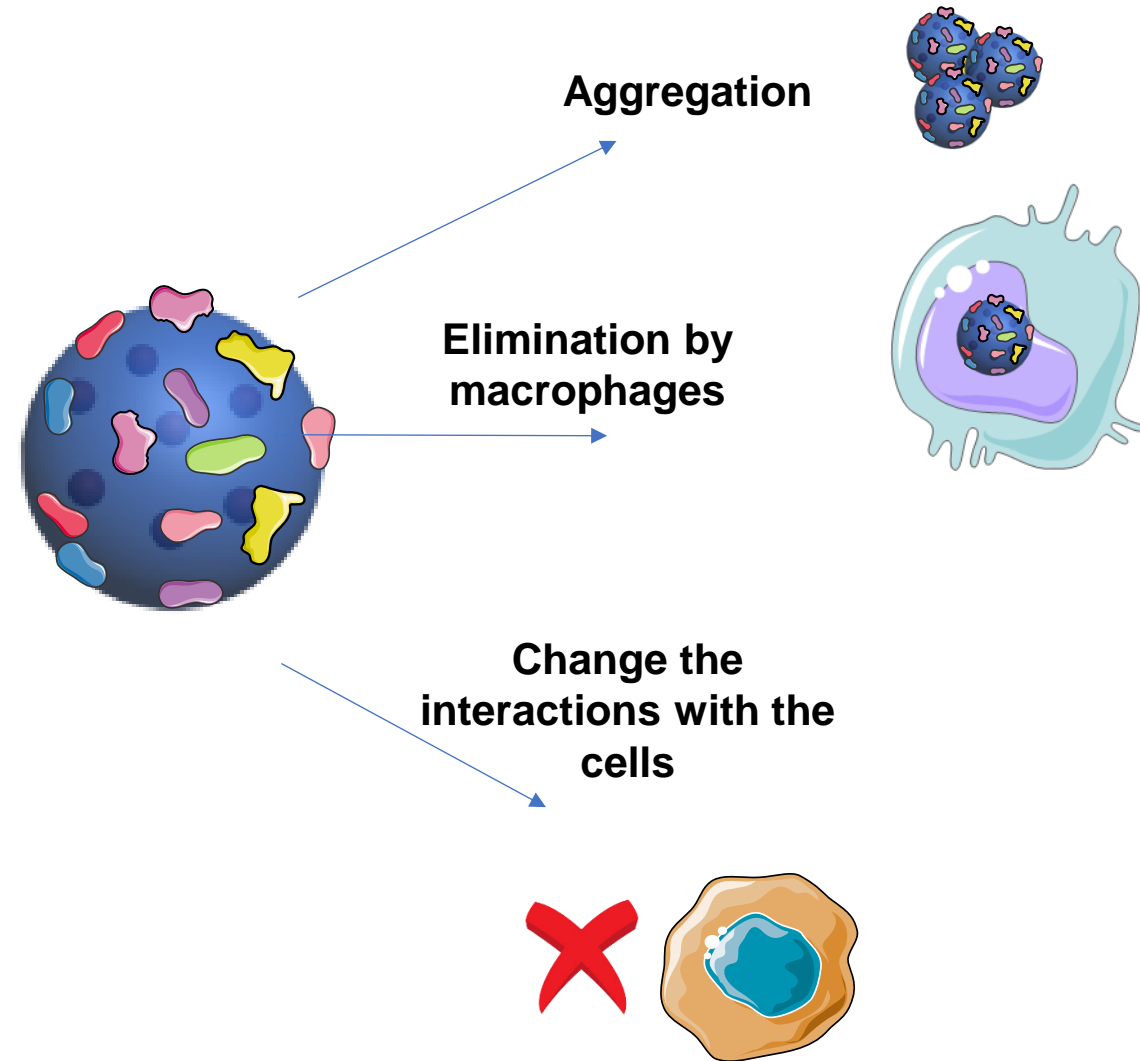
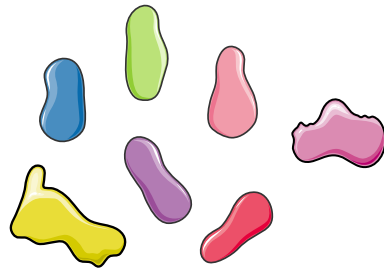
Interactions in the biological medium_the protein corona

Opsonins

- Coagulation proteins : fibrinogen/kininogen-1
- Acute phase proteins
- Tissue leakage proteins
- Components of the complement system
- Immunoglobulins

NON Opsonins

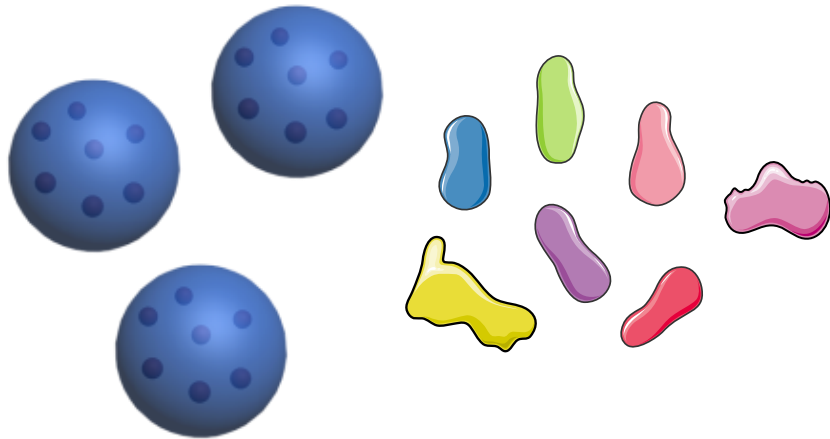
- Albumin
- Apoproteins



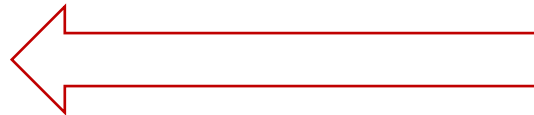
Acquisition of a specific molecular signature

In vivo fate

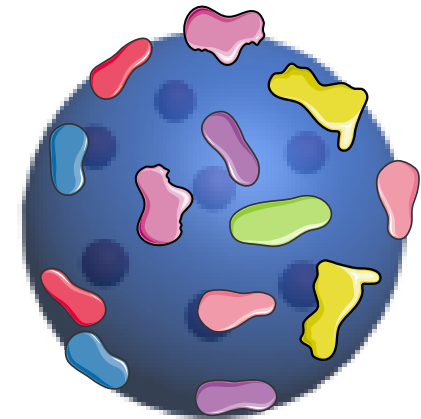
Interactions in the biological medium_the protein corona



- Hydrogen bonds
- Electrostatic interactions
- Hydrophobic interactions
- Acid-base interactions

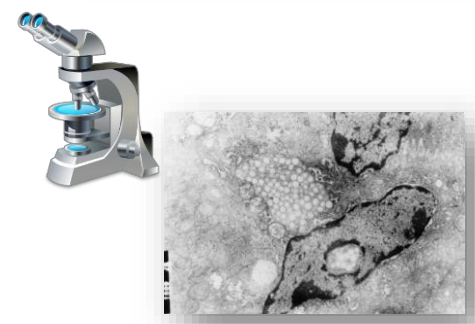
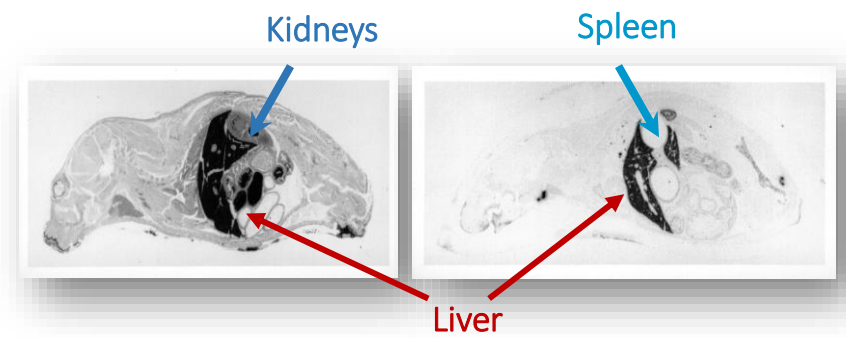
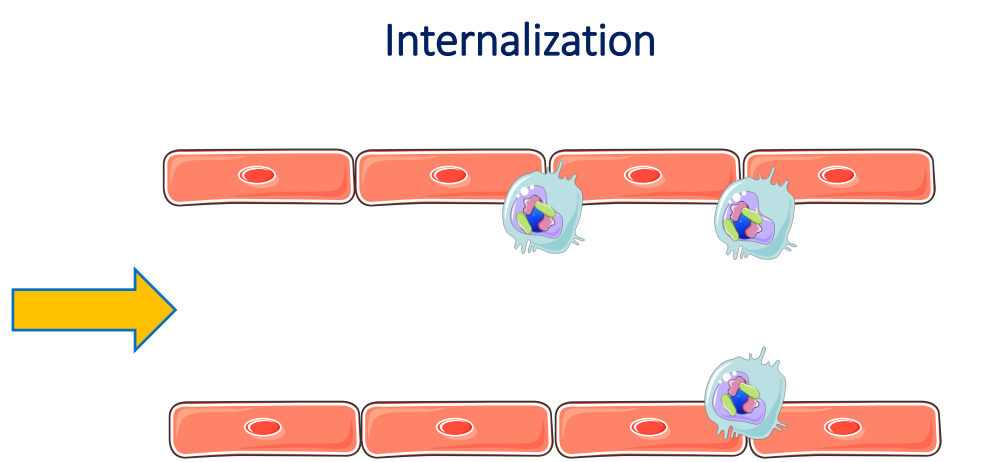
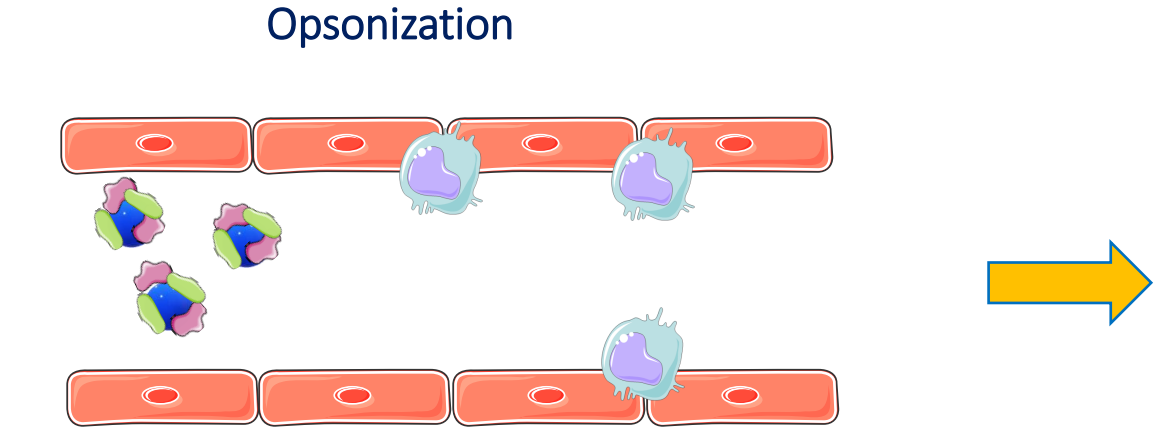
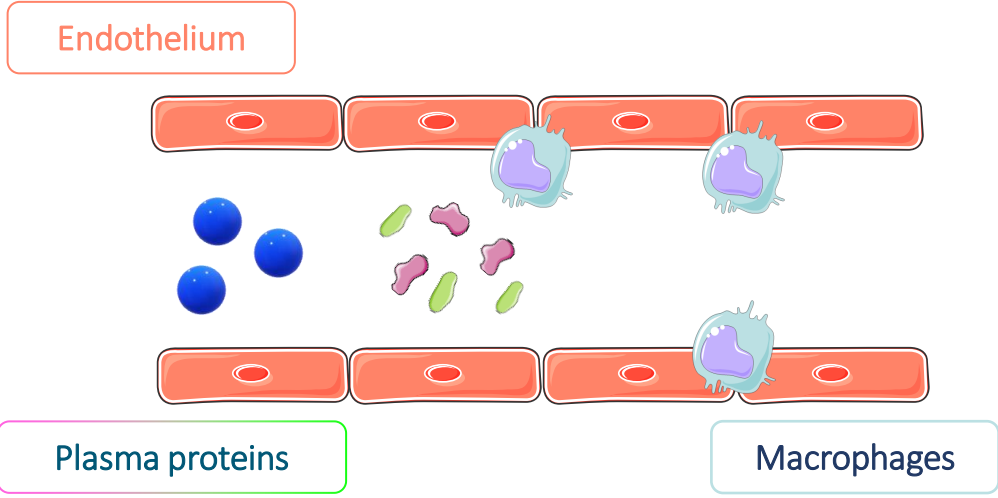


- Hydration/solvation forces
- Steric hindrance
- Electrostatic repulsion



First generation : Fate of nanoparticles after IV administration

- Macrophage uptake and liver accumulation



Nanoparticle uptake by Kupffer cells → Rapid removal from the circulation

In vivo fate

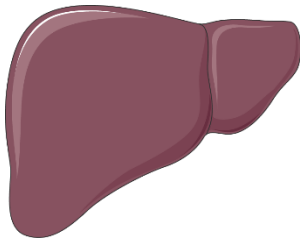
Interactions in the biological medium_the protein corona

Endocytosis/Phagocytosis

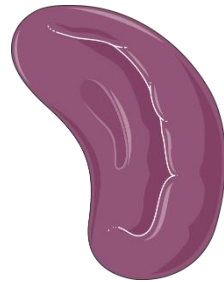


- Monocytes
- Tissue macrophages

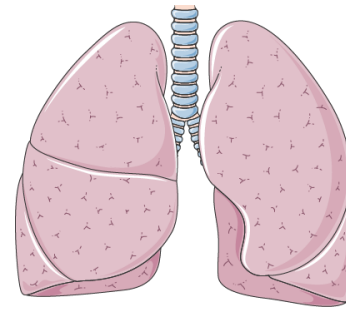
Mononuclear phagocyte system



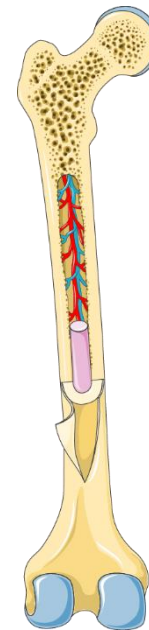
Liver



Spleen



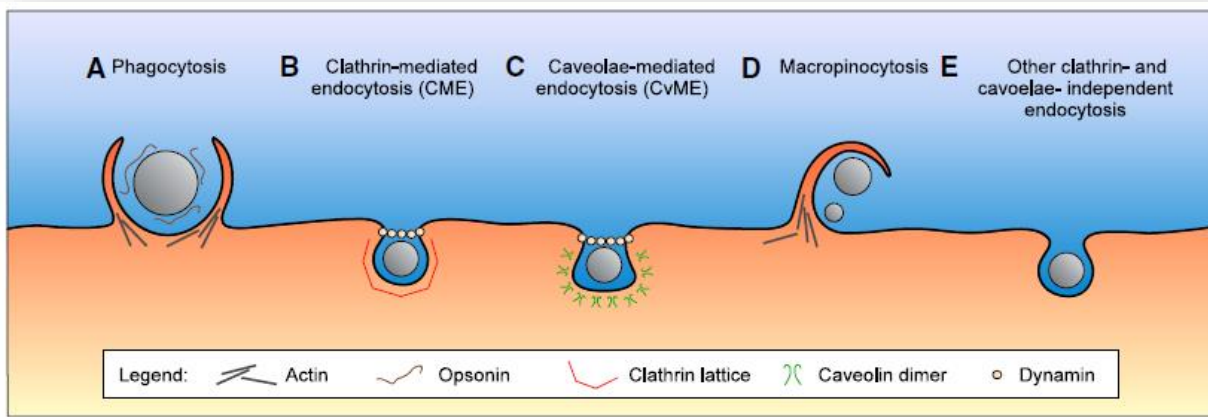
Lungs



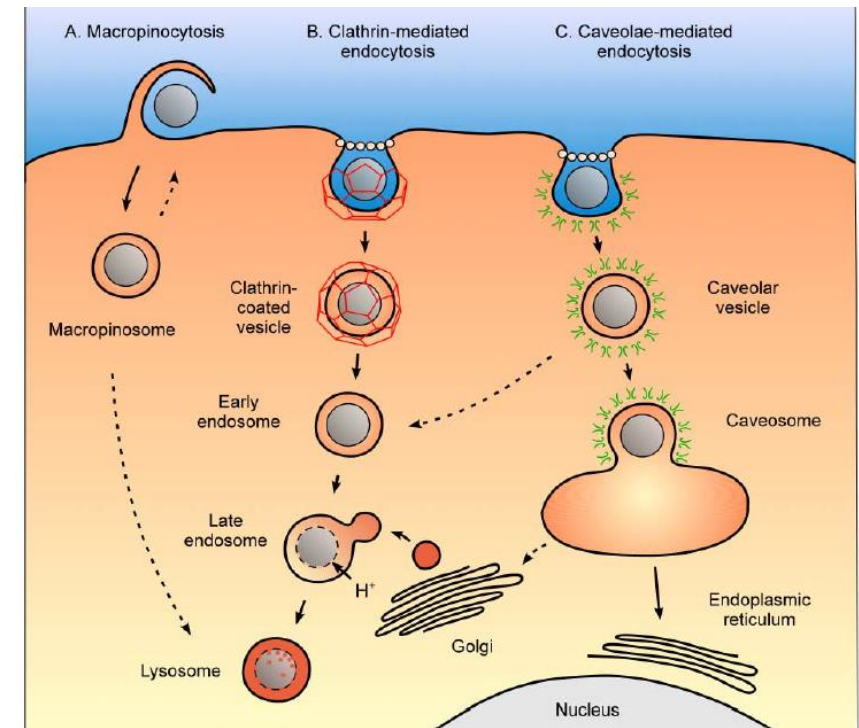
Bone marrow

In vivo fate

Internalization pathways

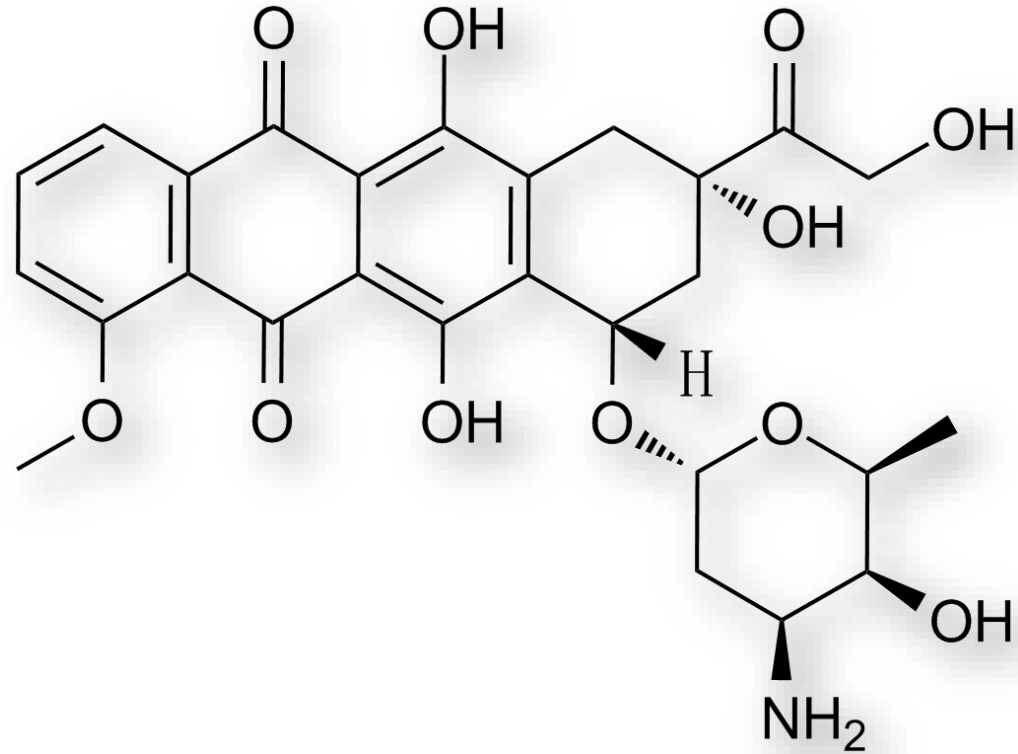


Endocytosis



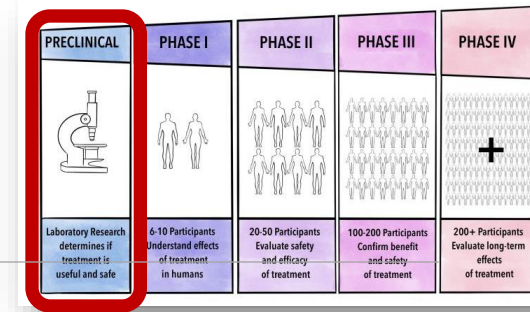
Antitumor chemotherapy

Doxorubicin

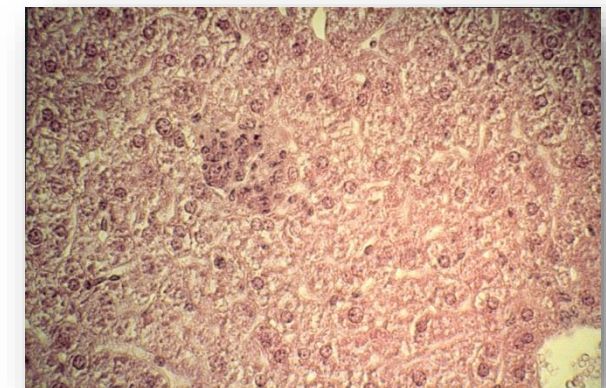
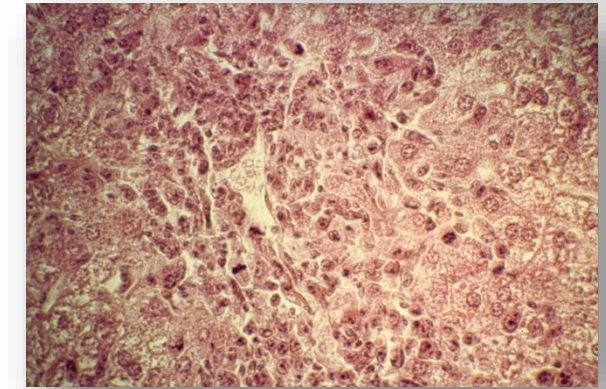
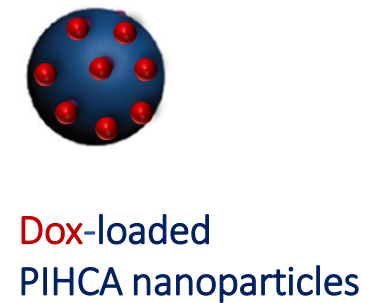
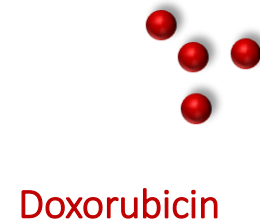
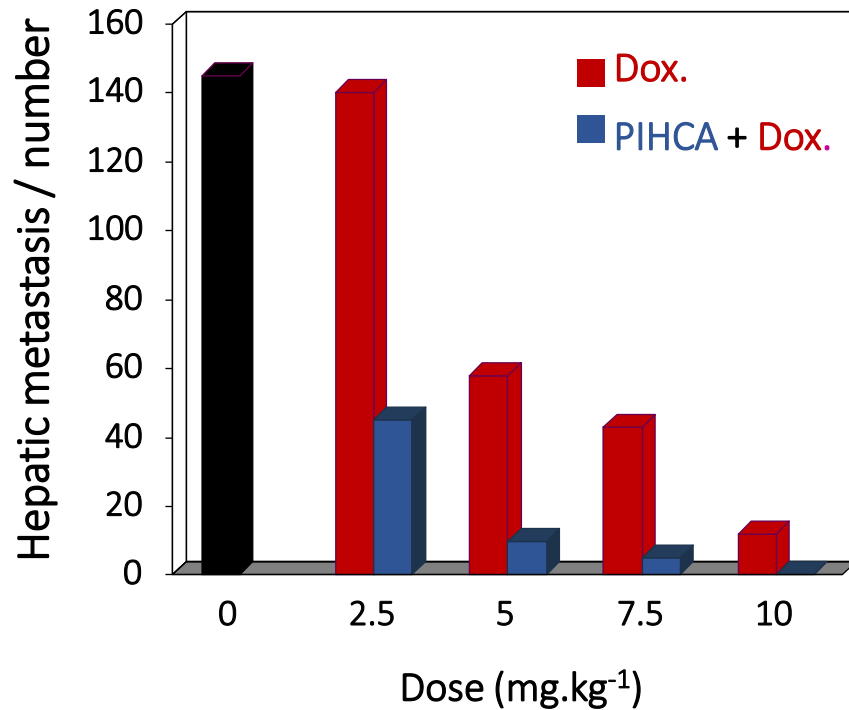


Antitumor chemotherapy

Doxorubicin _Livatag, doxorubicin transdrug



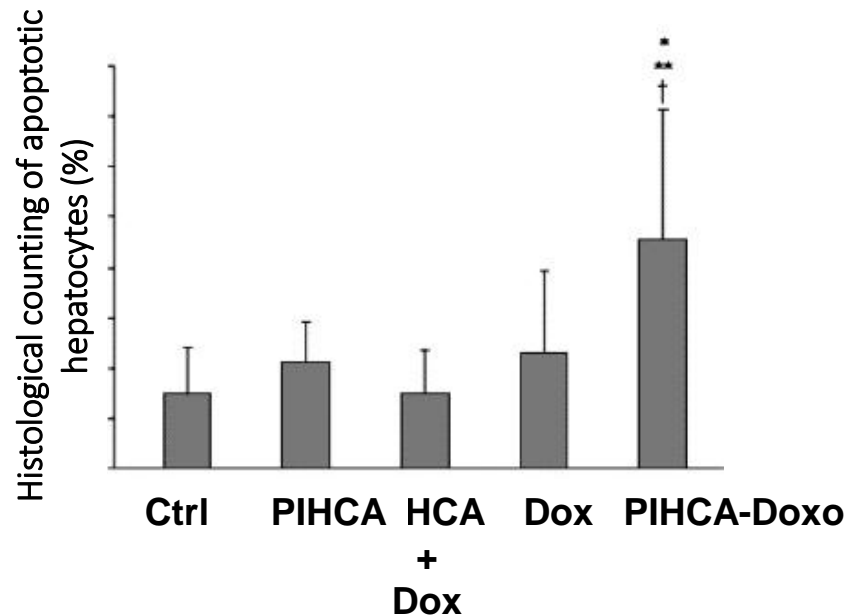
in vivo model of hepatic metastasis



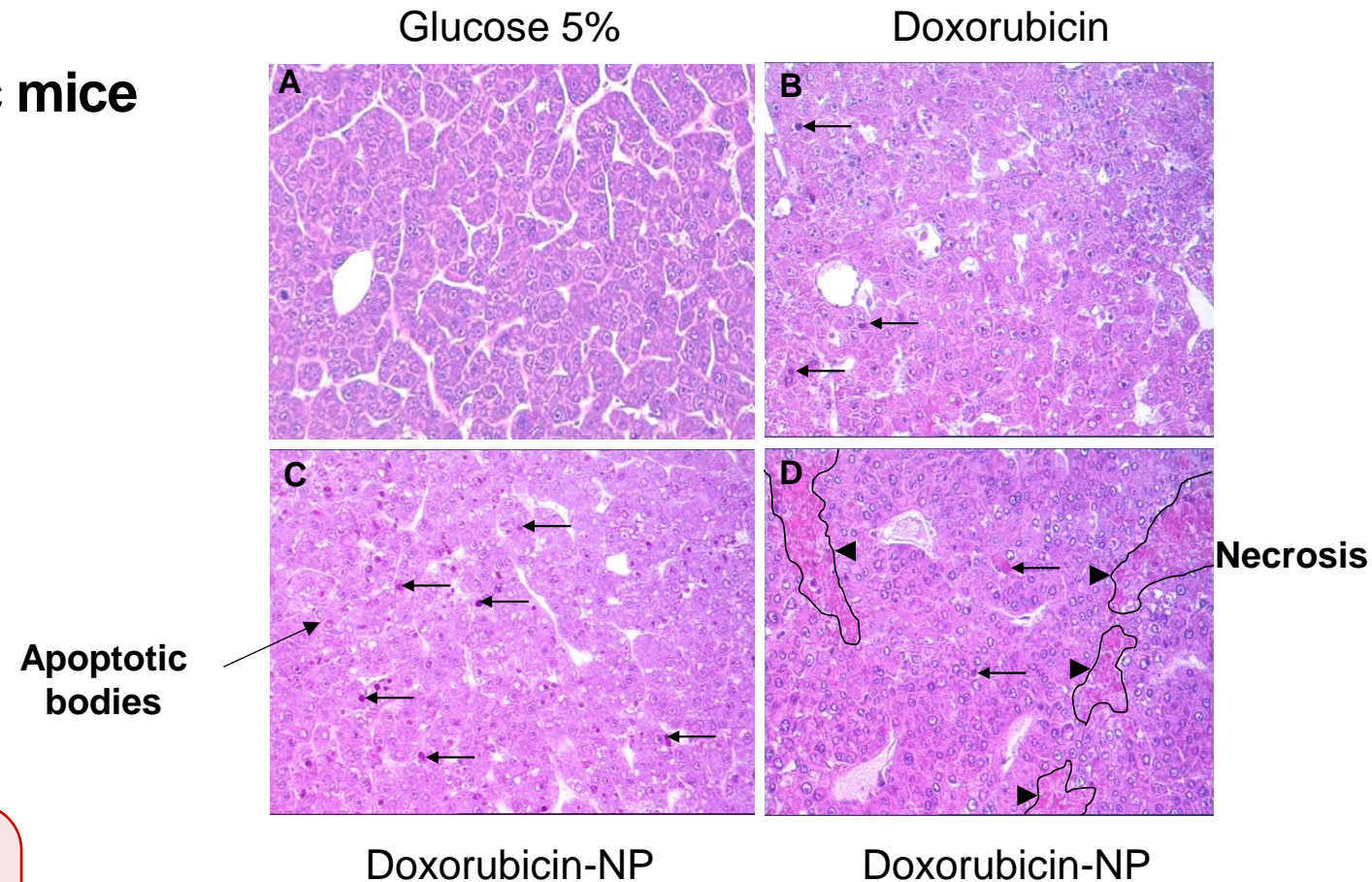
Antitumor chemotherapy

Doxorubicin _Livatag, doxorubicin transdrug

in vivo cytotoxicity in X/myc transgenic mice

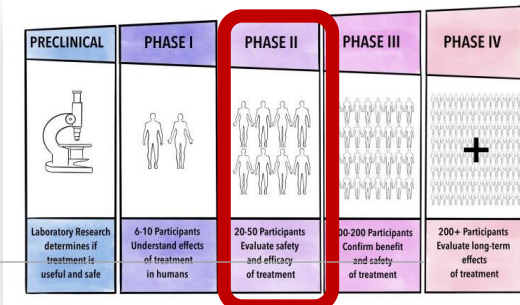


Potential breakthrough in the treatment of hepatocellular carcinoma



Antitumor chemotherapy

Doxorubicin _Livatag, doxorubicin transdrug



- PHASE II

Baseline
Tumor size 3000 mm²



intra-arterial infusion
(30 mg/m²)

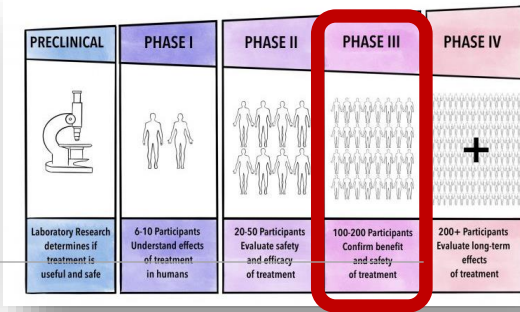


After 4 weeks
Evident necrotic area

Increased survival time 17 versus 15 months for patients getting current best of care
(transarterial chemoembolisation with a cytotoxic drug)

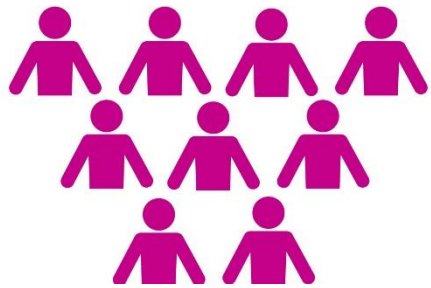
Antitumor chemotherapy

doxorubicin transdrug_ReLIVE: phase III NCT01655693

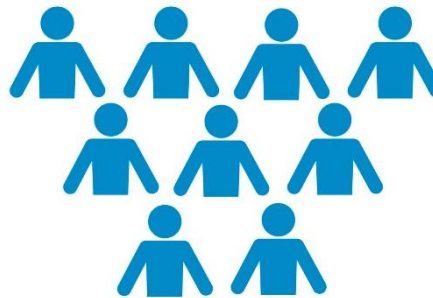


- 397 patients, 11 countries, 70 centers
- Randomized, open label, comparative 3 parallel arms study

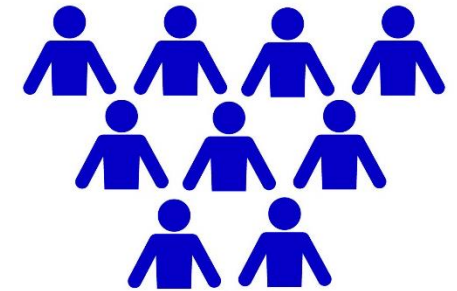
Administration through a slow 6 hours IV infusion every 4 weeks (n=263)



Best Standard Care



20 mg/m²



30 mg/m²



Antitumor chemotherapy

doxorubicin transdrug_ReLIVE: phase III *NCT01655693*

Endpoints

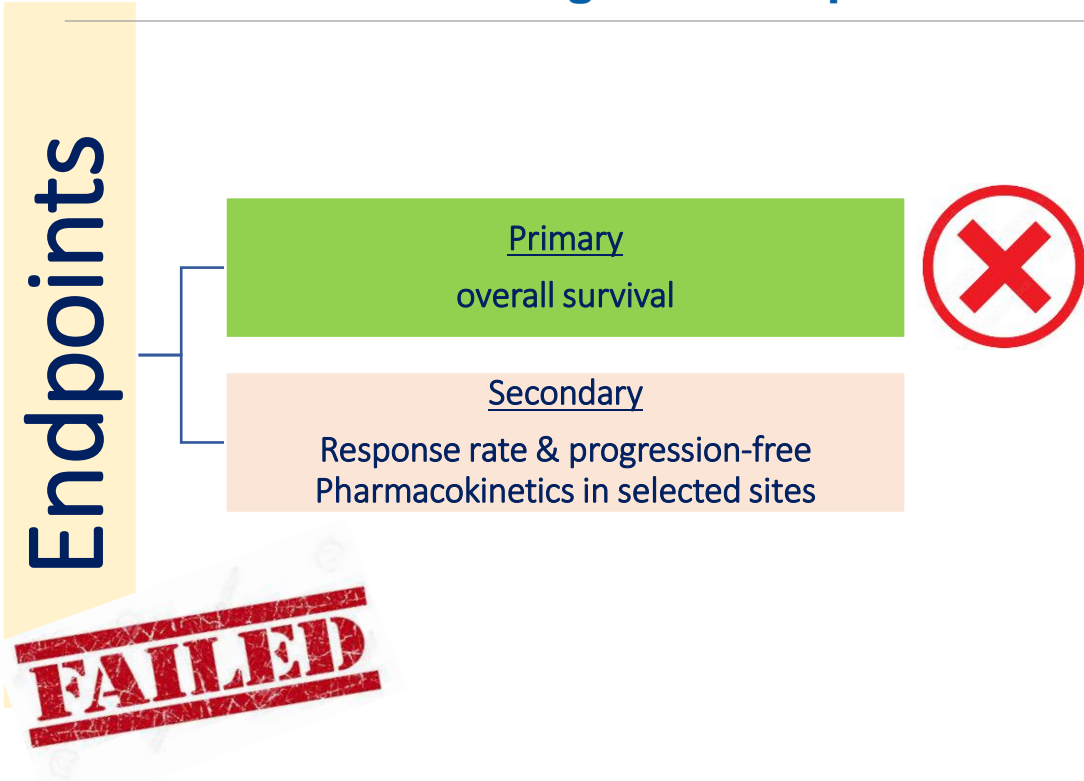
Primary
overall survival

Secondary
Response rate & progression-free
Pharmacokinetics in selected sites

ReLIVE: international phase III clinical study *NCT01655693*

Antitumor chemotherapy

doxorubicin transdrug_ReLIVE: phase III NCT01655693

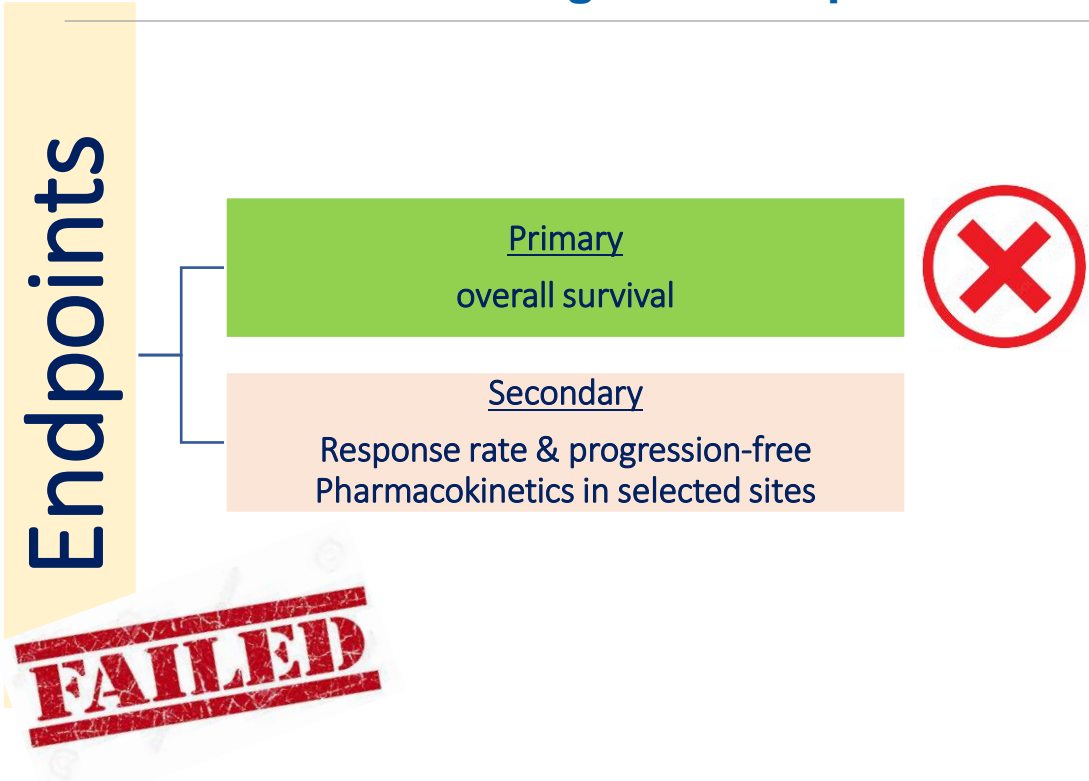


September 11, 2017

- Unexpected high survival in the comparative group
- Livatag® showed a similar effect to the control group
- No difference between the two arms (20 or 30mg/m²)
- Favorable overall safety and tolerability

Antitumor chemotherapy

doxorubicin transdrug_ReLIVE: phase III NCT01655693



WHY?

- Enrollment of patients with a better prognosis than in previous trials
- Placebo is **not** the control group
- Standard treatment is the control group (*47% gemcitabine plus oxaliplatin*)

September 11, 2017

- Unexpected high survival in the comparative group
- Livatag® showed a similar effect to the control group
- No difference between the two arms (20 or 30mg/m²)
- Favorable overall safety and tolerability

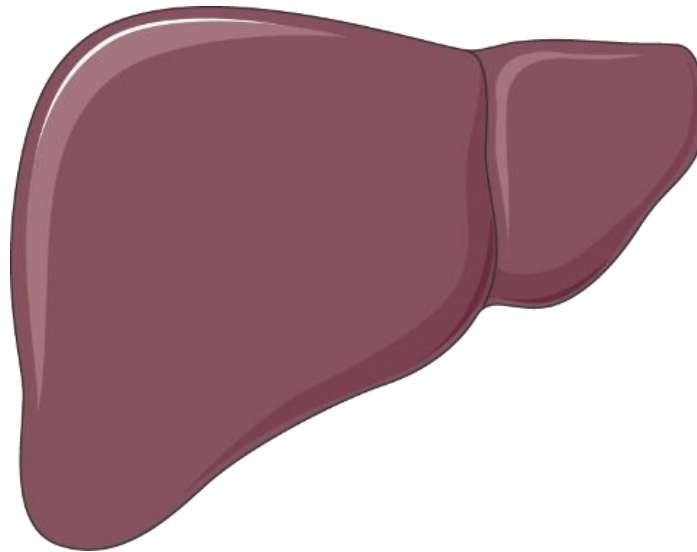


First generation

Conclusions

The first generation of nanocarriers was promising

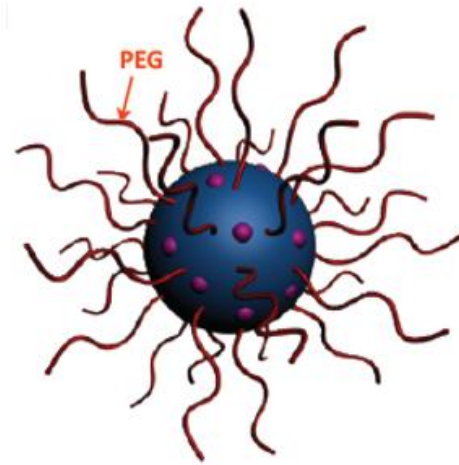
The liver is always the target, so many liver diseases are likely to benefit from such targeting



Nanomedicine generations

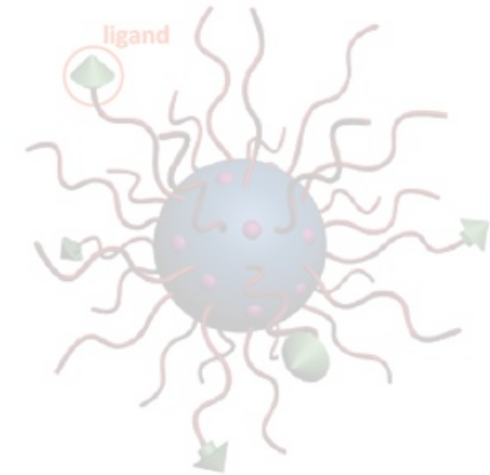


1st generation



2nd generation

Stealth/Long circulating



3rd generation

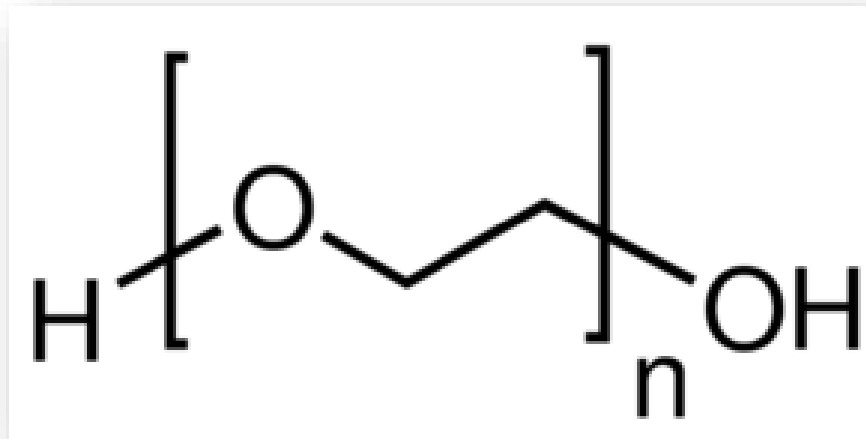
Stealth/Long circulating
Surface functionalized



In vivo fate

If you want to be invisible, look like water

Poly(ethylene glycol)

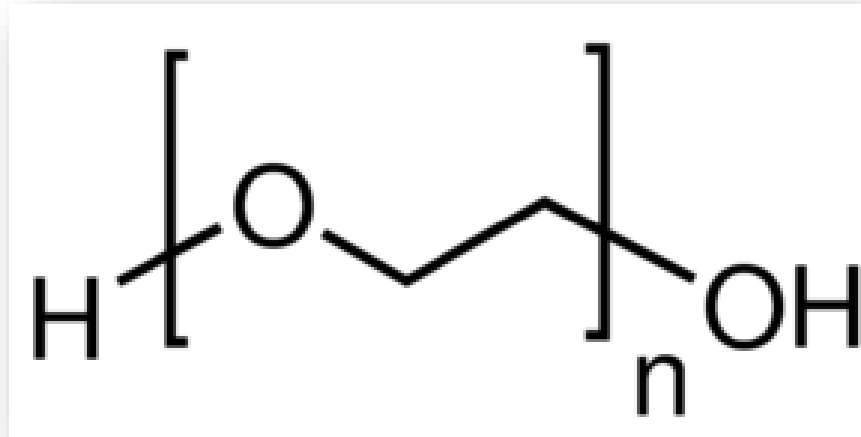


In vivo fate

If you want to be invisible, look like water

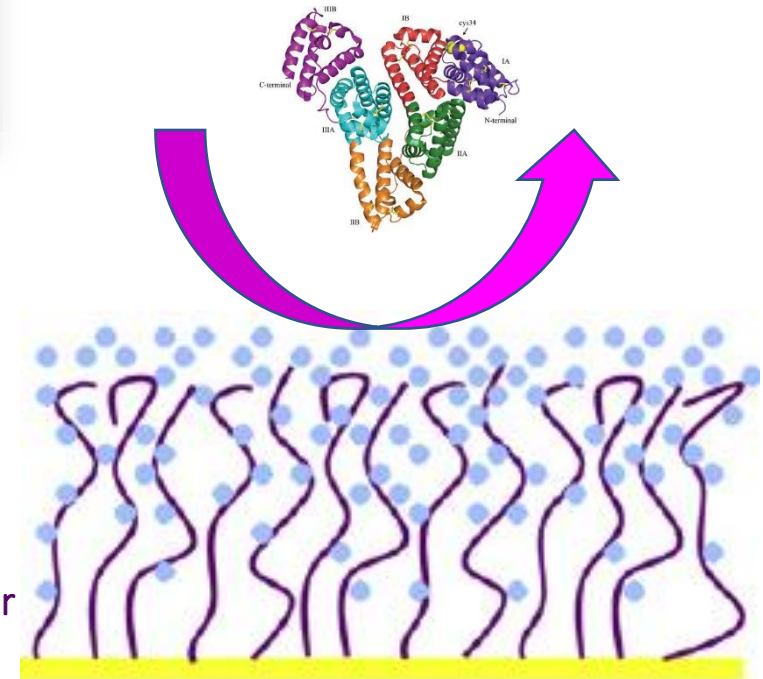
Poly(ethylene glycol)

- Non-ionic hydrophilic polymer
- Biocompatible
- Stealth effect
- Prolonged circulation



Hydration Layer

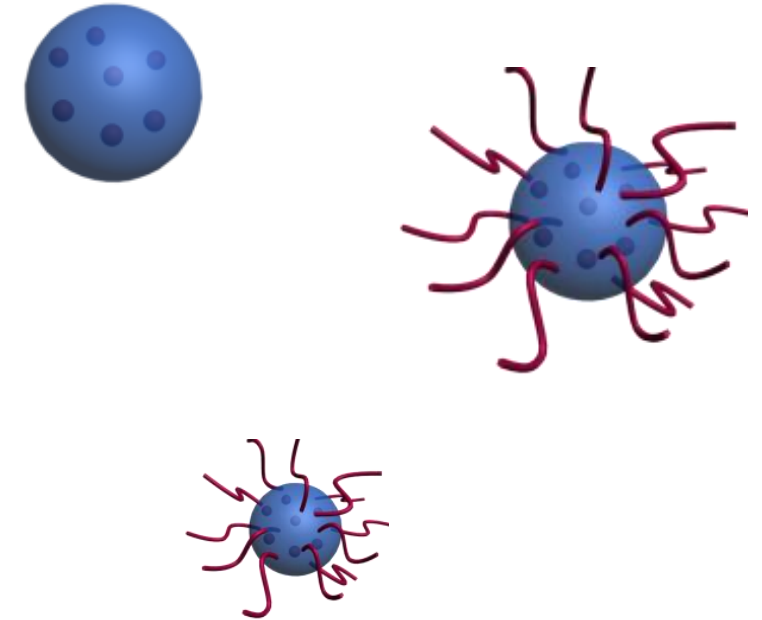
Hydrophilic polymer



In vivo fate

Poly (methoxypolyethyleneglycol)-co-nhexadecyl cyanoacrylate NPs

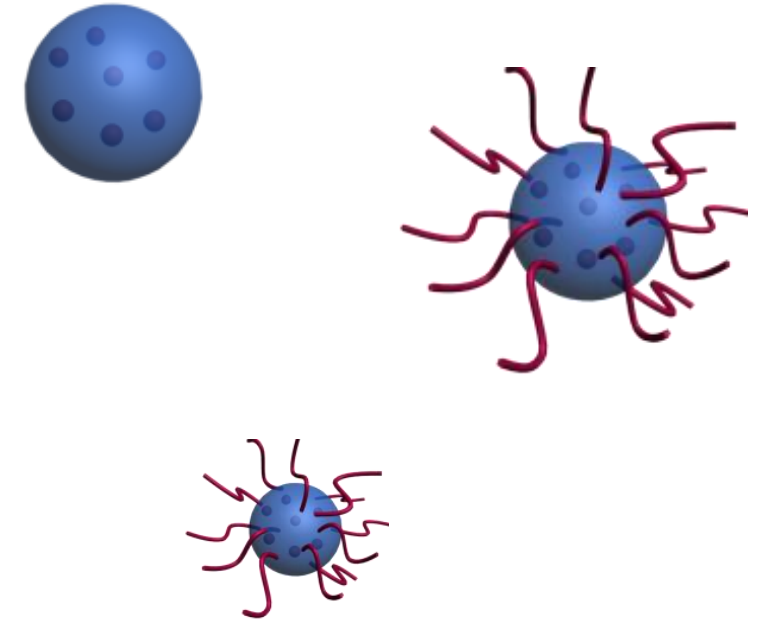
| Nanoparticles | Protein adsorbed (%) |
|--------------------------------------|----------------------|
| PEG ₅₀₀₀ -PHDCA (243 nm) | 34 |
| PEG ₅₀₀₀ -PHDCA (171 nm) | 23 |
| PEG ₅₀₀₀ -PHDCA (80 nm) | 6 |
| PEG ₂₀₀₀ -PHDCA (172 nm) | 29 |
| PEG ₁₀₀₀₀ -PHDCA (169 nm) | 9 |
| PHDCA (242 nm) | 58 |
| PHDCA (173 nm) | 56 |
| PHDCA (85 nm) | 57 |



In vivo fate

Poly (methoxypolyethyleneglycol)-co-nhexadecyl cyanoacrylate NPs

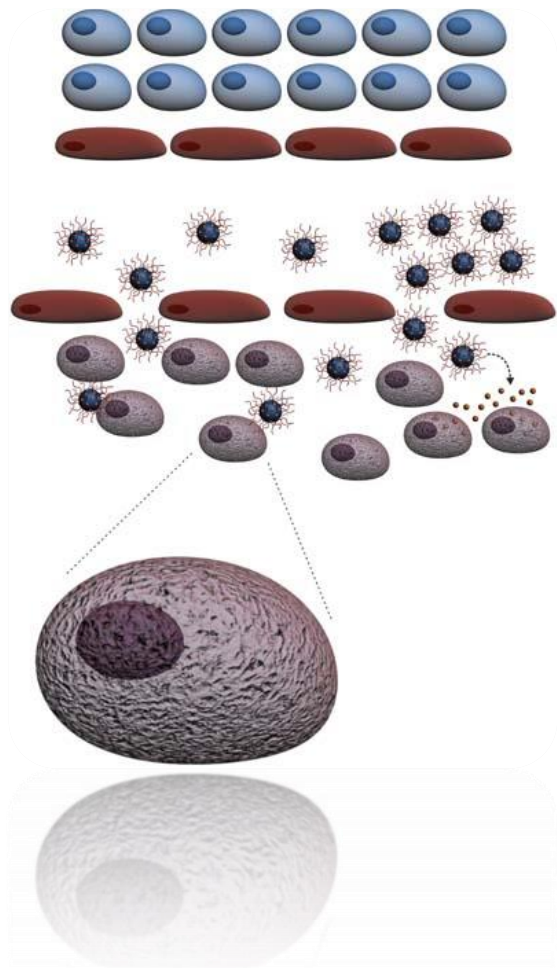
| Nanoparticles | Protein adsorbed (%) |
|--------------------------------------|----------------------|
| PEG ₅₀₀₀ -PHDCA (243 nm) | 34 |
| PEG ₅₀₀₀ -PHDCA (171 nm) | 23 |
| PEG ₅₀₀₀ -PHDCA (80 nm) | 6 |
| PEG ₂₀₀₀ -PHDCA (172 nm) | 29 |
| PEG ₁₀₀₀₀ -PHDCA (169 nm) | 9 |
| PHDCA (242 nm) | 58 |
| PHDCA (173 nm) | 56 |
| PHDCA (85 nm) | 57 |



Protein adsorption is surface and size dependent

Second generation

The enhanced permeability and retention effect (EPR)



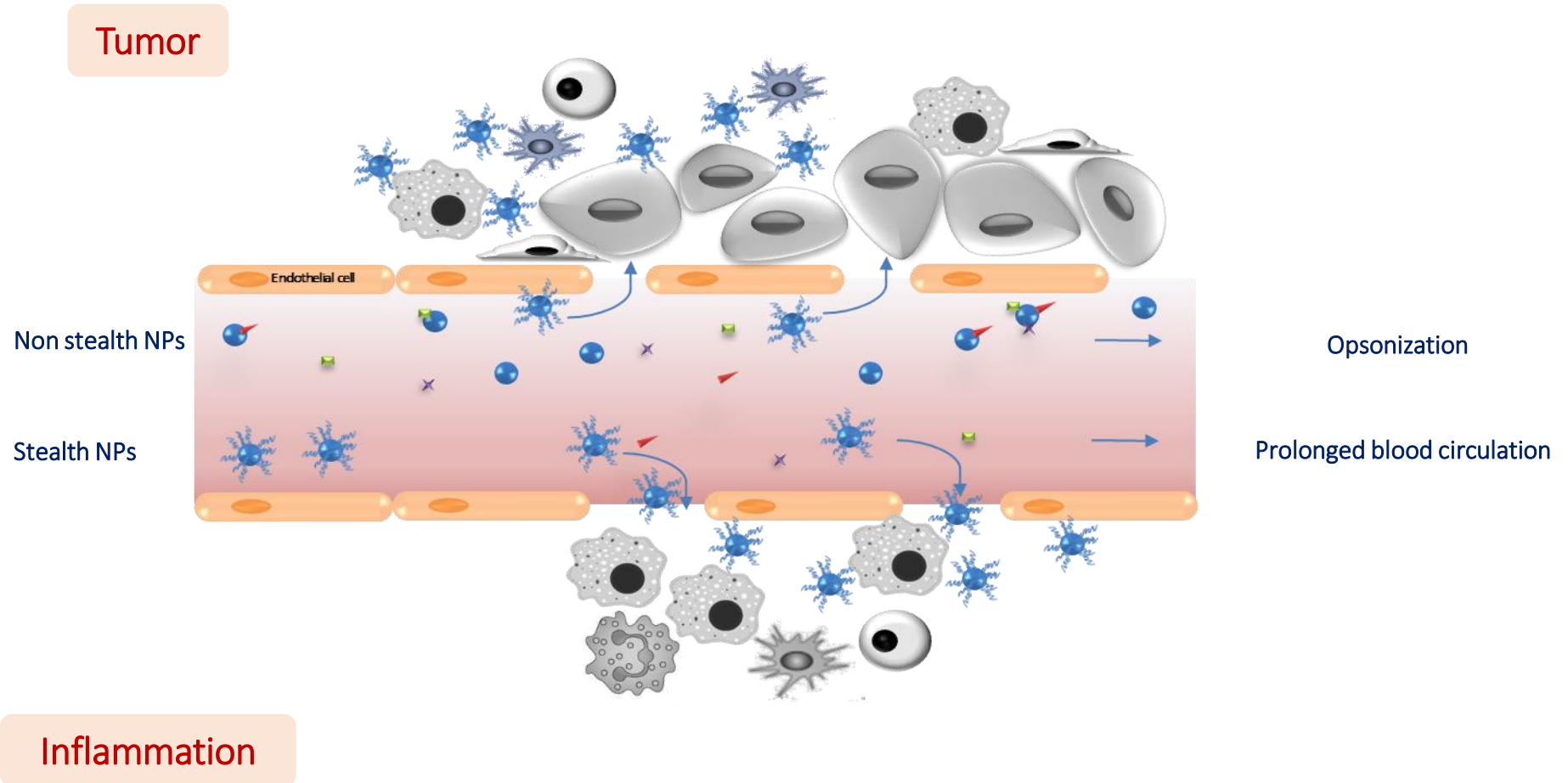
- **Enhanced permeability**
 - Stimulation of the blood vessel production
 - Important vascularization (blood supply)
 - Wide fenestrations, abnormal architectures
- **Enhanced retention**
 - Inefficient lymphatic drainage



Accumulation of nanoparticles in
tumor and inflamed tissues

Second generation

The enhanced permeability and retention effect (EPR)

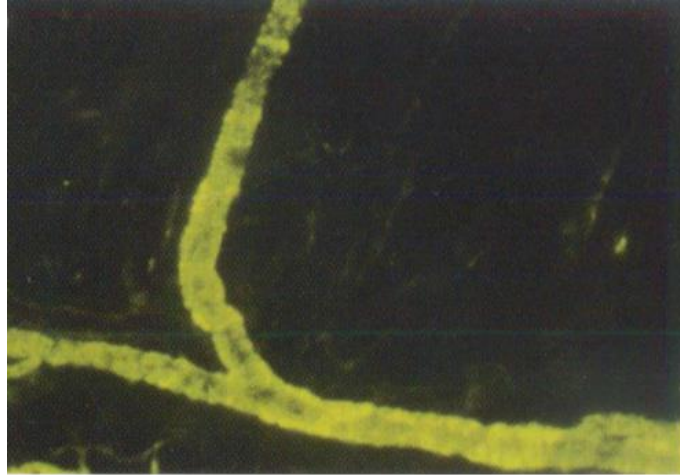


Second generation

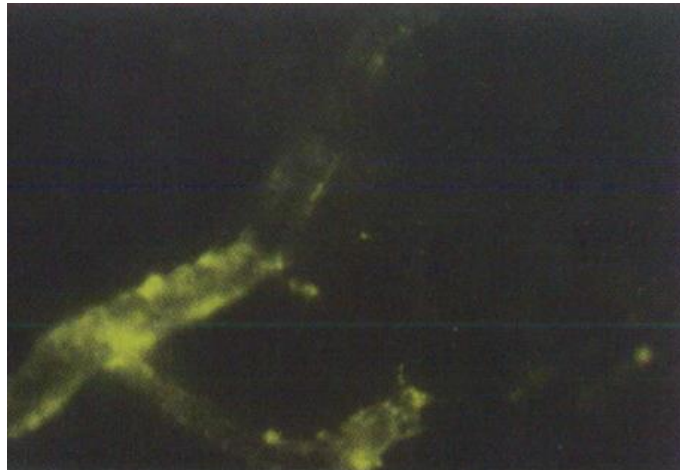
The enhanced permeability and retention effect (EPR)

Healthy tissue

@24h



@48h

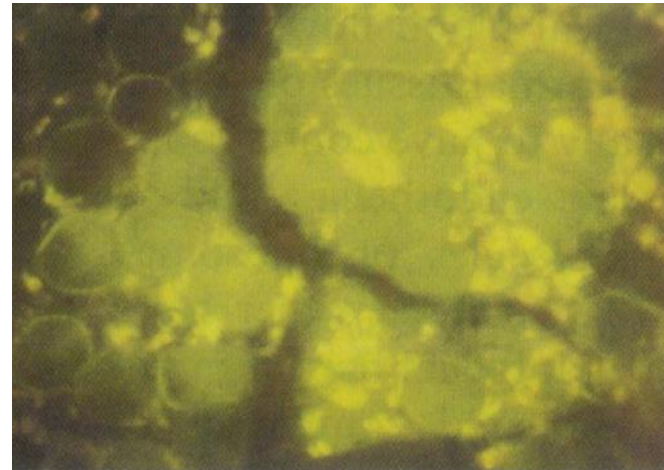


Tumor tissue

@30'

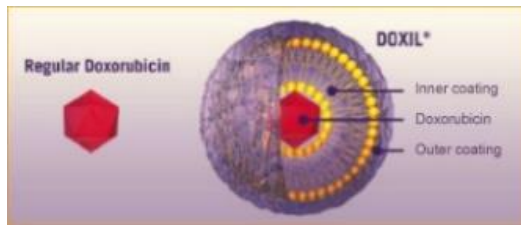


@24h

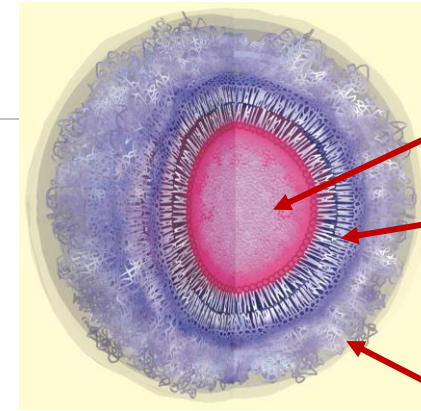
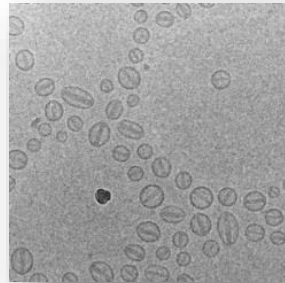


Second generation

nanomedicines in the market_Doxil (1995)



80-90 nm PEG-coated unilamellar liposomes



Doxorubicin

Lipid bilayer

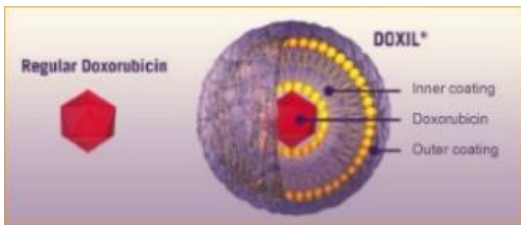
PEG

- Metastatic breast cancer
- Kaposi's sarcoma in patients with AIDS
- Multiple myeloma

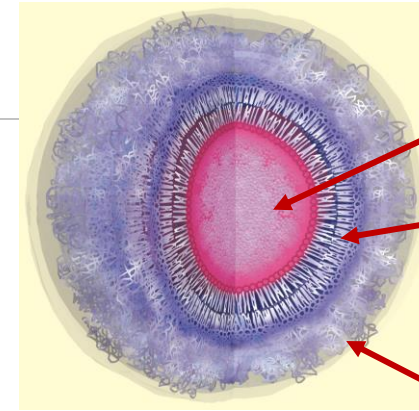
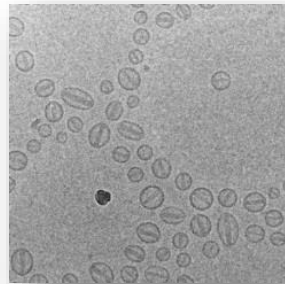
- Drug: doxorubicin

Second generation

nanomedicines in the market_Doxil (1995)



80-90 nm PEG-coated unilamellar liposomes

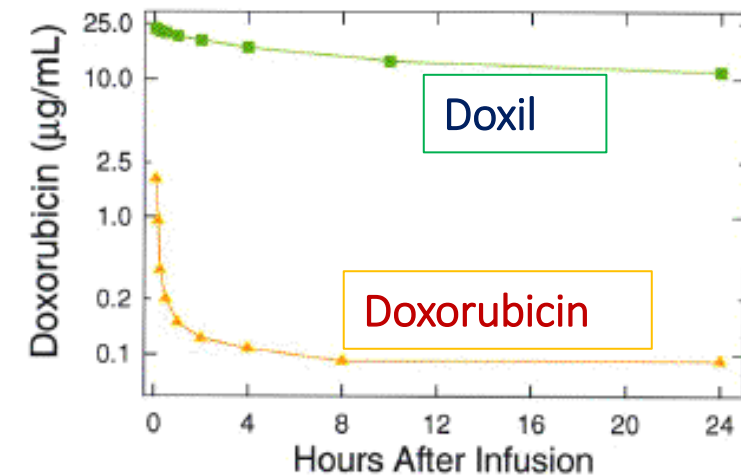


Doxorubicin

Lipid bilayer

PEG

- Plasma concentration

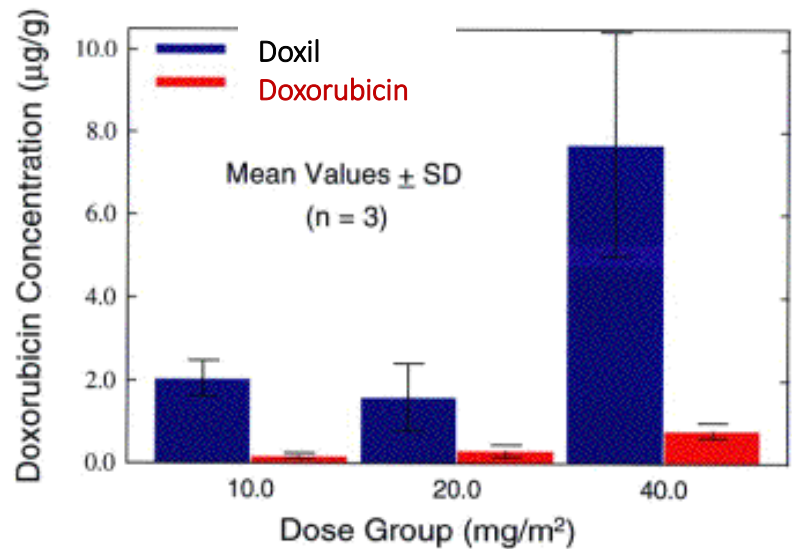
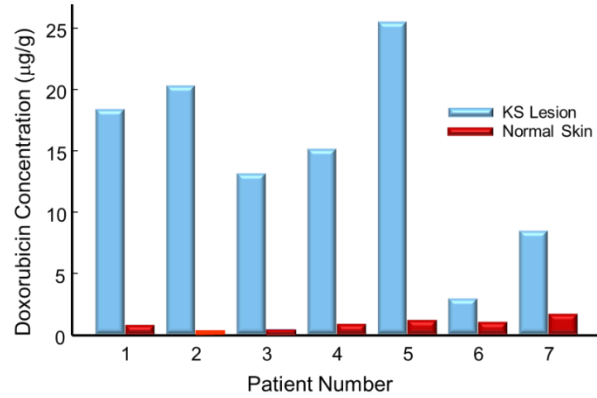


- Metastatic breast cancer
- Kaposi's sarcoma in patients with AIDS
- Multiple myeloma

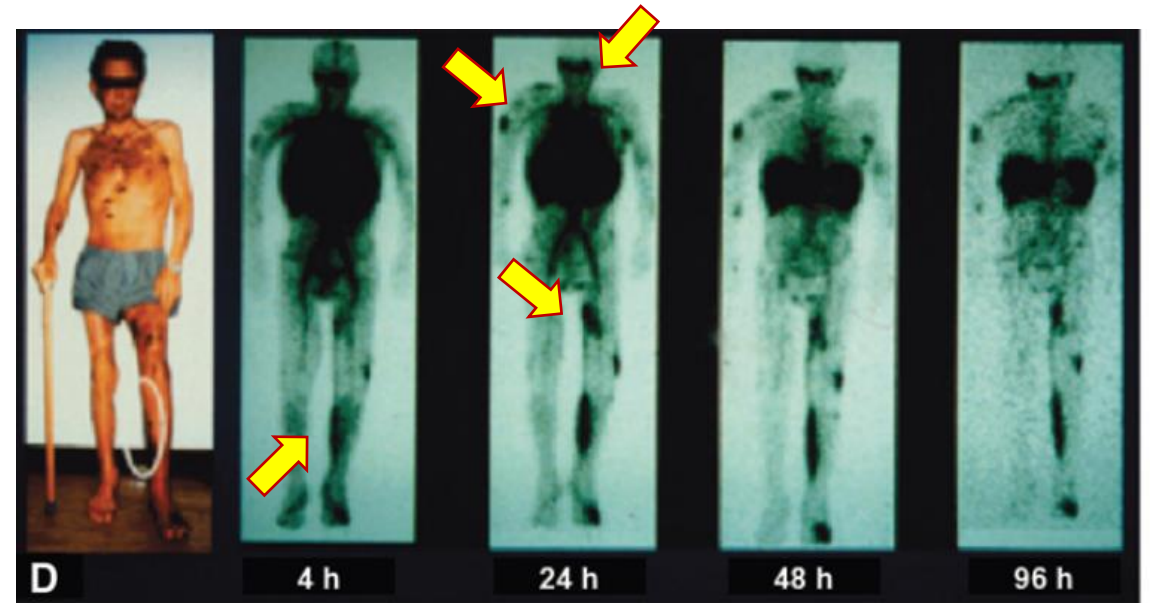
- Drug: doxorubicin

Doxil

Accumulation in KS lesions



Indium-111-labeled PEGylated liposome



Doxil

Cardiotoxicity

- Reduced
- Only 0.8% withdrawal due to cardiotoxicity
- Increasing dose and duration of treatment

Complement activation–related pseudo allergy

- Slower infusion rate
- Pretreat

Hand-foot syndrome

- Rich capillary network, increased blood flow
- Increased drug accumulation
- protracted slow release



Symptoms

| | |
|-----------|----------------------------|
| Grade I | Mild erythema |
| Grade II | Erythema with desquamation |
| Grade III | Blistering |
| Grade IV | Diffuse |

AMERICAN DREAM

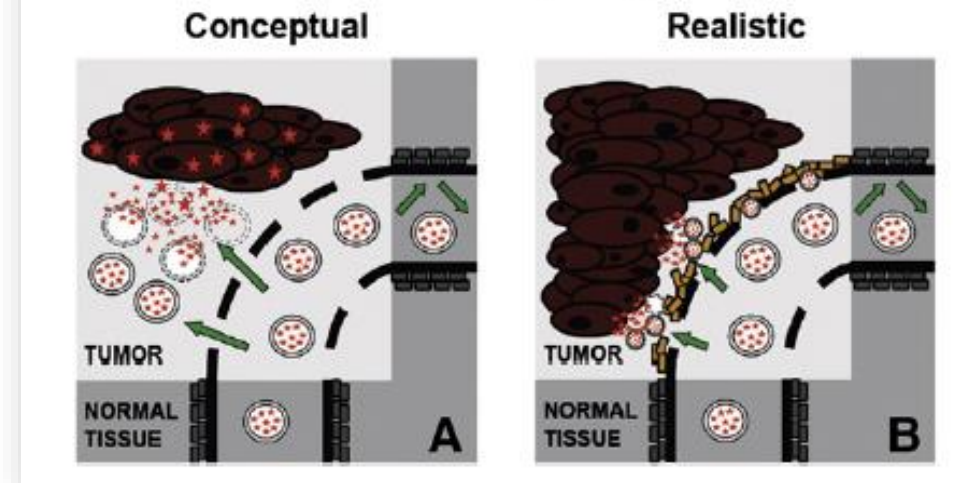
EXPECTATION



REALITY



Passive Drug Targeting

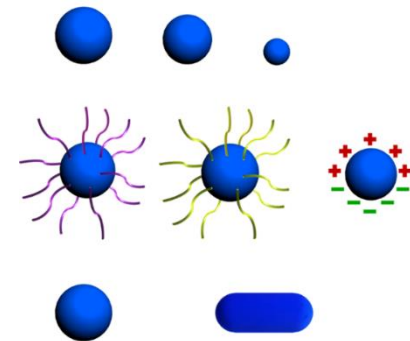


Tumor

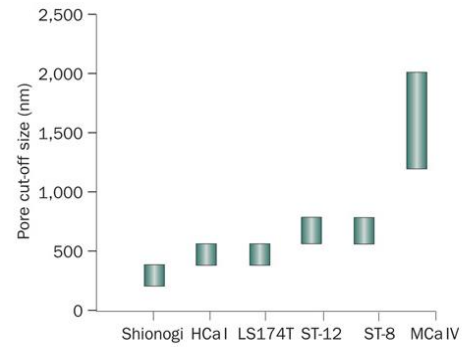
- Extent of the EPR effect and pores cut off
- Diffusion within the extracellular matrix
- Hydrostatic pressure within the tumor

Particles

- Mean diameter
- Charge and surface chemistry
- Shape

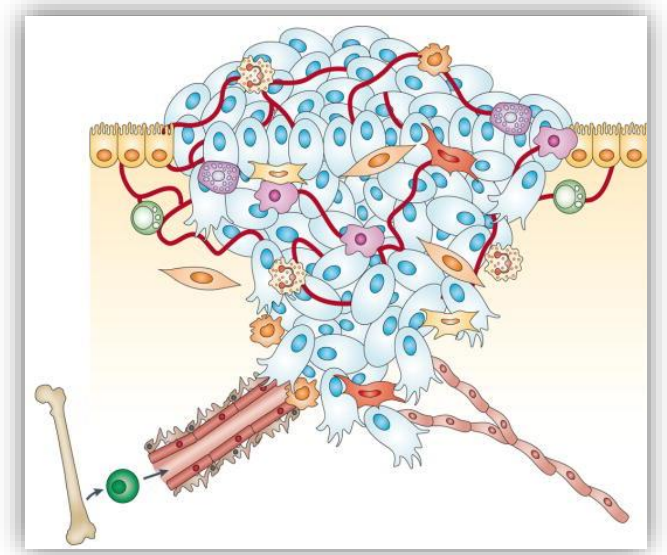


Variable pore size

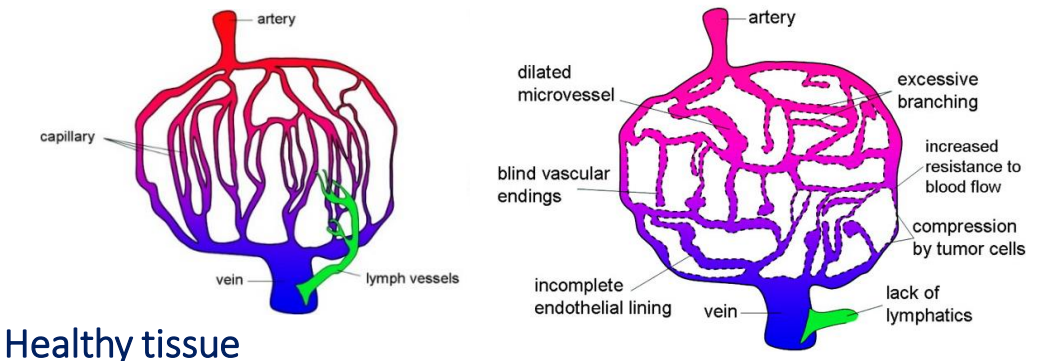


Hobbs, S. K. et al. Proc. Natl Acad. Sci. USA, 1998, 95, 4607

Heterogeneous tumor composition



Heterogeneous vasculature



Healthy tissue

Correlate EPR effect and response to treatment

Evaluate the extent of the vasculature leakage and tumor drug accumulation



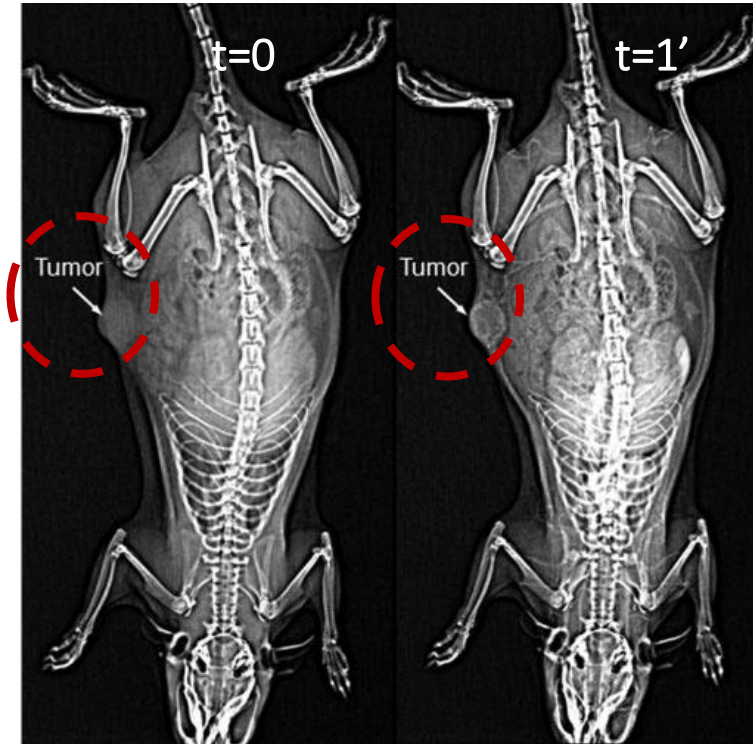
Predict the outcome of the treatment

Correlate EPR effect and response to treatment

Evaluate the extent of the vasculature leakage and tumor drug accumulation



Predict the outcome of the treatment



Good prognosis groups

highest X-Ray signal enhancement

Bad prognosis groups

lowest X-Ray signal enhancement

Iv injection of iodine-labeled liposomes

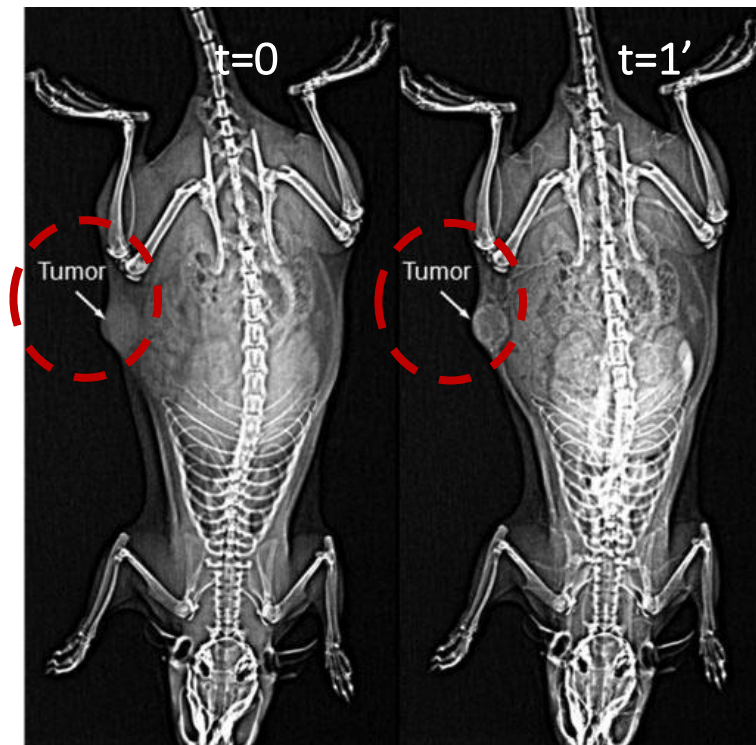
Vasculature visualization of tumor site and normal tissues

Correlate EPR effect and response to treatment

Evaluate the extent of the vasculature leakage and tumor drug accumulation



Predict the outcome of the treatment



Iv injection of iodine-labeled liposomes

Good prognosis groups

highest X-Ray signal enhancement

- Slower tumor grow rate
- leakier vasculature

Bad prognosis groups

lowest X-Ray signal enhancement

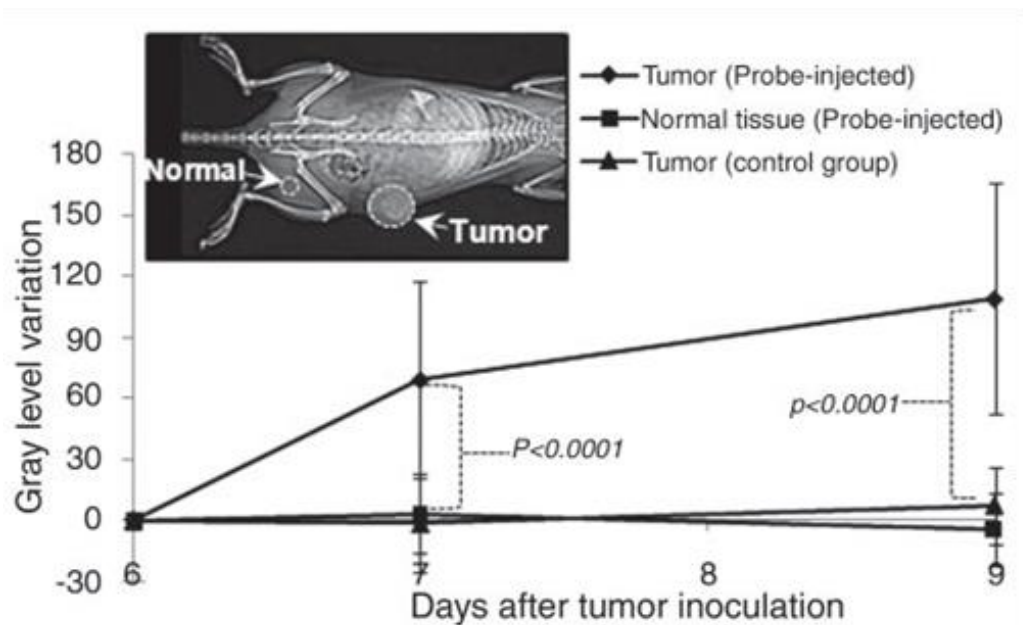
- Faster tumor grow rate
- intact vasculature

Doxorubicin-loaded liposomes treatment

Vasculature visualization of tumor site and normal tissues

Correlate EPR effect and response to treatment

- Gray levels signal enhancement



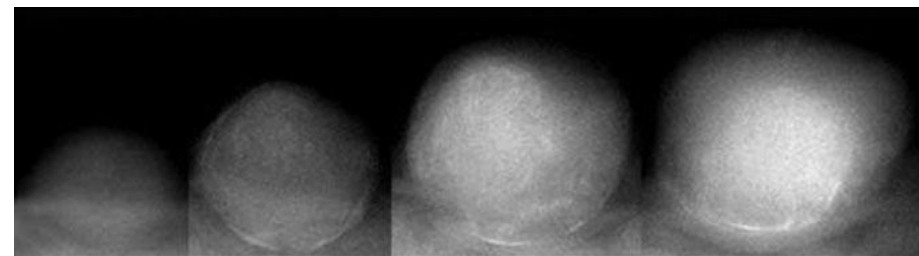
After probe administration:

- highest enhancement in tumor tissue
- no substantial enhancement in normal tissue

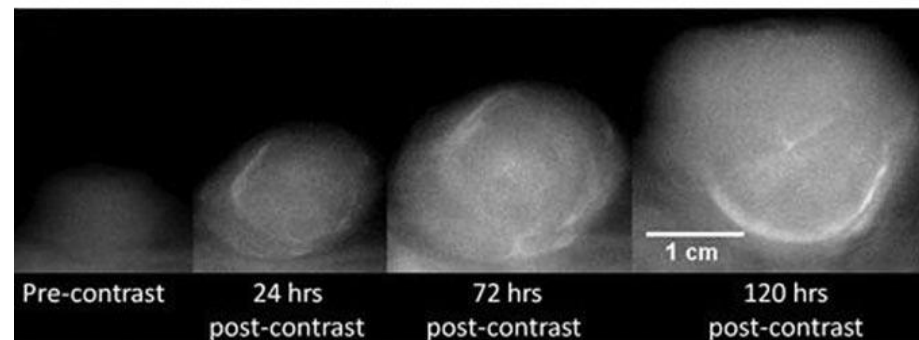
Without probe administration:

- no enhancement in tumor lesion of control group

Tumor A

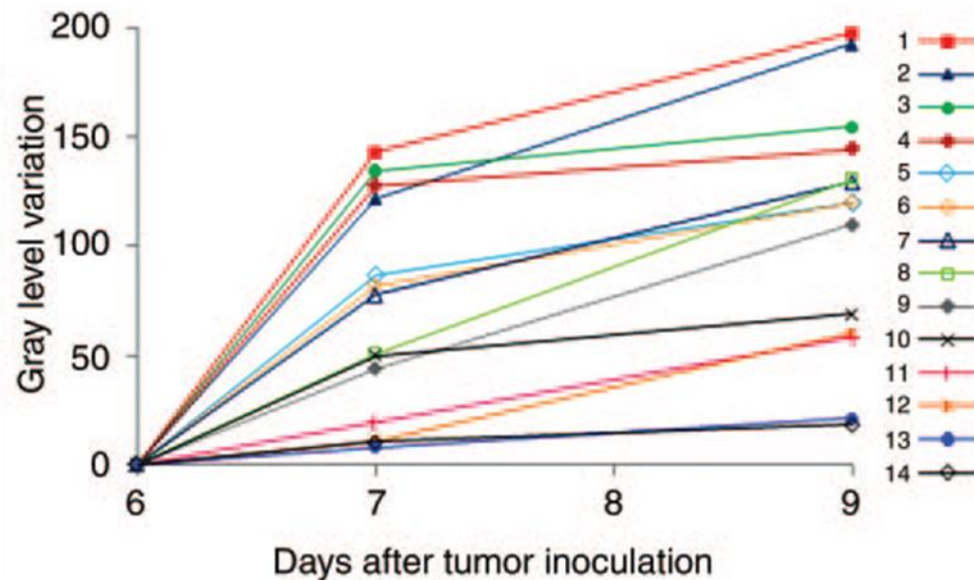


Tumor B



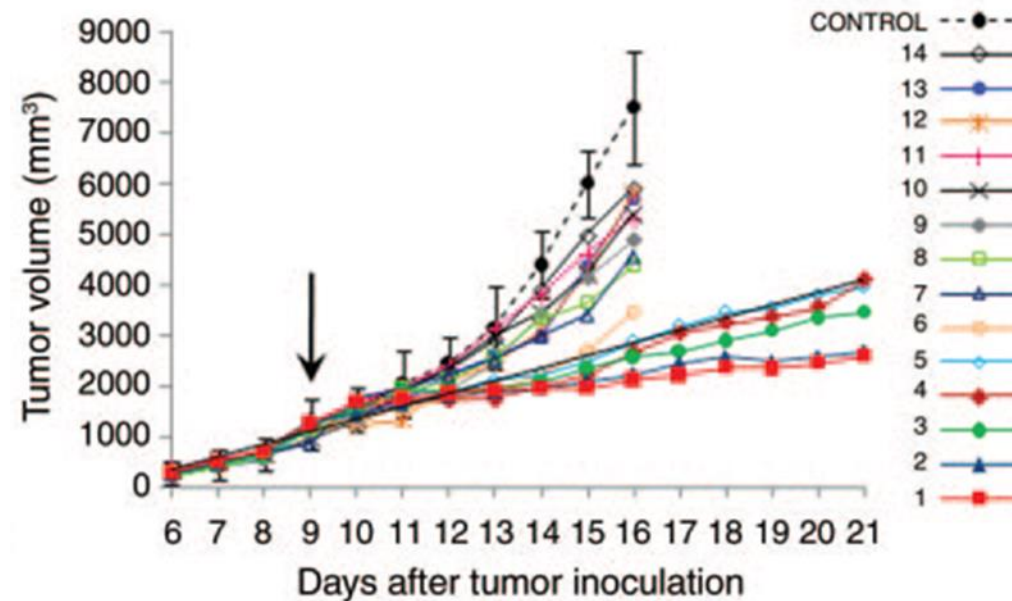
Correlate EPR effect and response to treatment

- Tumor permeability



High variability of tumor leakiness

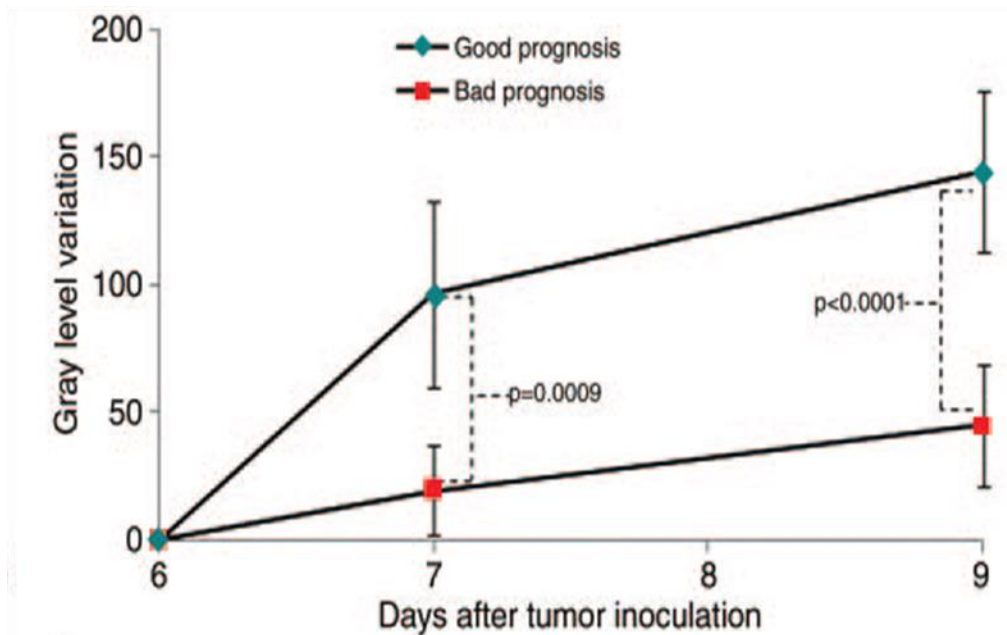
- In vivo efficacy



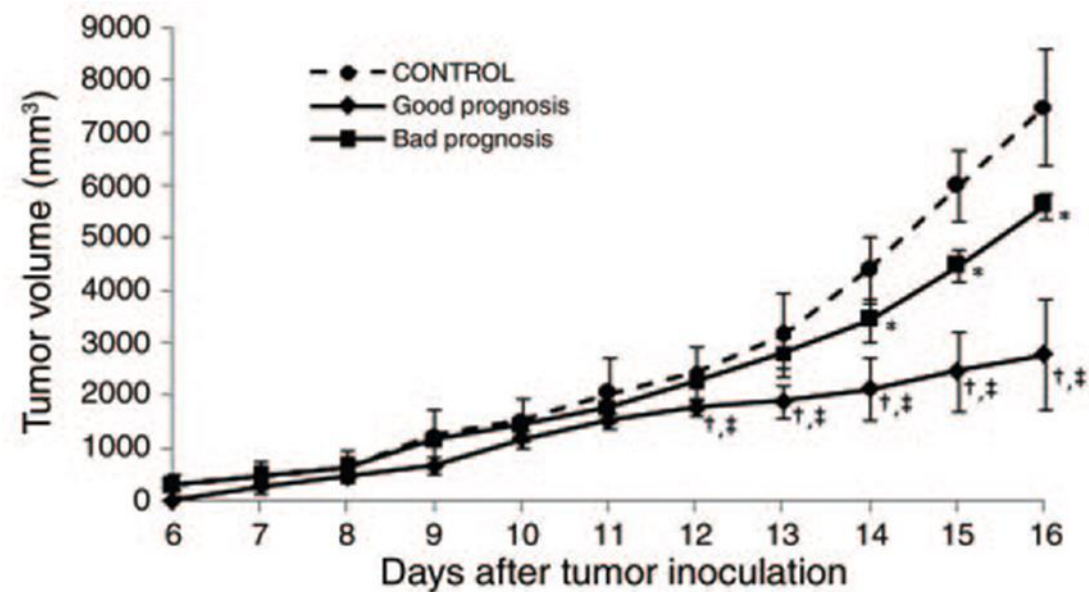
High variability of tumor response

Correlate EPR effect and response to treatment

- Tumor permeability



- In vivo efficacy

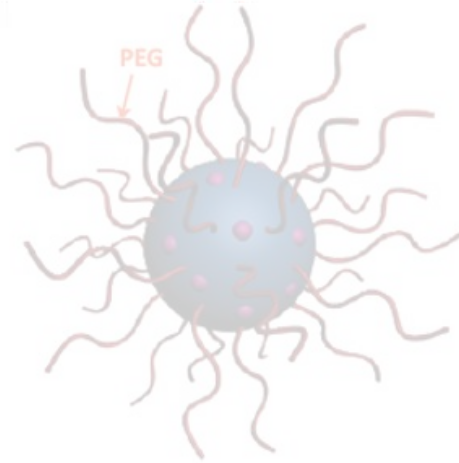


Significant higher response to chemotherapy of good-prognosis subgroup

Nanomedicine generations

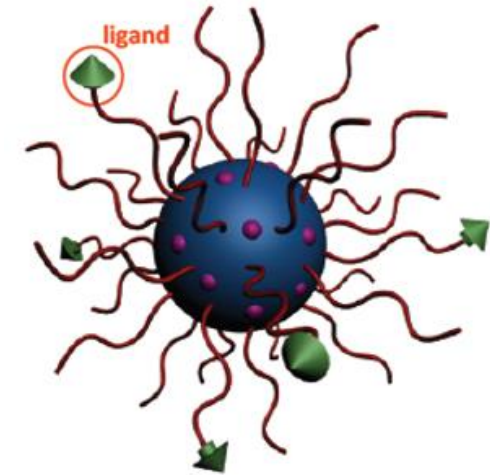


1st generation



2nd generation

Stealth/Long circulating



3rd generation

Stealth/Long circulating
Surface functionalized

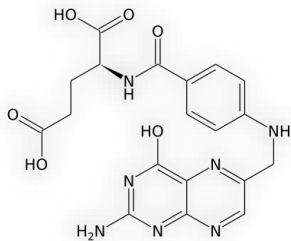


Third generation

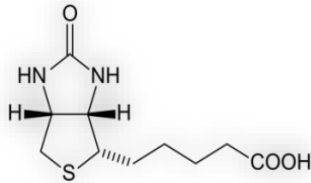
ligand mediated targeting

• Small molecules

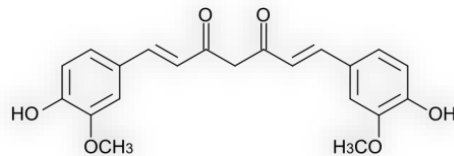
Folic acid



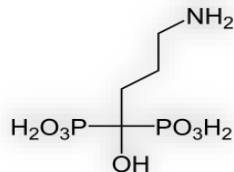
Biotin



Curcumin

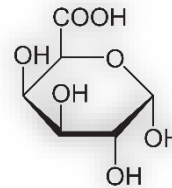


Alendronate

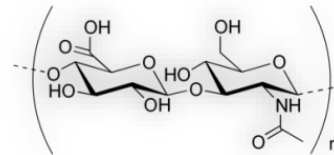


• Carbohydrates

Galactose



Hyaluronan



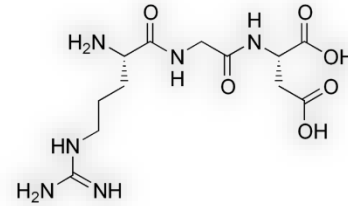
• Antibodies



• Peptides/proteins

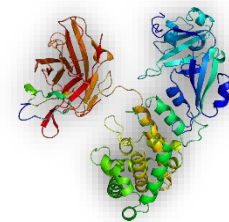
RGD peptides

GRGDS
CRGDKGPDC
Cyclo(RGDDFK)

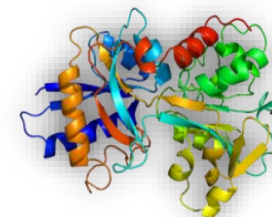


Cell penetrating peptides

EGF



Transferrin



Third generation

ligand mediated targeting

THE JOURNAL OF BIOLOGICAL CHEMISTRY
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Vol. 269, No. 5, Issue of February 4, pp. 3198-3204, 1994
Printed in U.S.A.

Delivery of Liposomes into Cultured KB Cells via Folate Receptor-mediated Endocytosis*

(Received for publication, June 25, 1993, and in revised form, September 1, 1993)

Robert J. Lee and Philip S. Low‡

From the Department of Chemistry, Purdue University, West Lafayette, Indiana 47907

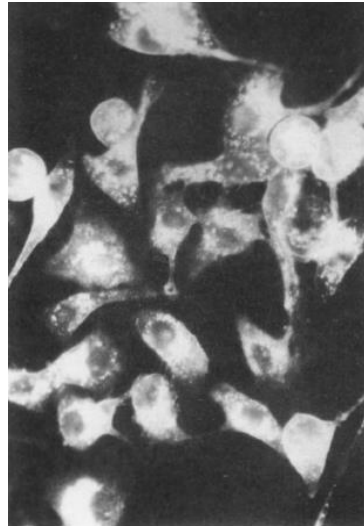


- Uptake *Confocal microscopy*

4h @ 37°C

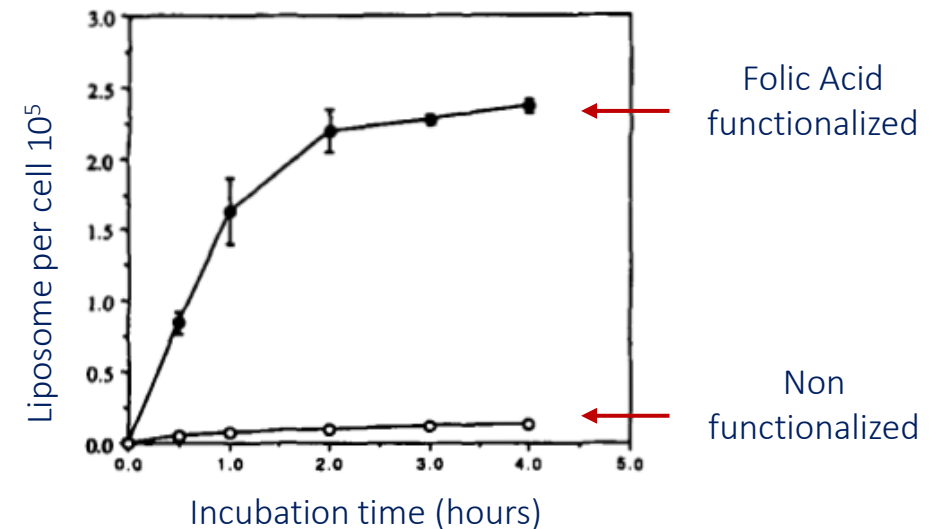


Non functionalized



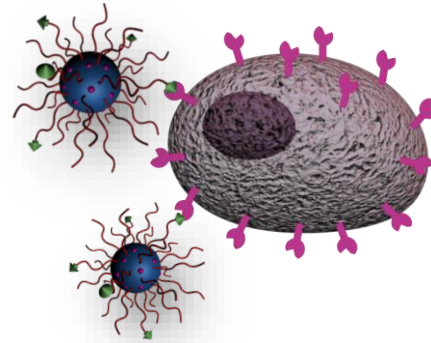
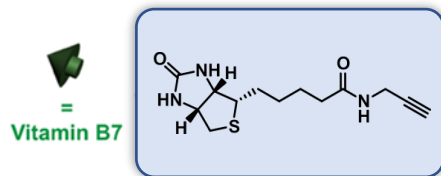
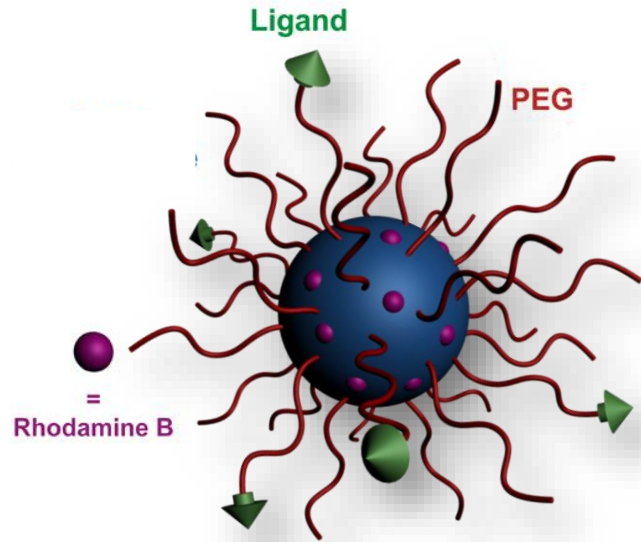
Folic Acid functionalized

- Internalization kinetic *fluorescence spectroscopy*

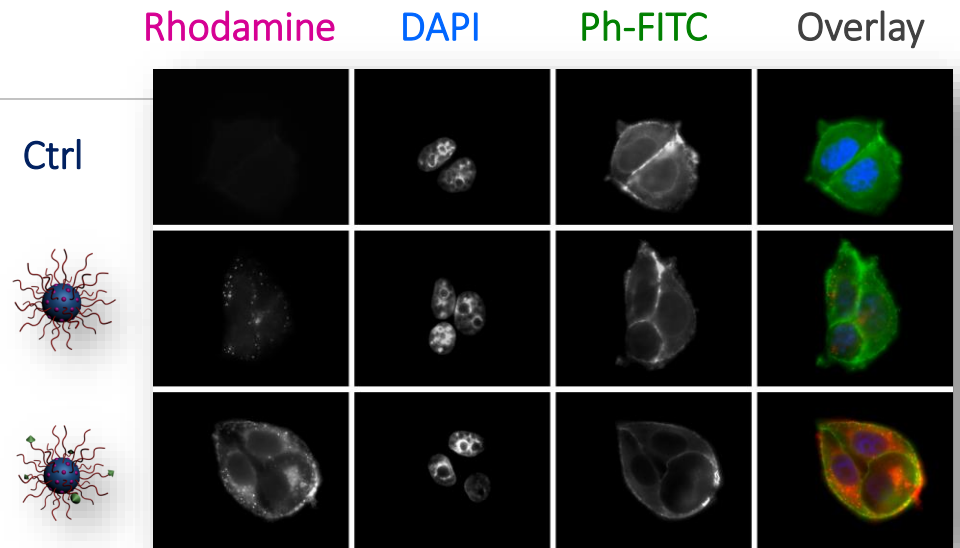


Third generation

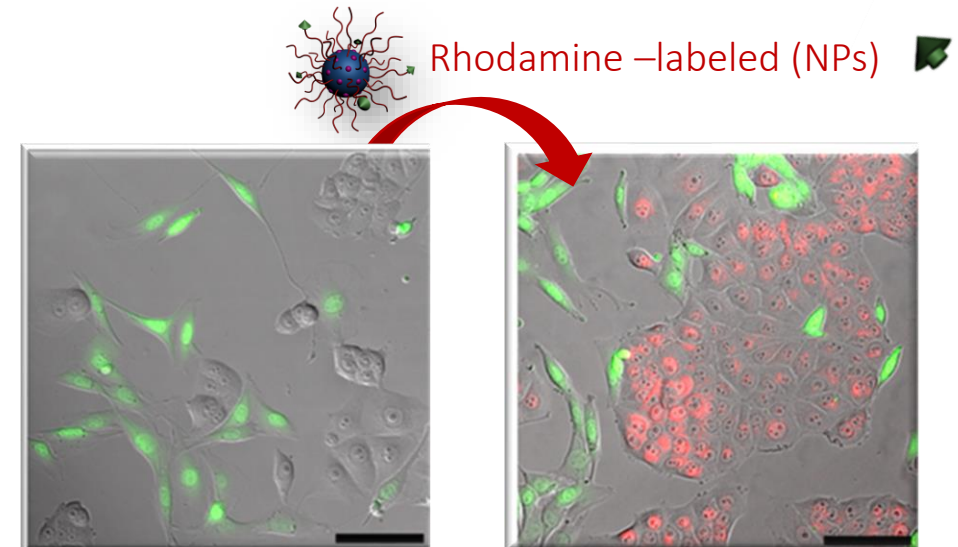
ligand mediated targeting



- Uptake



- Selectivity



- Green-labeled fibroblasts
- Unstained cancer cells

Third generation

ligand mediated targeting






Table 1. Clinical trials for actively targeted cancer nanomedicines

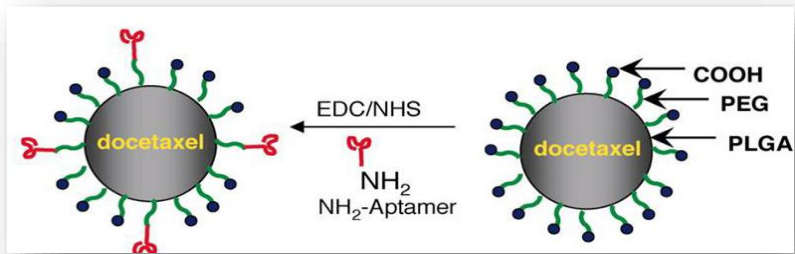
| Ligand type | Name | Ligand | Target | Nanocarrier | Payload | Indication | NCT no. | Status | Ref. |
|--------------------|--------------|-------------------------------|------------------|-------------------------|-----------------------------|----------------------------|------------|---------------------|---------------------|
| Antibodies | TargomiRs | Anti-EGFR bispecific antibody | EGFR | Minicell | miR-16-based microRNA mimic | NSCLC MPM | 02369198 | Phase I | 165 |
| Antibody fragments | C225-ILs-DOX | Anti-EGFR Fab' | EGFR | Liposome | DOX | Solid tumors | 01702129 | Phase I | 188 |
| | MM-302 | Anti-HER2 scFv | HER2 | Liposome | DOX | Breast cancer | 01304797 | Phase I | 189 |
| | SGT-53 | Anti-TfR scFv | TfR | Liposome | p53 plasmid | Solid tumors | 00470613 | Phase I | 190 |
| | | | | | | Pancreatic cancer | 02340117 | Phase II | 204 |
| | SGT-94 | Anti-TfR scFv | TfR | Liposome | RB94 plasmid | GUC | 01517464 | Phase I | 191 |
| | Lipovaxin-MM | Anti-DC-SIGN V _H | DC-SIGN | Liposome | Melanoma antigens and IFN-γ | Melanoma | 01052142 | Phase I | 192 |
| Proteins | MBP-426 | Tf | TfR | Liposome | Oxaliplatin | Solid tumors AGC or EAC | 00355888 | Phase I | 248 |
| | CALAA-01 | Tf | TfR | Polymeric nanoparticles | RRM2 siRNA | Solid tumors | 00964080 | Phase I/II | 249 |
| Peptides | 2B3-101 | GSH | GSH transporters | Liposome | DOX | Breast cancer | 01386580 | Phase I/II | 279 |
| | Rexin-G | vWF-derived motif | Collagen | Retroviral vector | dn-CCNG1 | Osteosarcoma | 00572130 | Phase II | 259 |
| | | | | | | Sarcoma | 00505713 | Phase I/II | 259 |
| | | | | | Pancreatic cancer | 00504998 | Phase I/II | 260 | |

AGC advanced gastric cancer, *dn-CCNG1* dominant-negative mutant construct of cyclin G1, DOX doxorubicin, EAC esophageal adenocarcinoma, GUC genitourinary cancers, MPM malignant pleural mesothelioma, NSCLC non-small cell lung cancer, Tf transferrin, vWF Von Willebrand factor

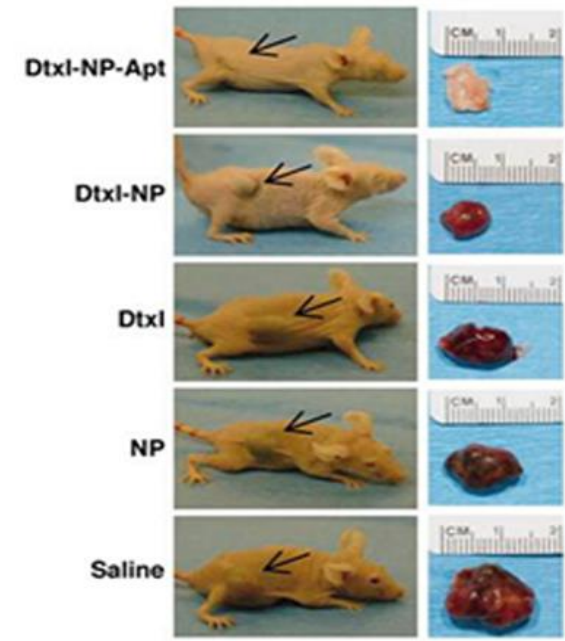
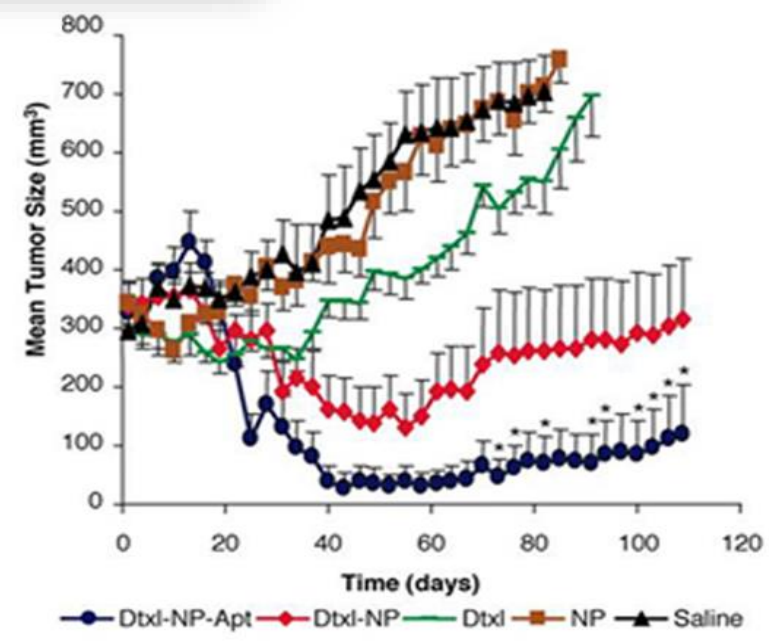
Third generation

prostate specific membrane antigen (PSMA) targeting

| PRECLINICAL | PHASE I | PHASE II | PHASE III | PHASE IV |
|--|---|---|---|---|
|  |  |  |  |  |
| Laboratory Research determines if treatment is useful and safe | 6-10 Participants Understand effects of treatment in humans | 20-50 Participants Evaluate safety and efficacy of treatment | 100-200 Participants Confirm benefit and safety of treatment | 200+ Participants Evaluate long-term effects of treatment |

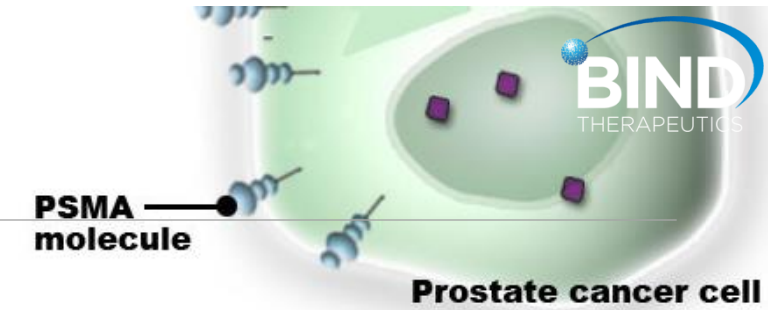


Intratumoral injection

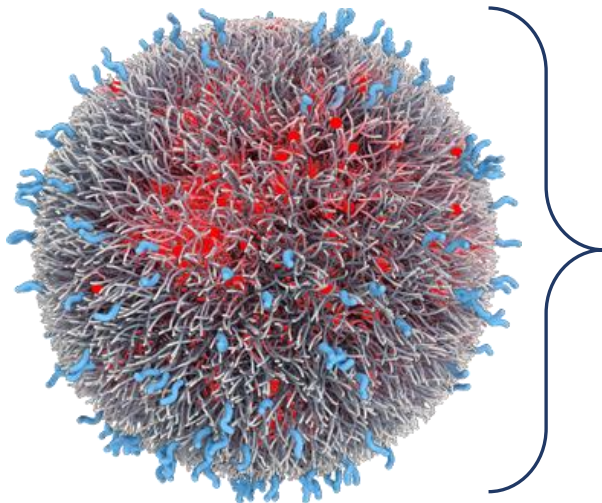


Third generation

prostate specific membrane antigen (PSMA) targeting



Accurins



Targeting ligands
Stealth and protective layer
Controlled-release polymer matrix
Therapeutic payload



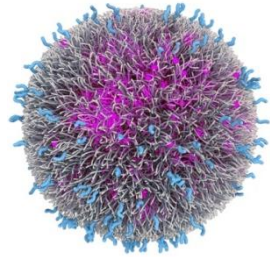
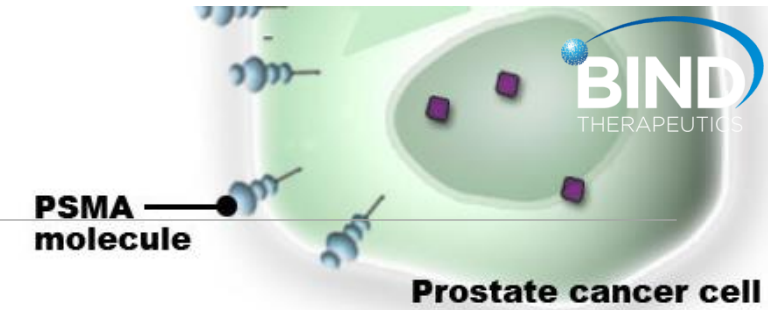
- **BIND-014** (PSMA-targeted docetaxel)
- **BIND-510** PSMA-targeted vincristine
- **PLK1, KSP inhibitor accurins**

| TUMOR | PATIENTS EXPRESSING PSMA | |
|---------------------|--------------------------|----------------|
| | TUMOR CELLS | NEOVASCULATURE |
| Prostate | 184/184 (100%) | 2/12 (17%) |
| Breast | 0/6 (0%) | 5/6 (83%) |
| Colorectal | 0/130 (0%) | 110/130 (85%) |
| Renal Cell | 0/75 (0%) | 67/75 (89%) |
| Bladder | 8/167 (5%) | 167/167 (99%) |
| Gastric | 0/119 (0%) | 79/119 (66%) |
| Neuroendocrine | 0/5 (0%) | 5/5 (100%) |
| Melanoma | 0/5 (0%) | 5/5 (100%) |
| Pancreatic Duct | 0/4 (0%) | 4/4 (100%) |
| NSCLC | 0/5 (0%) | 5/5 (100%) |
| Soft Tissue Sarcoma | 0/6 (0%) | 5/6 (83%) |

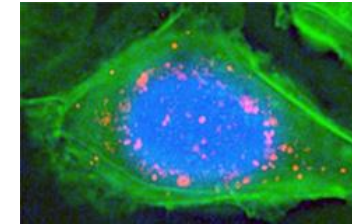
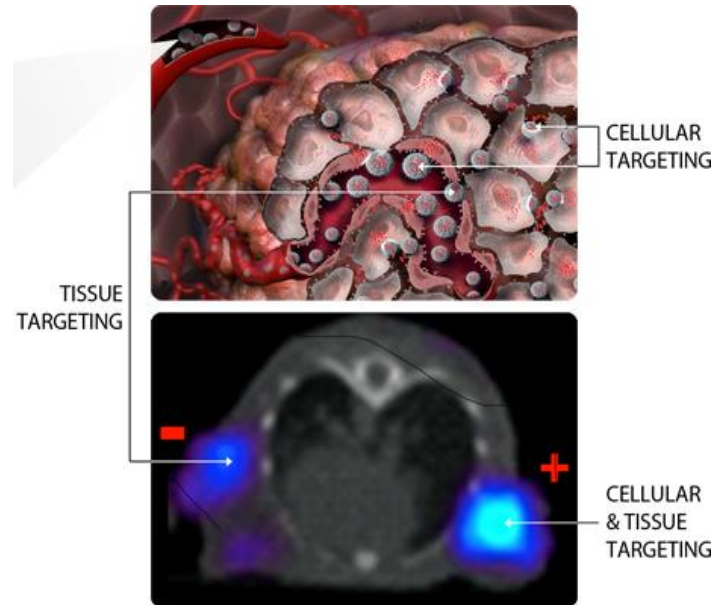
PSMA is not found in normal vasculature

Third generation

prostate specific membrane antigen (PSMA) targeting



SPECT imaging of ^{111}In -labeled PSMA-targeted nanoparticles in PSMA-positive and negative prostate tumor xenografts



Early tests in animals and small clinical trials showed that the approach was safer than docetaxel alone

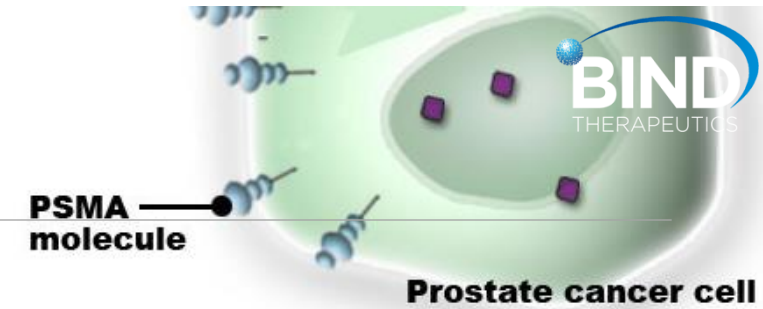


Later clinical trials disappointed

- BIND-014 failed against cervical and head-and-neck cancers
- Efficacy on lung cancer was not clear

Third generation

prostate specific membrane antigen (PSMA) targeting



Last updates February-April 2016

5 studies found for: BIND-014
[Modify this search](#) | [How to Use Search Results](#)

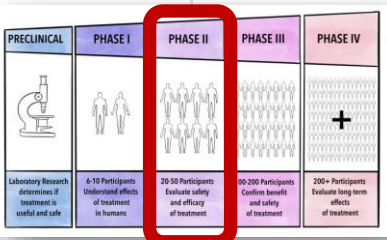
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Include only open studies Exclude studies with Unknown status

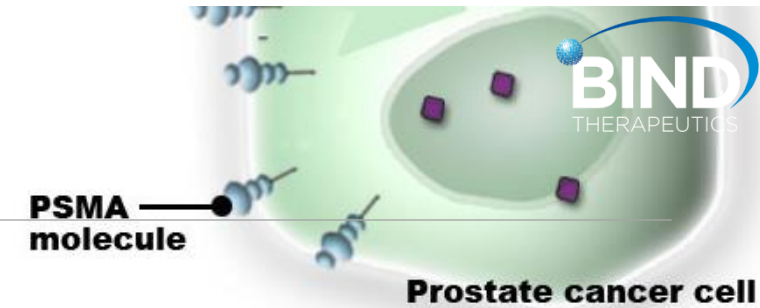
| Rank | Status | Study |
|------|------------|--|
| 1 | Completed | A Phase 2 Study to Determine the Safety and Efficacy of BIND-014 (Docetaxel Nanoparticles for Injectable Suspension), Administered to Patients With Metastatic Castration-Resistant Prostate Cancer Conditions: CRPC; Prostate Cancer Intervention: Drug: BIND-014 |
| 2 | Completed | A Study of BIND-014 Given to Patients With Advanced or Metastatic Cancer Conditions: Metastatic Cancer; Cancer; Solid Tumors Intervention: Drug: BIND-014 |
| 3 | Completed | A Phase 2 Study to Determine the Safety and Efficacy of BIND-014 (Docetaxel Nanoparticles for Injectable Suspension) as Second-line Therapy to Patients With Non-Small Cell Lung Cancer Condition: Non-small Cell Lung Cancer Intervention: Drug: BIND-014 |
| 4 | Completed | A Study of BIND-014 (Docetaxel Nanoparticles for Injectable Suspension) as Second-line Therapy for Patients With KRAS Positive or Squamous Cell Non-Small Cell Lung Cancer Conditions: KRAS Positive Patients With Non-small Cell Lung Cancer; Squamous Cell Non-small Cell Lung Cancer Intervention: Drug: BIND-014 (Docetaxel Nanoparticles for Injectable Suspension) |
| 5 | Terminated | A Study of BIND-014 in Patients With Urothelial Carcinoma, Cholangiocarcinoma, Cervical Cancer and Squamous Cell Carcinoma of the Head and Neck Conditions: Urothelial Carcinoma; Cholangiocarcinoma; Cervical Cancer; Squamous Cell Carcinoma of Head and Neck Intervention: Drug: BIND-014 (docetaxel nanoparticles for injectable suspension) |

[^ TO TOP](#)



Third generation

prostate specific membrane antigen (PSMA) targeting



Last updates February-April 2016

5 studies found for: BIND-014
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Include only open studies Exclude studies with Unknown status

| Rank | Status | Study |
|------|------------|---|
| 1 | Completed | <p>A Phase 2 Study to Determine the Safety and Efficacy of BIND-014 (Docetaxel Nanoparticles for Injectable Suspension), Administered to Patients With Metastatic Castration-Resistant Prostate Cancer</p> <p>Conditions: CRPC; Prostate Cancer Intervention: Drug: BIND-014</p> |
| 2 | Completed | <p>A Study of BIND-014 Given to Patients With Advanced or Metastatic Cancer</p> <p>Conditions: Metastatic Cancer; Cancer; Solid Tumors Intervention: Drug: BIND-014</p> |
| 3 | Completed | <p>A Phase 2 Study to Determine the Safety and Efficacy of BIND-014 (Docetaxel Nanoparticles for Injectable Suspension) as Second-line Therapy to Patients With Non-Small Cell Lung Cancer</p> <p>Condition: Non-small Cell Lung Cancer Intervention: Drug: BIND-014</p> |
| 4 | Completed | <p>A Study of BIND-014 (Docetaxel Nanoparticles for Injectable Suspension) as Second-line Therapy for Patients With KRAS Positive or Squamous Cell Non-Small Cell Lung Cancer</p> <p>Conditions: KRAS Positive Patients With Non-small Cell Lung Cancer; Squamous Cell Non-small Cell Lung Cancer Intervention: Drug: BIND-014 (Docetaxel Nanoparticles for Injectable Suspension)</p> |
| 5 | Terminated | <p>A Study of BIND-014 in Patients With Urothelial Carcinoma, Cholangiocarcinoma, Cervical Cancer and Squamous Cell Carcinoma of the Head and Neck</p> <p>Conditions: Urothelial Carcinoma; Cholangiocarcinoma; Cervical Cancer; Squamous Cell Carcinoma of Head and Neck Intervention: Drug: BIND-014 (docetaxel nanoparticles for injectable suspension)</p> |

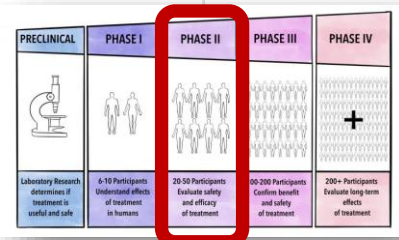
[^ TO TOP](#)

TROUBLED TIMES

BIND Therapeutics raised US\$70.5 million in an initial public offering of stock in September 2013. But the company's stock price has fallen in response to its recent financial woes.



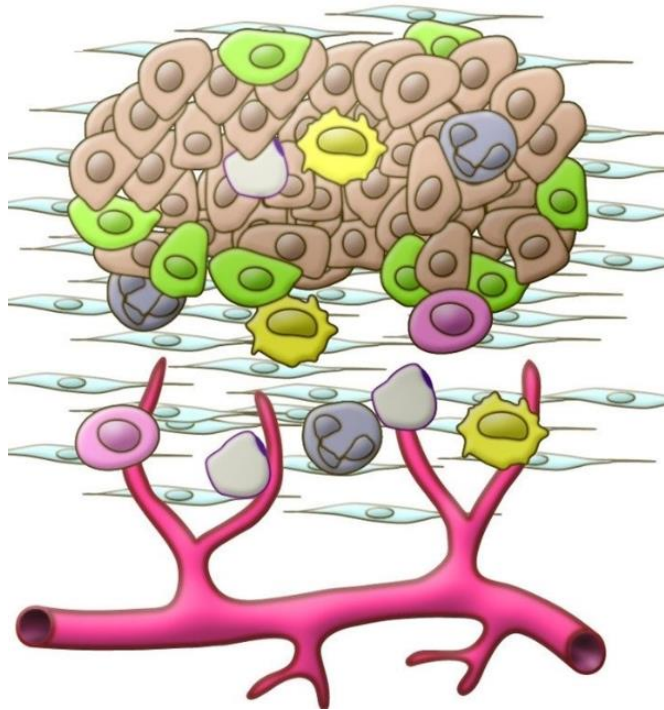
BANKRUPTCY



Need to reach the biological target

The abnormal microenvironment impairs uniform delivery and efficacy of therapeutic agents

Transport through the microenvironment



Extravasation

Efficient drug delivery to cancer cells requires crossing of multiple biological barriers

Need to have relevant predictive models

Fourth generation: stimuli responsive



Efficient spatio temporal and dosage release control



- Endogenous stimuli

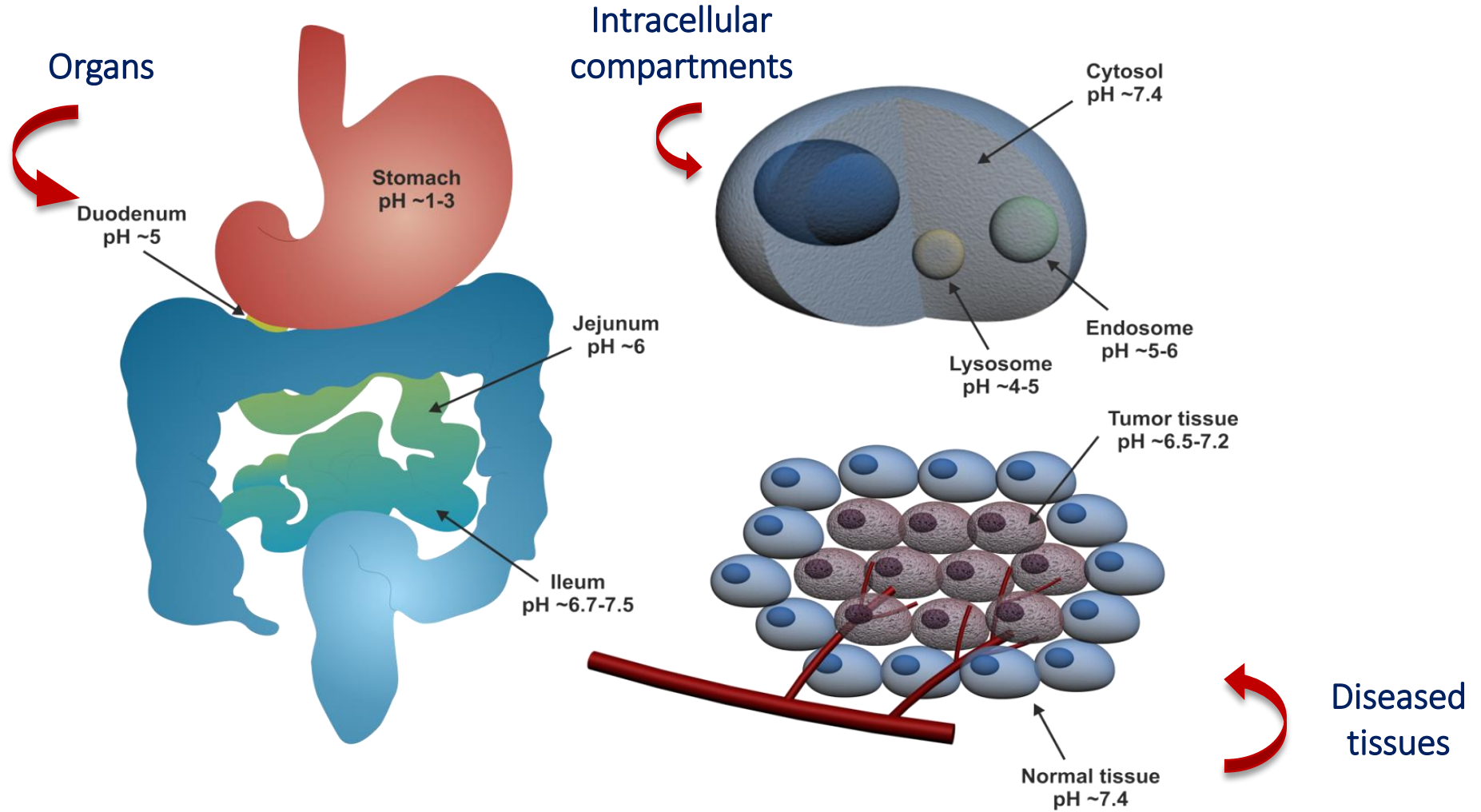
- pH
- Redox status (glutathion concentrations)
- Enzymatic activity

- Exogenous stimuli

- Magnetic/electric field
- Light
- Ultrasound
- Temperature

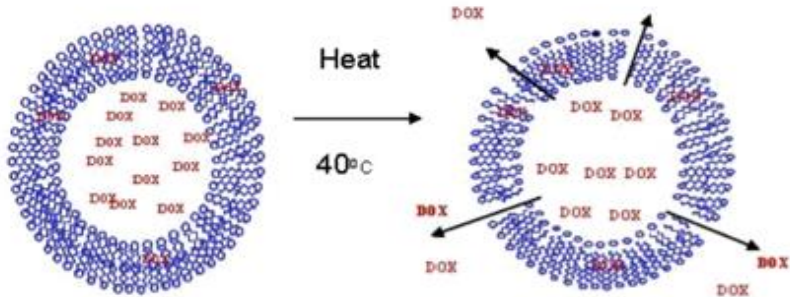
Fourth generation: pH sensitive

- Body pH variations

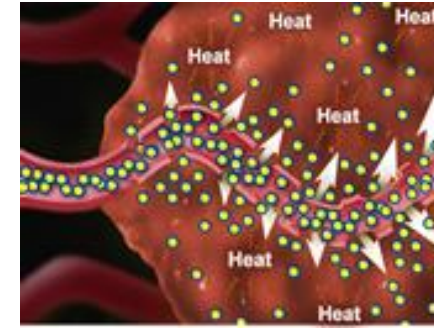


Fourth generation : temperature sensitive

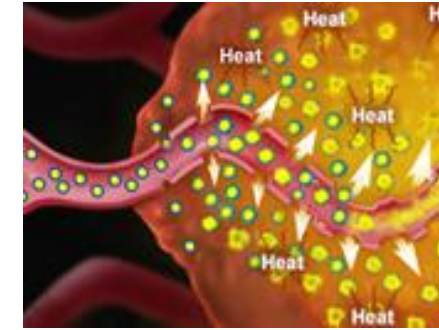
- Heat-activated doxorubicin loaded liposomes : ThermoDox[®]



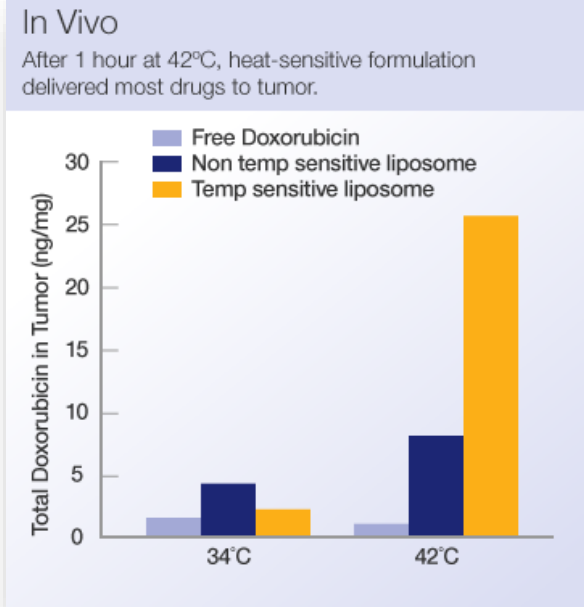
“Leaky” tumor blood Vessels



Heat adds permeability



Heat-triggered release

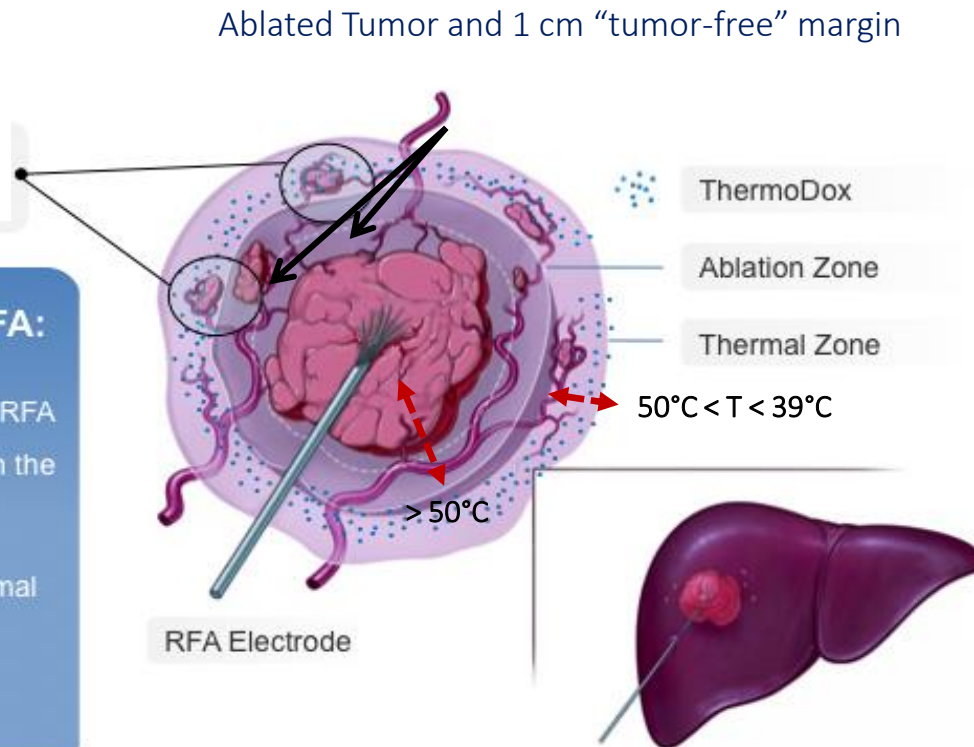


| INDICATION | PRODUCT/STUDY | PRECLINICAL | PHASE 1-2 | PHASE 3 |
|---------------|--------------------------------------|-------------|-----------|---------|
| Primary Liver | ThermoDox [®] /OPTIMA Study | Yes | Yes | Yes |
| Ovarian | GEN-1/OVATION Study | Yes | Yes | No |
| Glioblastoma | GEN-1 | Yes | Yes | No |
| Bladder | ThermoDox [®] | Yes | Yes | No |



Fourth generation: temperature sensitive

- Heat-activated doxorubicin loaded liposomes : ThermoDox[®]



ThermoDox + RFA:

- Infuse ThermoDox ~15 minutes prior to RFA
- Drug concentrates in the "Thermal Zone"
- Ablation releases doxorubicin in "Thermal Zone" expanding treatment area and destroying micro-metastases

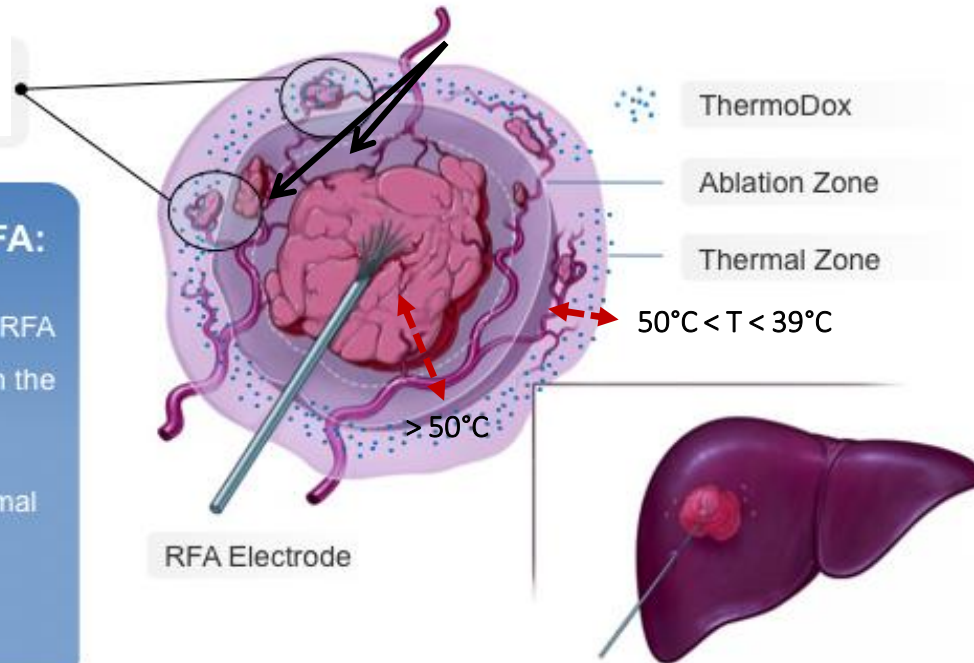


- Micro - metastasis outside the ablation zone "kill" area.
- Potential site of recurrence if not treated

Fourth generation: temperature sensitive

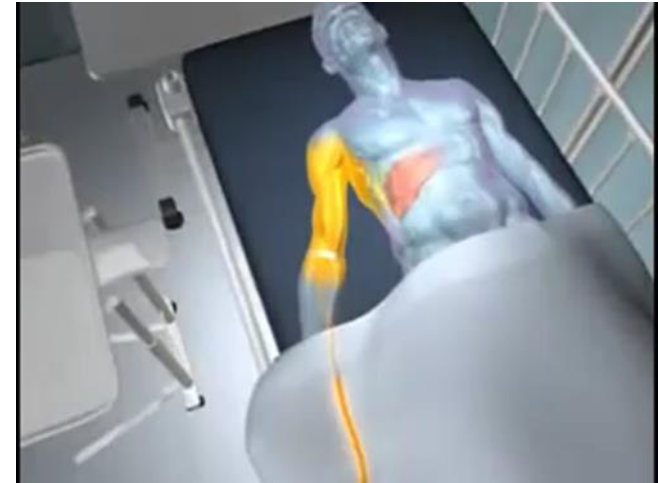
- Heat-activated doxorubicin loaded liposomes : ThermoDox[®]

Ablated Tumor and 1 cm "tumor-free" margin

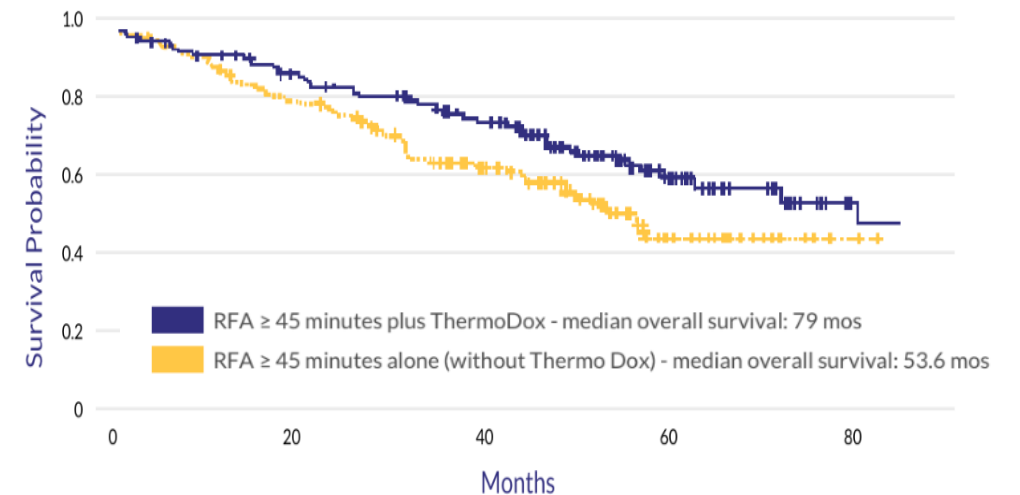


ThermoDox + RFA:

- Infuse ThermoDox ~15 minutes prior to RFA
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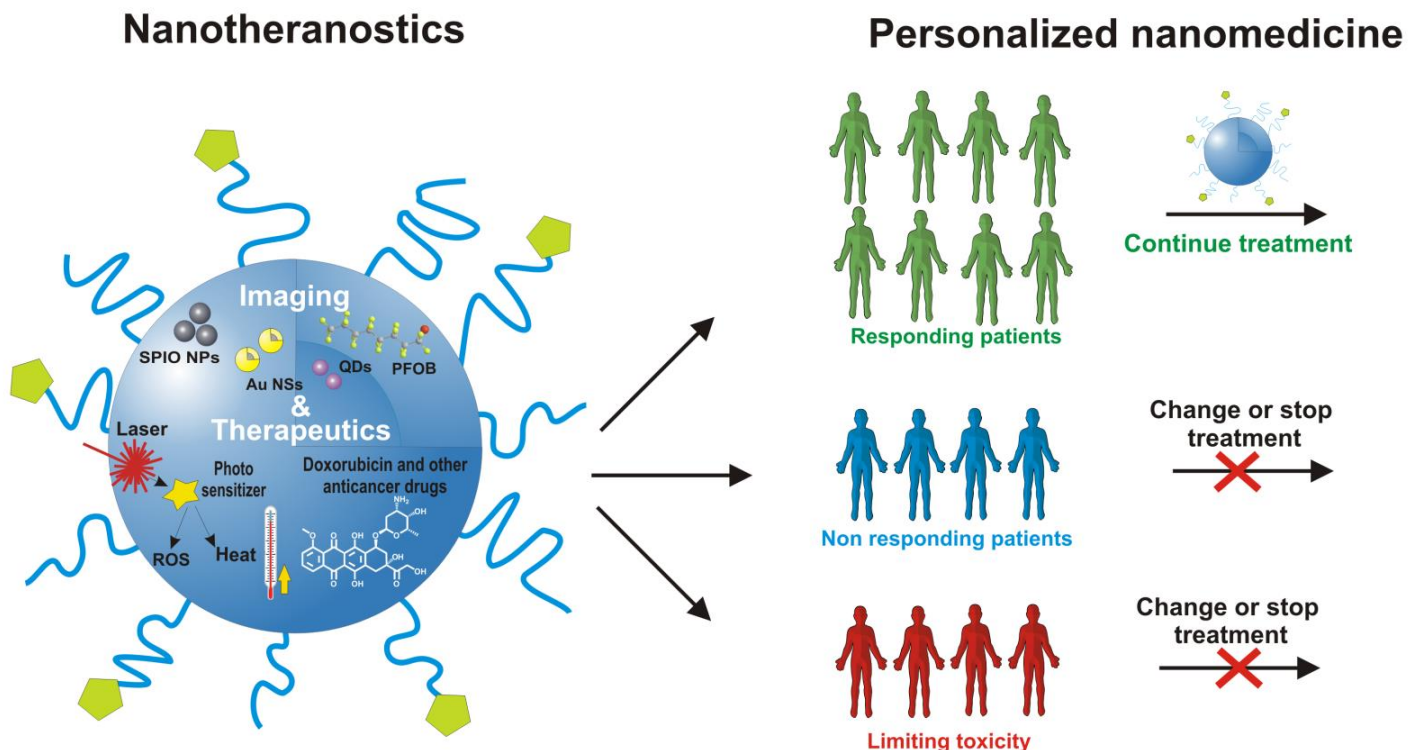


- Survival data for single-lesion patients



- Micro - metastasis outside the ablation zone "kill" area.
- Potential site of recurrence if not treated

• Moving to the personalized medicine



Combine targeted therapeutic & diagnostic functions

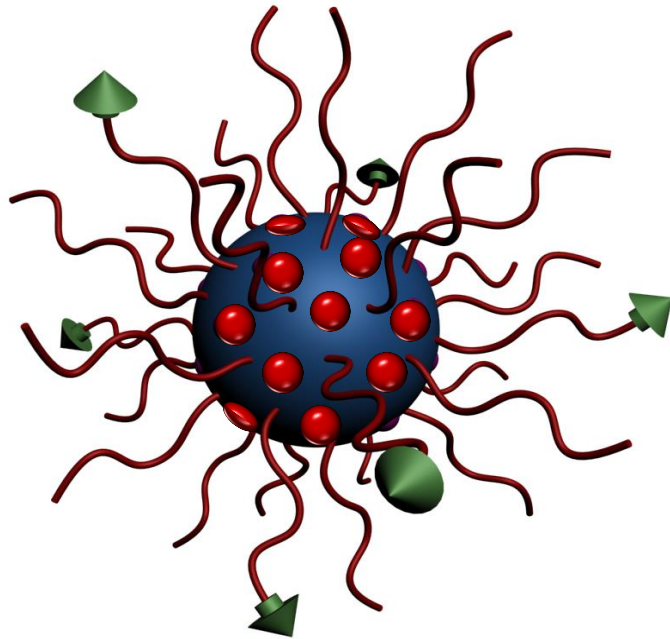
- Non invasive longitudinal monitoring
- Assessment of disease progression
- Evaluation of intervention efficacy at an early stage



Optimized and individualized treatment protocols

Nanomedicine for drug delivery

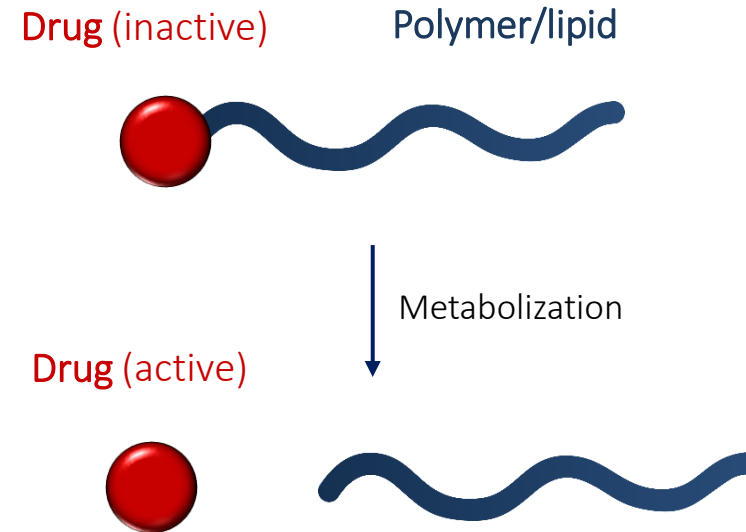
Physical drug encapsulation



Important limitations:

- Poor drug loading (< 5%)
- Burst release of surface adsorbed drug

The prodrug strategy

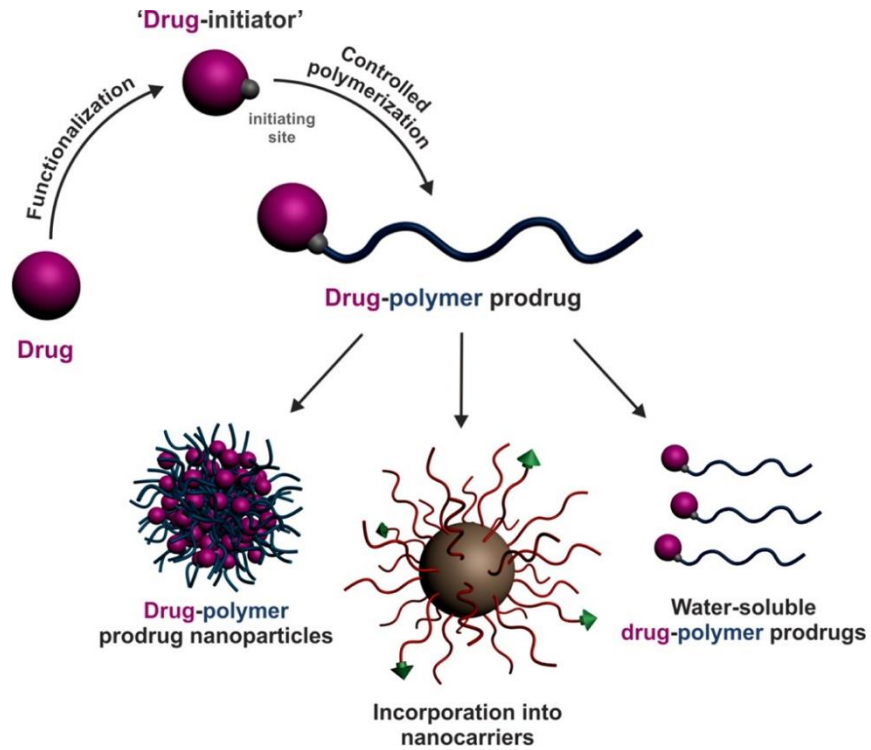


Advantages:

- Sustained drug release
- Increase of the drug chemical stability
- Reduced toxicity before metabolization occurs

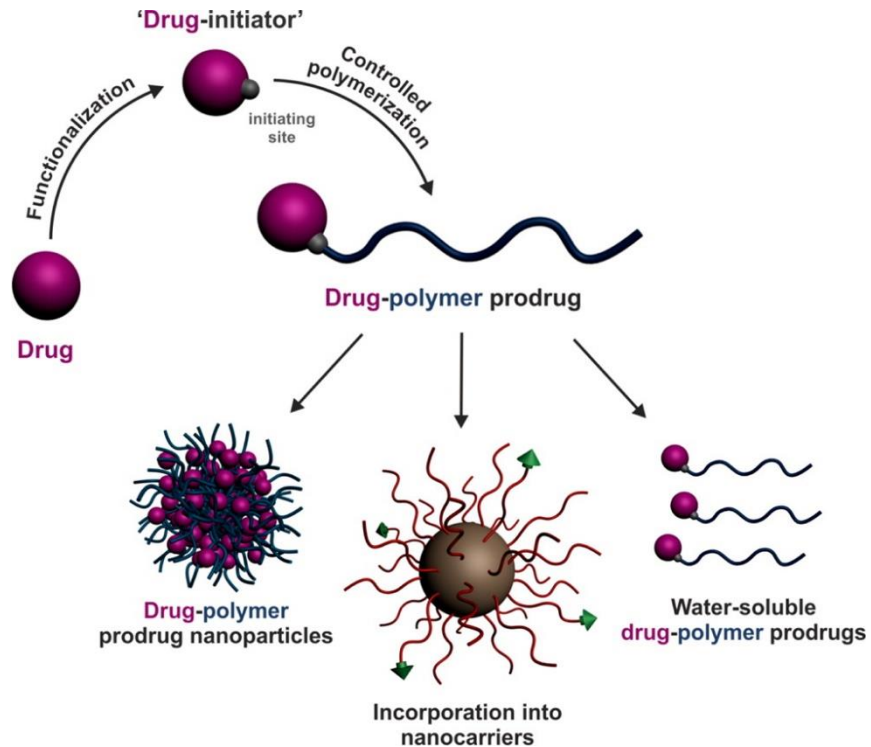
The prodrug approach

- Polymer prodrugs



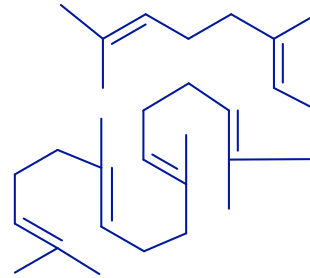
The prodrug approach

- Polymer prodrugs



- Lipid Prodrugs

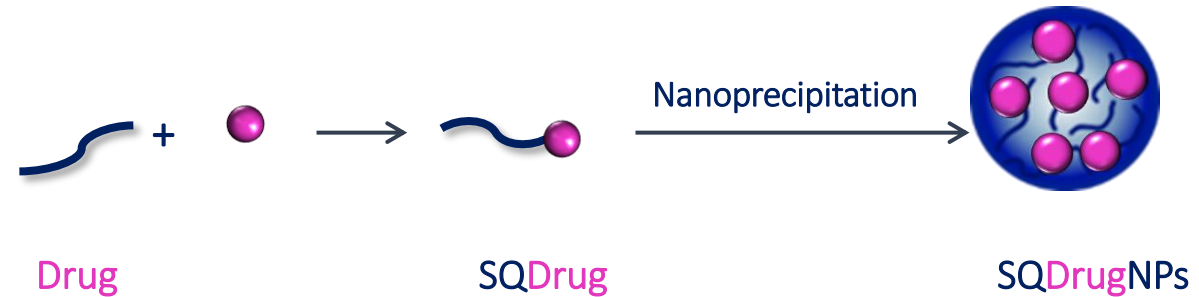
Squalene (SQ)



- Acyclic triterpene widely distributed in nature
- Intermediate in the cholesterol biosynthetic pathway
- Dynamically folded conformation in aqueous solution

The squalenoylation approach

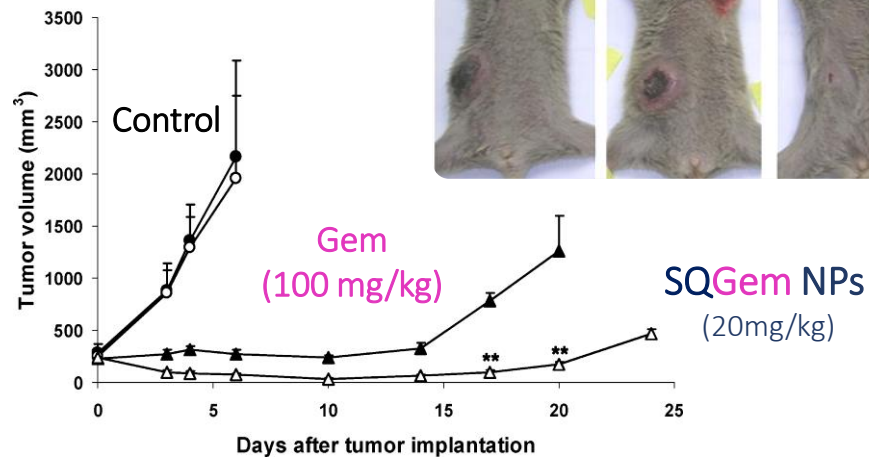
chemical conjugation of squalene to a biologically active drug molecule leading to bioconjugates which self-assemble as nanoparticles in water



The prodrug approach: squalene based

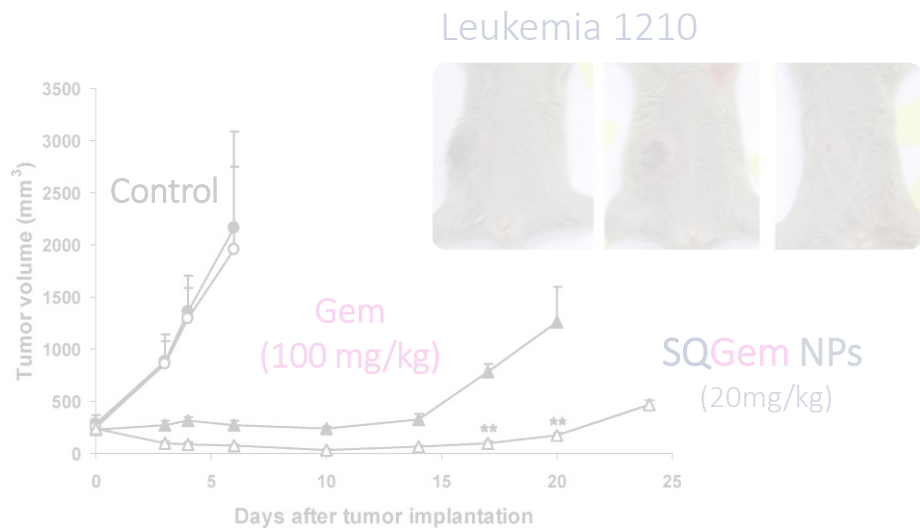
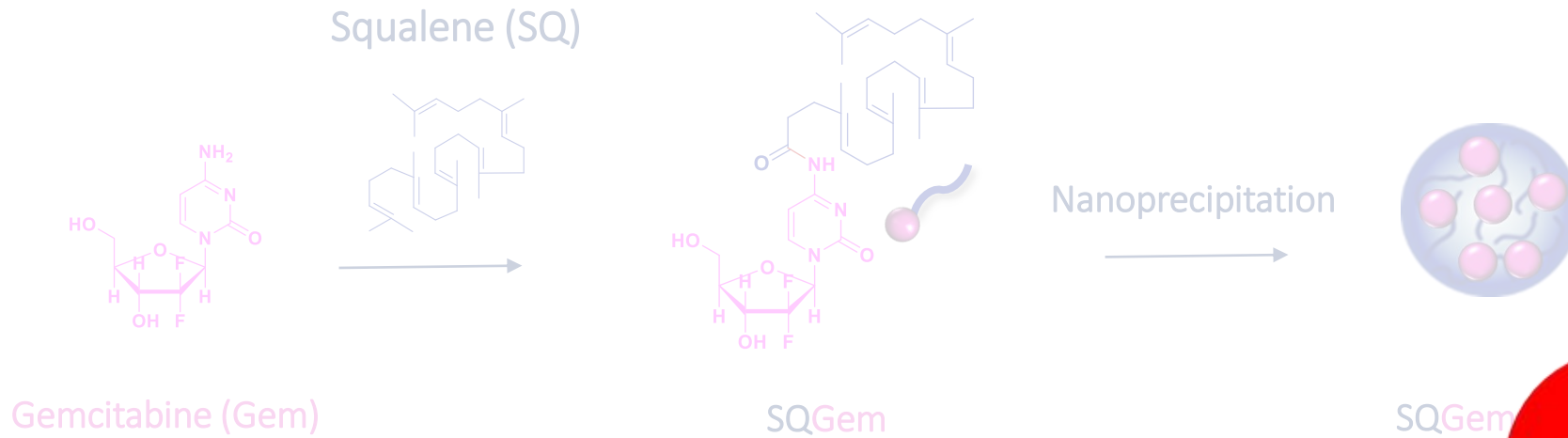


Leukemia 1210



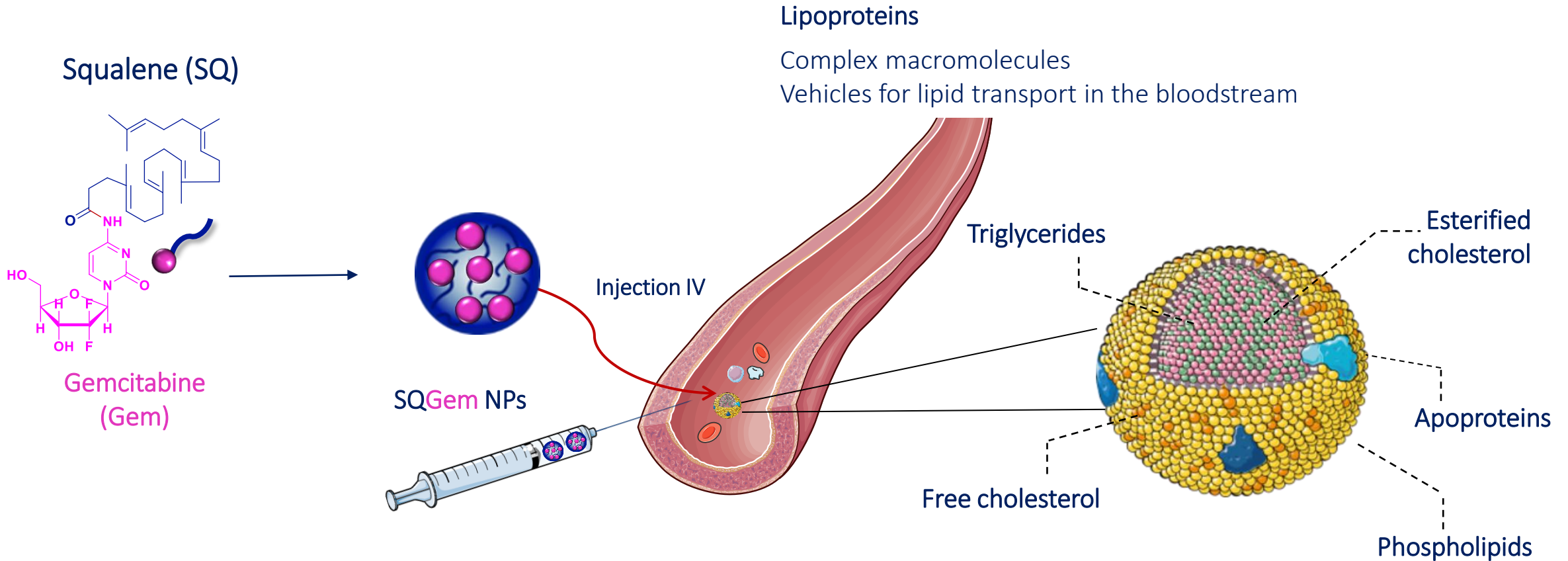
- ↑ $t_{1/2}$ (1.6 h vs. 8.6 h)
- ↑ drug loading
- Overcome resistance phenomena
- ↑ anticancer activity

The prodrug approach: squalene based



- ↑ $t_{1/2}$ (1.6 h vs 0.6 h)
- ↑ drug loading
- No surface functionalization**
- Overcome resistance phenomena
- ↑ anticancer activity

In vivo fate of lipid prodrug-based nanoparticles (NPs)



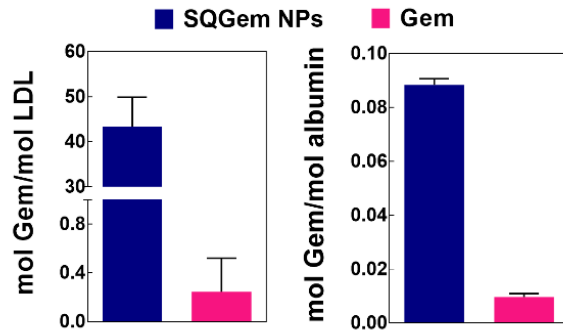
Cholesterol: transported in circulation by lipoproteins

Squalene: precursor in the cholesterol biosynthesis

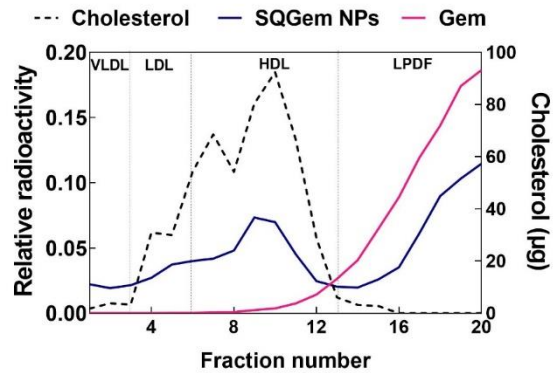
Behaviour analogy?

Lipoproteins as indirect drug carriers

- *In vitro* & *in vivo* studies



500 times higher affinity of SQGem for LDL compared to albumin

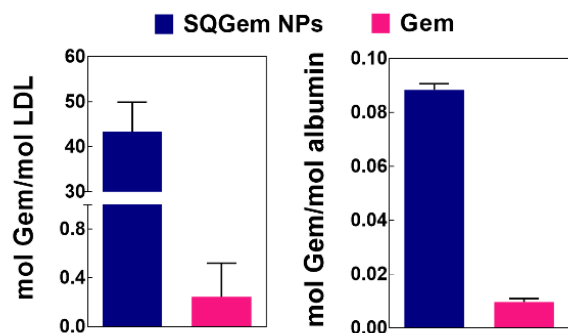


Preferential association with lipoproteins

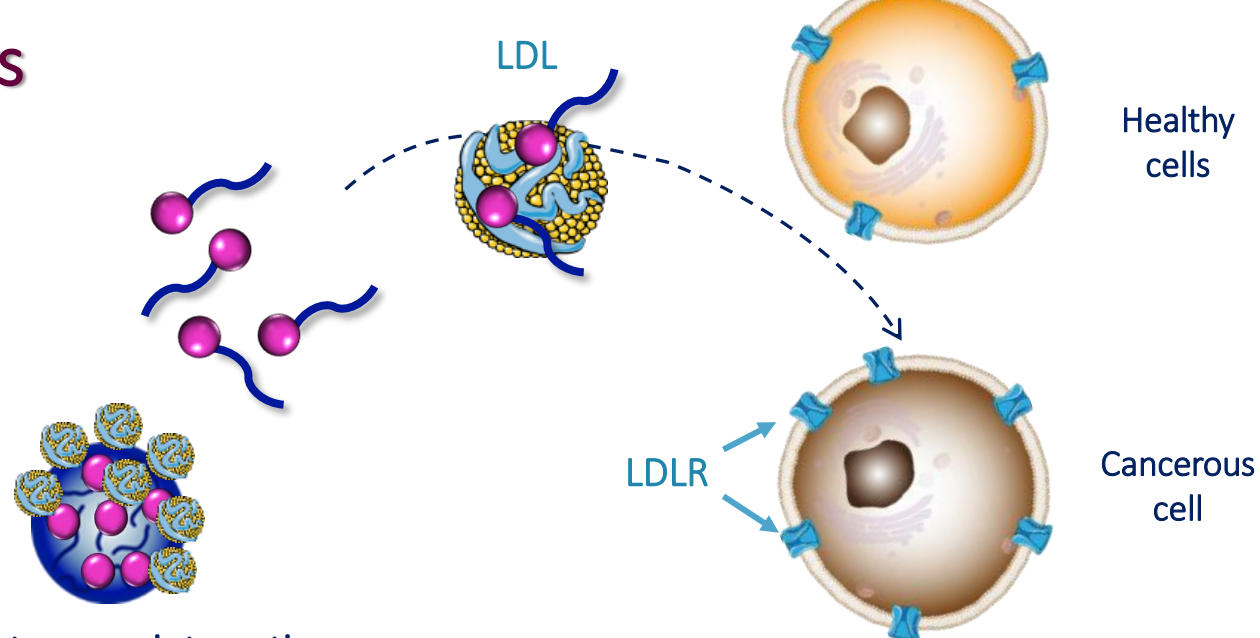
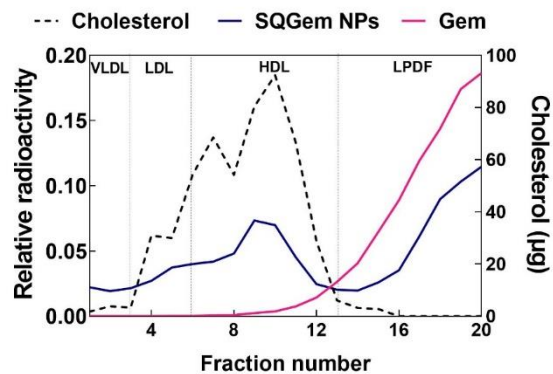
Interaction with the main cholesterol transporters in the circulation

Lipoproteins as indirect drug carriers

In vitro & *in vivo* studies



500 times higher affinity of SQGem for LDL compared to albumin



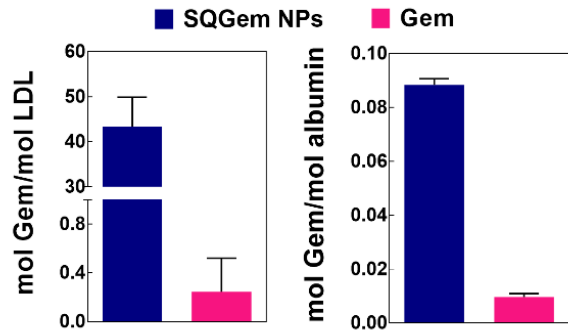
Spontaneous interaction
NP disassembly

Preferential association with lipoproteins

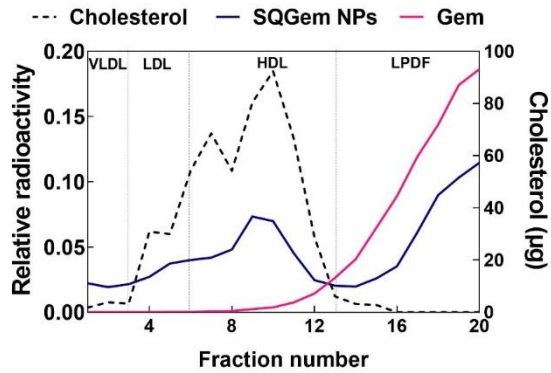
Interaction with the main cholesterol transporters in the circulation

Lipoproteins as indirect drug carriers

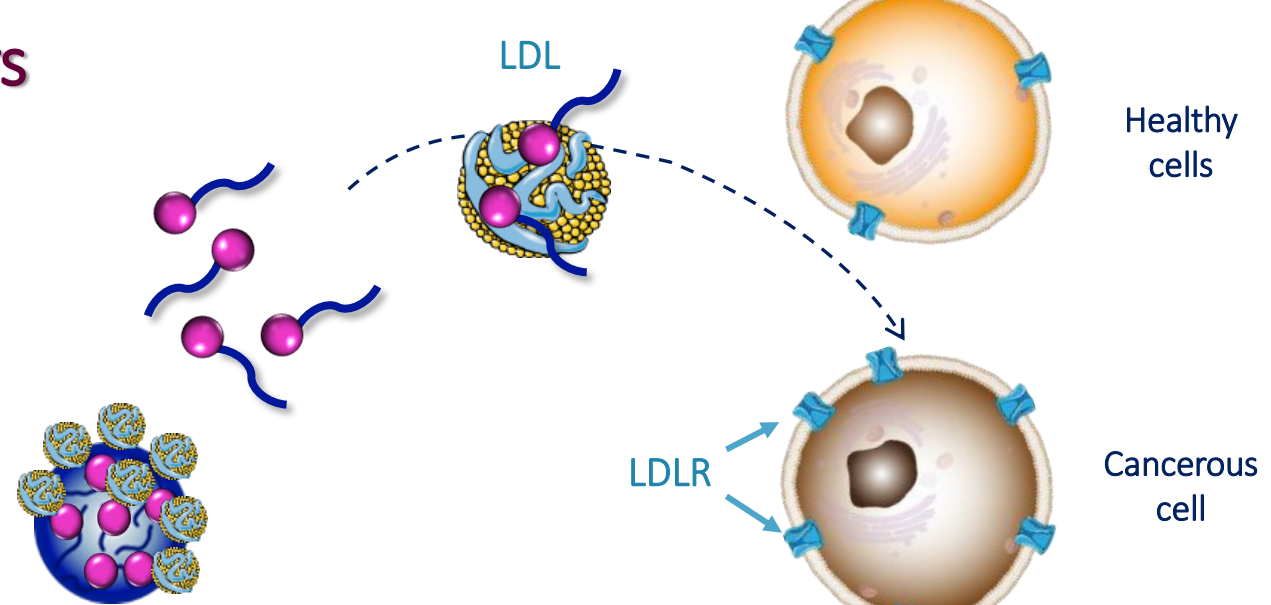
In vitro & in vivo studies



500 times higher affinity of SQGem for LDL compared to albumin



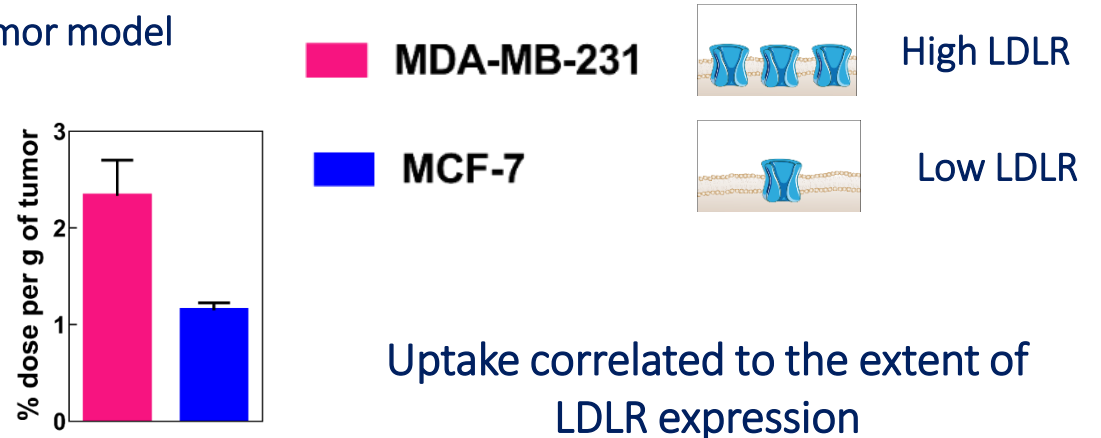
Preferential association with lipoproteins
Interaction with the main cholesterol transporters in the circulation



Spontaneous interaction
NP disassembly

Radioactivity quantification

In vivo tumor model



Uptake correlated to the extent of LDLR expression

Lipoproteins as direct drug carriers

- Current loading strategies
 - Incorporation of drugs into endogenous isolated particle

Complex LDL isolation

Potential contamination

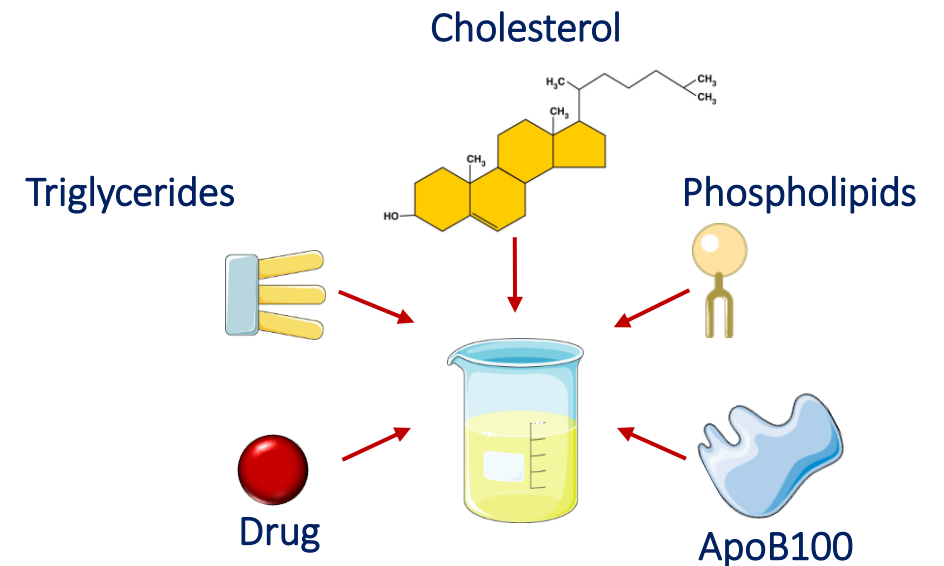
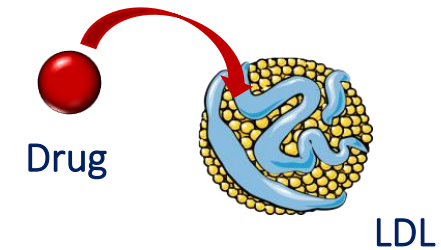
Storage concerns (aggregation/degradation)

- Design of drug loaded synthetic lipoprotein-like systems

Batch reproducibility

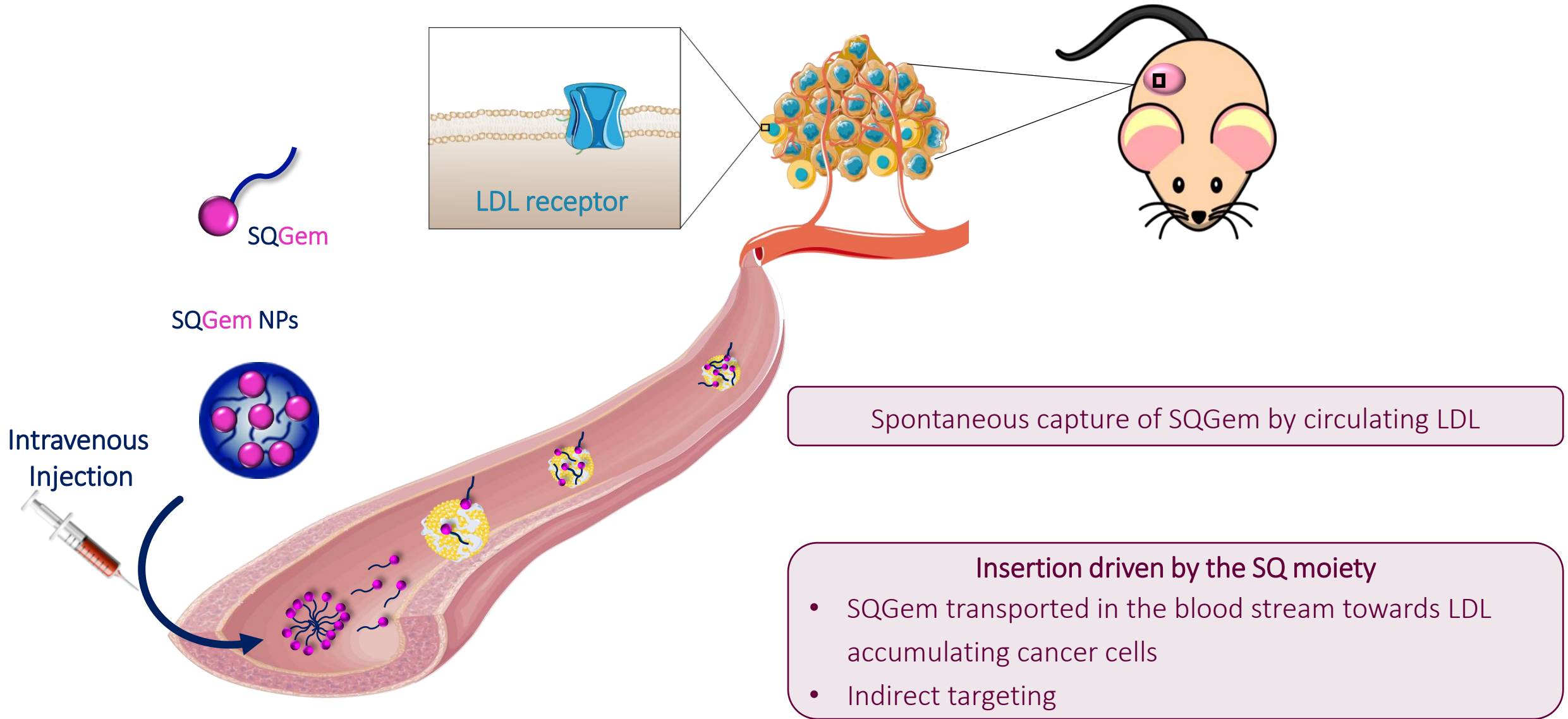
Costs of large-scale production

Synthetic carriers



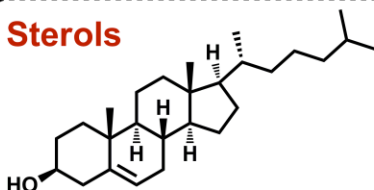
Too many drawbacks: no industrial development

Lipoproteins as indirect drug carriers



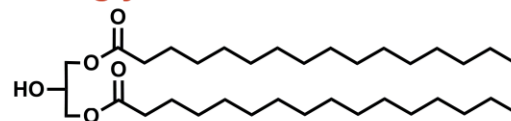
Other lipid prodrugs

Sterols



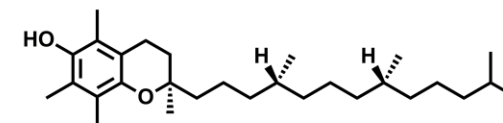
Cholesterol (Chol)

Diglycerides



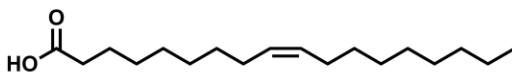
Glycerol 1,3-dipalmitate (Digly)

Fat-Soluble vitamins

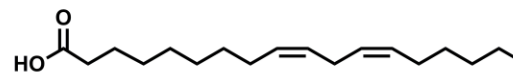


Alpha-tocopherol (VitE)

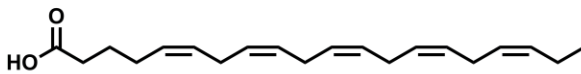
Unsaturated fatty acids



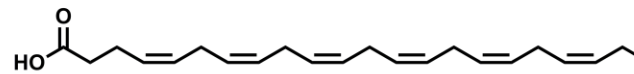
Oleic acid (OA)



Linoleic acid (LA)

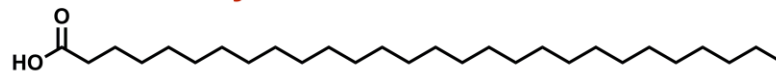


Eicosapentaenoic acid (EPA)



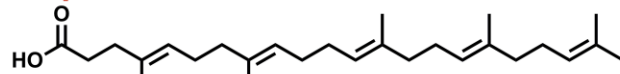
Docosahexaenoic acid (DHA)

Saturated fatty acids

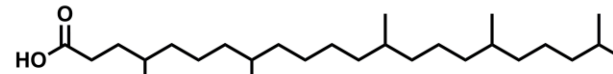


Octacosanoic acid (C28)

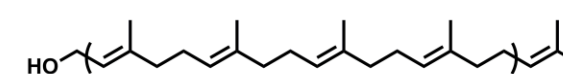
Terpenes and derivatives



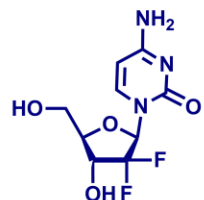
Squalene (SQ)



Saturated Squalenic acid (RSQ)

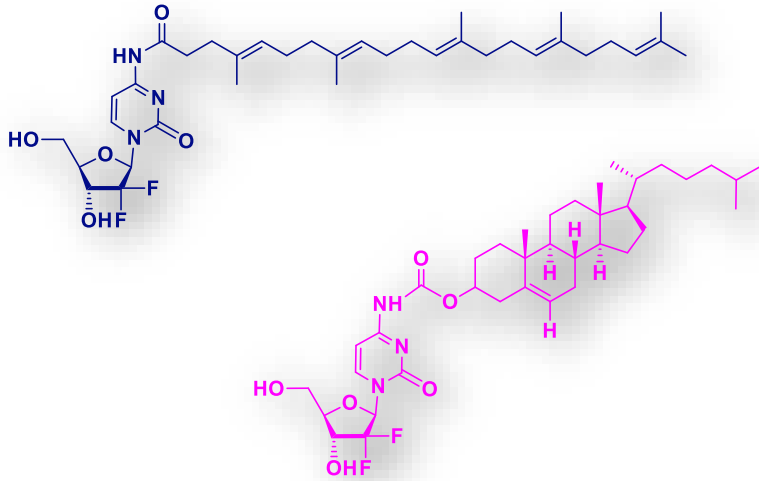


Solanesol (Sol)



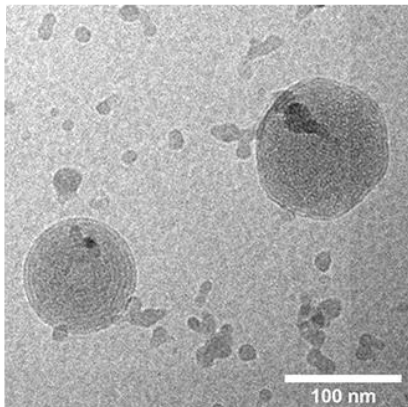
Gemcitabine

Lipid prodrugs: Cholesterol Gemcitabine

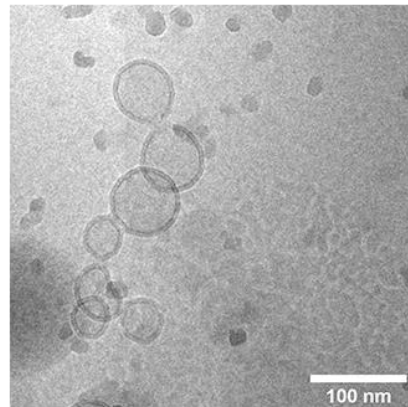


| Conjugate | Mean diameter (nm) | Polydispersity index (Pdl) | Zeta Potential (mV) | Drug loading (%) |
|-----------|--------------------|----------------------------|---------------------|------------------|
| SQGem | 82 ± 7 | 0.11 ± 0.03 | -20 ± 7 | 40.7 |
| CholGem | 97 ± 15 | 0.09 ± 0.02 | -21 ± 7 | 38.9 |

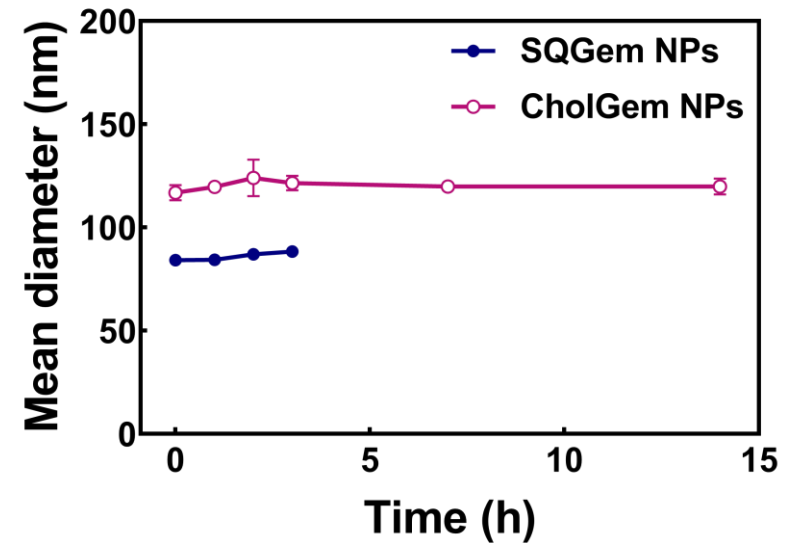
- Stability over time (RT, mQ)



SQGem NPs

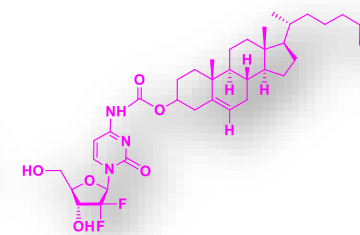
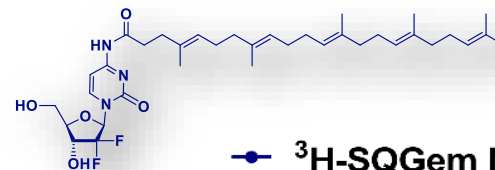


CholGem NPs

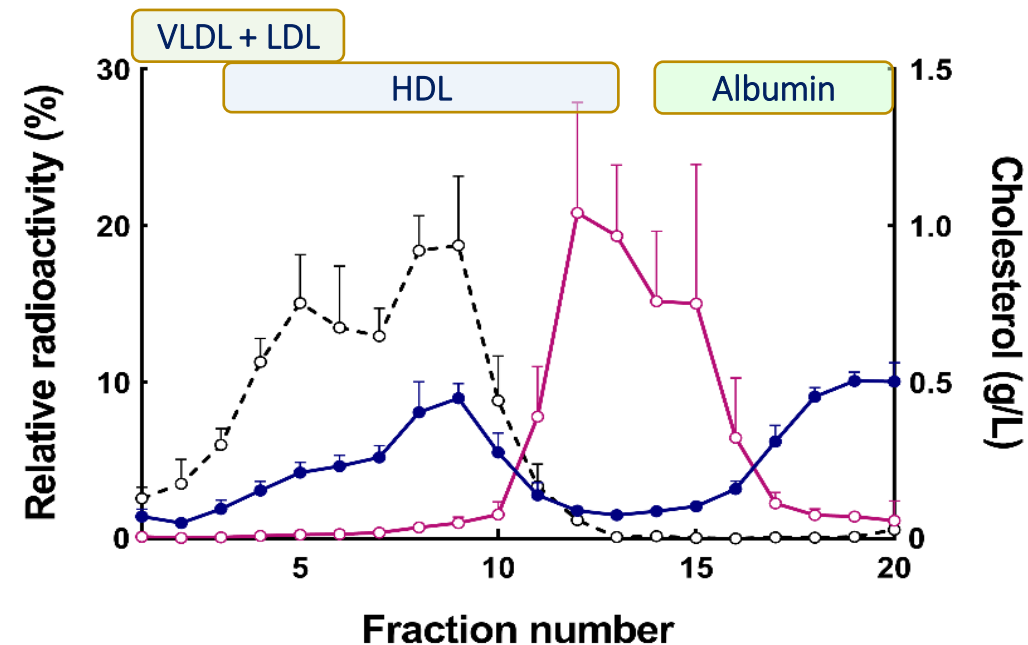
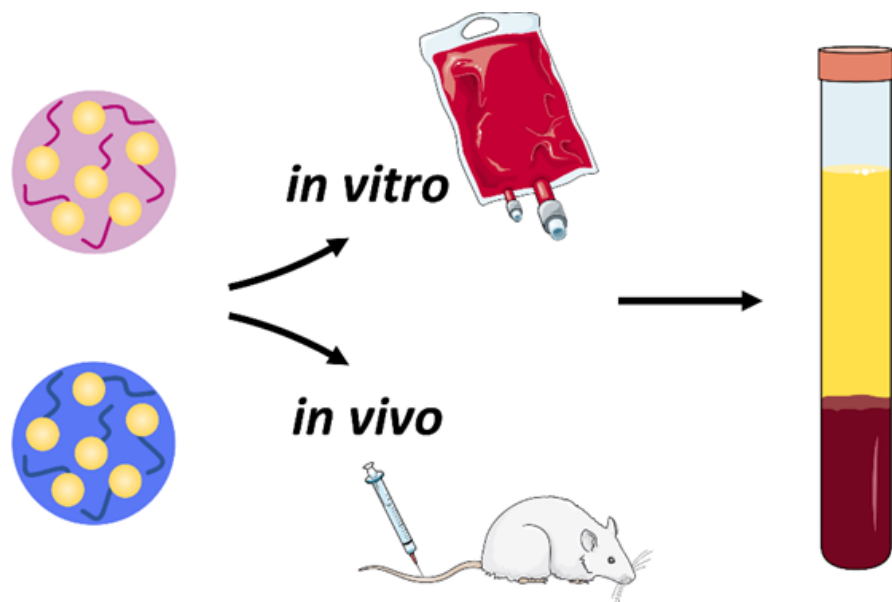


Lipid prodrugs: Cholesterol Gemcitabine

- Plasma distribution



● ³H-SQGem NPs ● ³H-CholGem NPs ○ Cholesterol

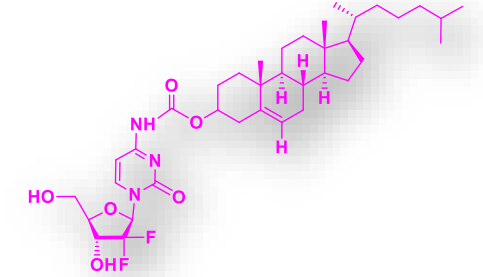
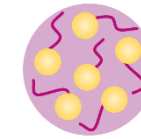
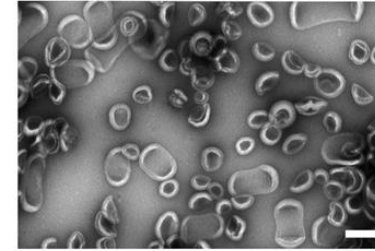
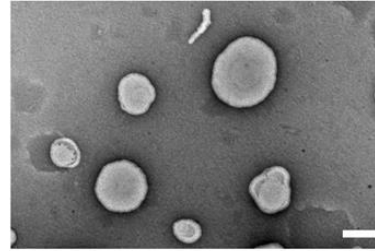
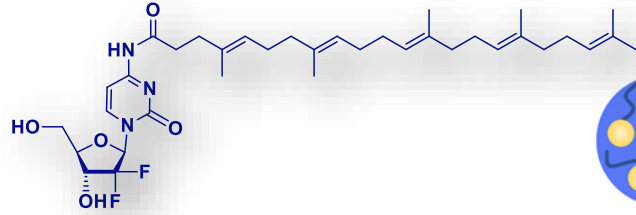


SQGem follows endogenous cholesterol profile and albumin

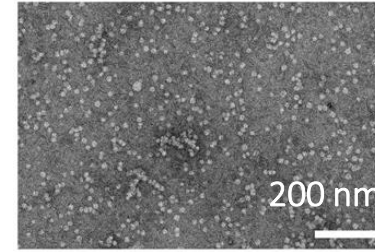
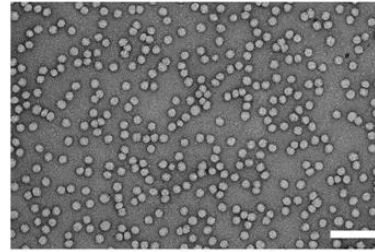
CholGem found in albumin and LP-deficient fractions

Lipid prodrugs: Cholesterol Gemcitabine

- Physical mixtures : 5' @ 37° C



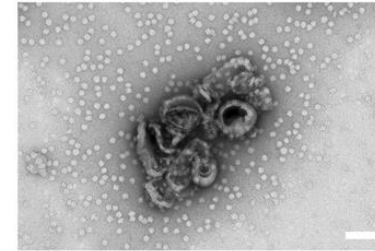
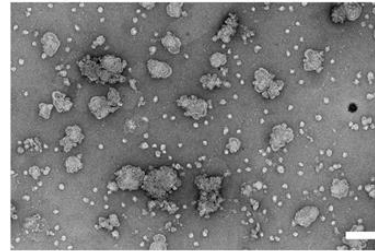
LDL



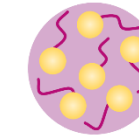
HDL



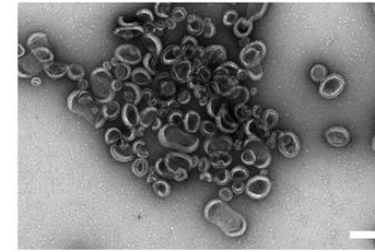
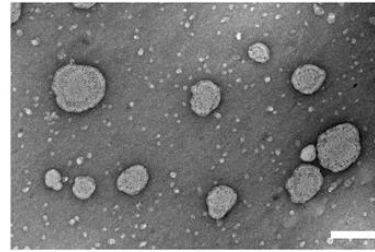
LDL



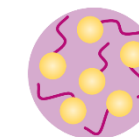
LDL



HDL



HDL

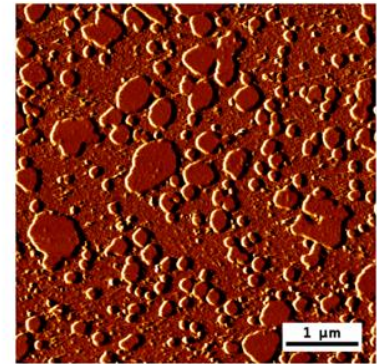
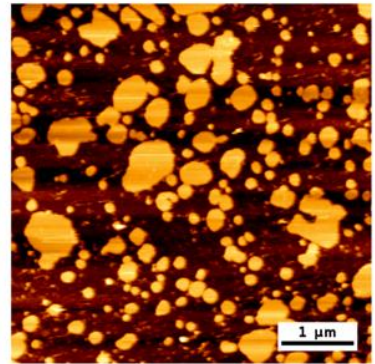
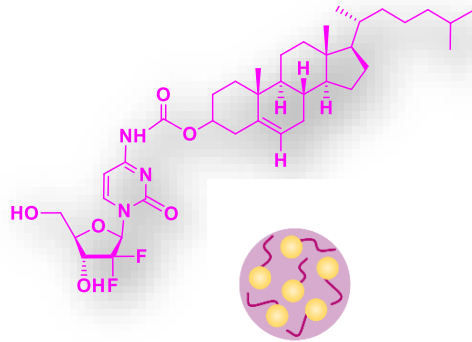
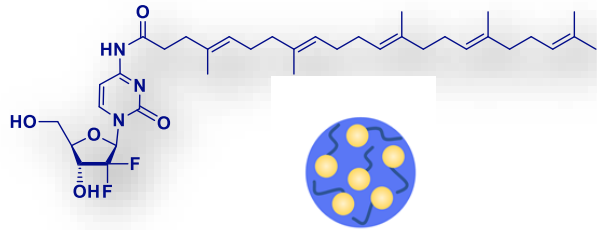


Merging of NPs & LPs

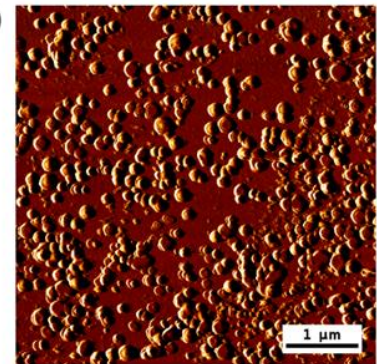
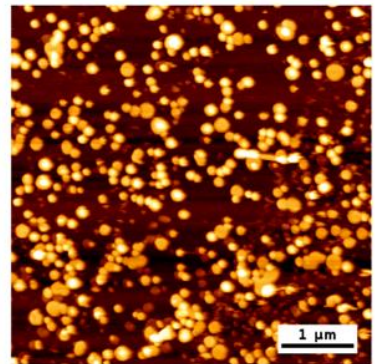
Simple co-existence

Lipid prodrugs: Cholesterol Gemcitabine

- AFM analysis: lysine-coated MICA surface



Patch formation and spreading



Flattening but no breaking

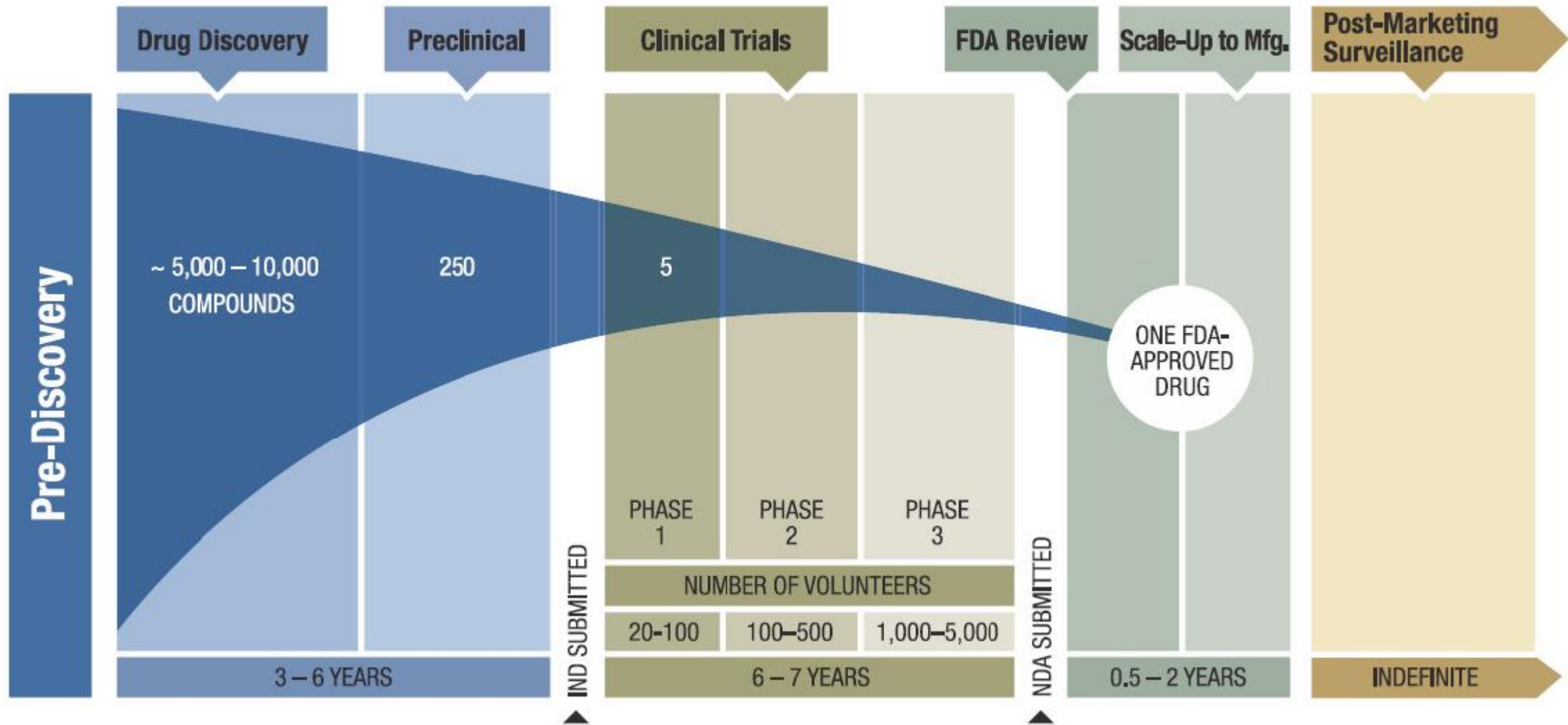
The physico-chemical properties of the NPs strongly influence the fate in the bloodstream

Nanoscale drug delivery systems

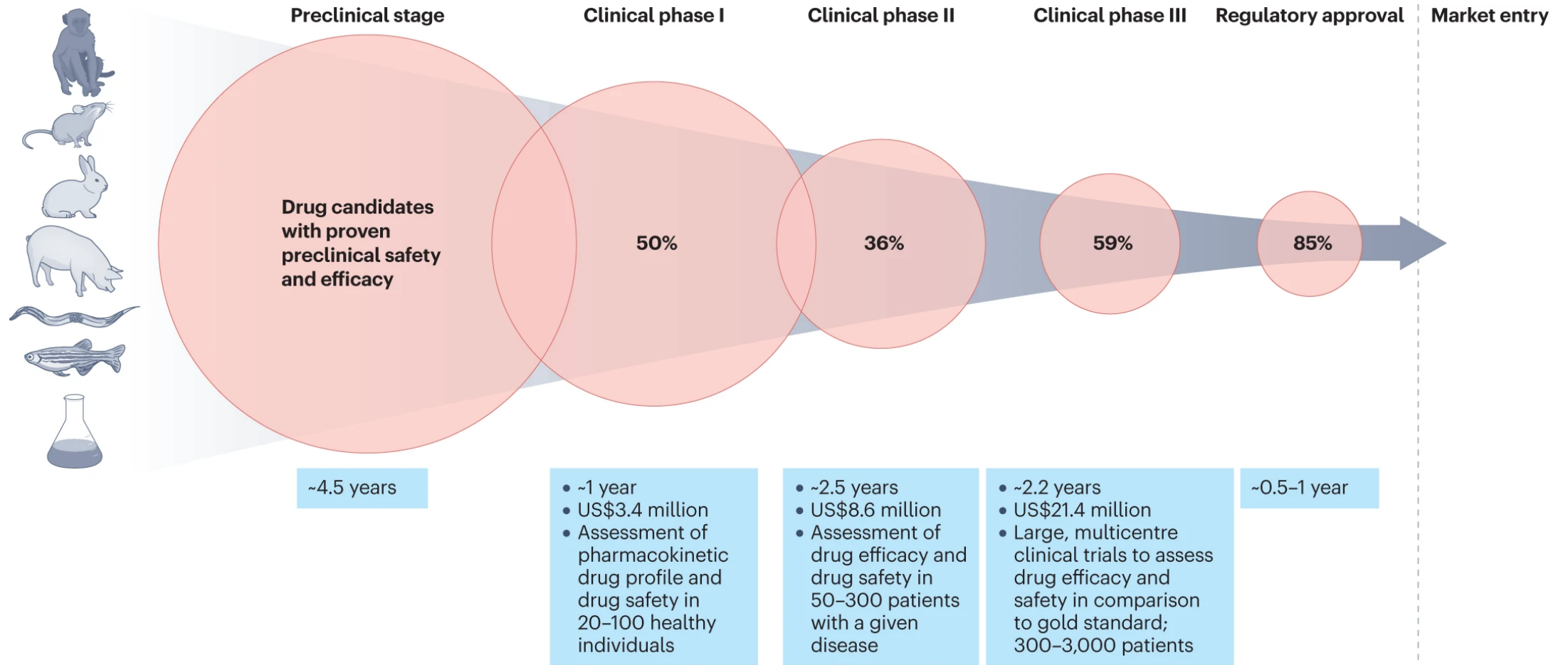
From the bench to the bedside

Need of a relevant preclinical evaluation (UE 3)

Drug development timeline



Drug development timeline

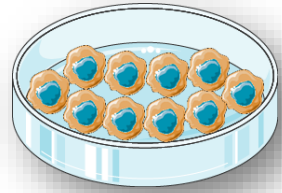


Physiologically relevant models

- Patients



2D



Easy and convenient set-up



Highly reductionist



Flat cells, simple geometry



Lack of architecture



Less realistic drug response



- *In vivo* studies



Very useful



Expensive, time consuming



Specie differences

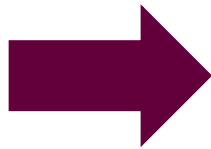


Ethical issues

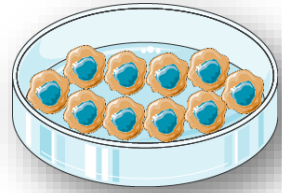


Physiologically relevant models

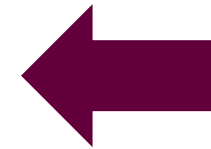
- Patients



2D



- Easy and convenient set-up
- Highly reductionist
- Flat cells, simple geometry
- Lack of architecture
- Less realistic drug response



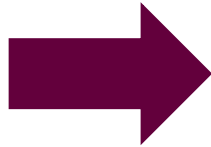
- *In vivo* studies

- Very useful
- Expensive, time consuming
- Specie differences
- Ethical issues

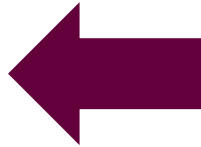


Physiologically relevant models

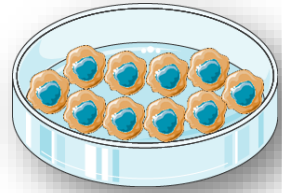
- Patients



- Cell-to-cell, cell-to-matrix interaction
- Oxygen, nutrient and waste gradient
- Recreation of the microenvironment
- Vascularization



2D



- Easy and convenient set-up +
- Highly reductionist -
- Flat cells, simple geometry -
- Lack of architecture -
- Less realistic drug response -

- *In vivo* studies



- Very useful +
- Expensive, time consuming -
- Specie differences -
- Ethical issues -

FDA Modernization Act 2.0

...make use of “certain alternatives to animal testing, including cell-based assays and computer models, to obtain an exemption from the Food and Drug Administration to investigate the safety and effectiveness of a drug”...

“removes a requirement to use animal studies as part of the process to obtain a license for a biological product that is biosimilar or interchangeable with another biological product”



ANIMAL RESEARCH

FDA no longer has to require animal testing for new drugs

Agency can rely on animal-free alternatives before human trials

By Meredith Wadman

New medicines need not be tested in animals to receive U.S. Food and Drug Administration (FDA) approval, according to legislation signed by President Joe Biden in late December 2022. The change—long sought by animal welfare organizations—could signal a major shift away from animal use after more than 80 years of drug safety regulation.

“This is huge,” says Tamara Drake, director of research and regulatory policy at the Center for a Humane Economy, a nonprofit animal welfare organization and key driver of the legislation. “It’s a win for industry. It’s a win for patients in need of cures.”

In place of the 1938 stipulation that potential drugs be tested for safety and efficacy in animals, the law allows FDA to promote a drug or biologic—a larger molecule such as an antibody—to human trials after either animal or nonanimal tests. Drake’s group and the nonprofit Animal Wellness Action, among others that pushed for changes, argue that in clearing drugs for human trials the agency should rely more heavily on computer modeling, “organ chips,” and other nonanimal methods that have been developed over the past 10 to 15 years.

But pro-research groups are downplaying the law, saying it signals a slow turning of the tide—not a tsunami that will remake the drug approval process overnight. Jim Newman, communications director at Americans for Medical Progress, which advocates for animal research, argues non-animal technologies are still “in their infancy” and won’t be able to replace animal models for “many, many years.” FDA still retains tremendous discretion to require animal tests, he notes, and he doesn’t expect the agency to change tack anytime soon.

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FDA Modernization Act 2.0



Five alternatives to animal testing

Researchers are rapidly developing non-animal alternatives that promise more accurate and cost-effective approaches to the discovery process. "I think what's going to happen is that as the field becomes more and more comfortable, confident, and experienced with using these newer methods, eventually they will completely replace the use of animals," says **Aysha Akhtar, M.D., M.P.H.**, co-founder and CEO of the Center for Contemporary Sciences, a non-profit that is working to advance research and testing approaches that are rooted in human biology.

Organoids

Organoids are cultures of stem cells capable of differentiating and spontaneously self-organizing into small 3D structures that mimic, to an extent, organs. Heart, lung, and other organoids offer screening platforms for drugs, as well as mechanistic insights.



Researchers at the Center for Alternatives to Animal Testing at the Johns Hopkins Bloomberg School of Public Health have created brain organoids for studying neurodegenerative disease, electrophysiology, and even intelligence.

Human tissue

Studies on tissue derived from volunteers and surgical procedures offer opportunities to evaluate therapeutic interventions on accurate models of the disease. For example, researchers studying vitiligo, an autoimmune skin disorder, can directly assess how a potential intervention impacts autoimmune processes in skin tissue derived from people with vitiligo. Such experiments generate data that promote a level of precision medicine unattainable using animal models.



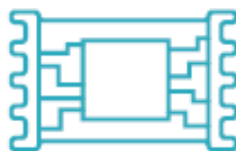
Phase 0 clinical trials

In Phase 0 trials, study participants are given sub-therapeutic levels of an investigational drug, followed by tests to identify changes in physiology. Despite the low dosage, data concerning potential toxicity and efficacy may be derived.



Organ-on-a-chip

These microfluidic devices contain tiny channels lined with living cells and are designed to reflect the architecture and physiology of an organ. This involves capturing the basic elements required for biological activity, including various cell types, structures, and microenvironments, and recreating them in a matrix. By stringing organ-on-a-chips together in a biologically relevant



fashion, researchers can create multi-organ systems or even a human-on-a-chip. Such efforts recently resulted in the first FDA approval of human trials for a drug candidate without preclinical animal efficacy data.

Digital twins

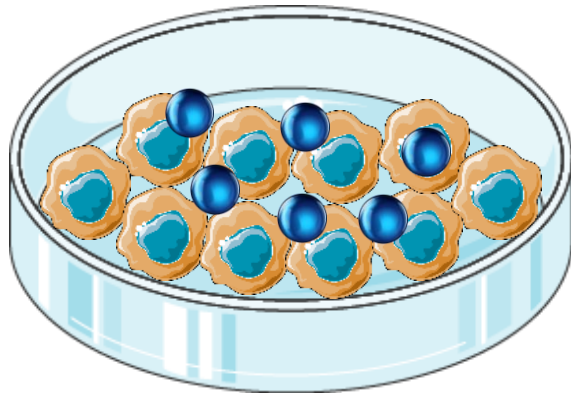
The application of machine learning methods takes advantage of enormous amounts of data from patient records and previous clinical trials to generate predictive models of patient response to an intervention. The creation of a "digital twin" could limit the need for animal testing and the number of patients required for a clinical trial. Theoretically, the model's accuracy would progressively increase with each subsequent trial based on the newly generated data.



Cell culture models

2D

 Drug / NPs

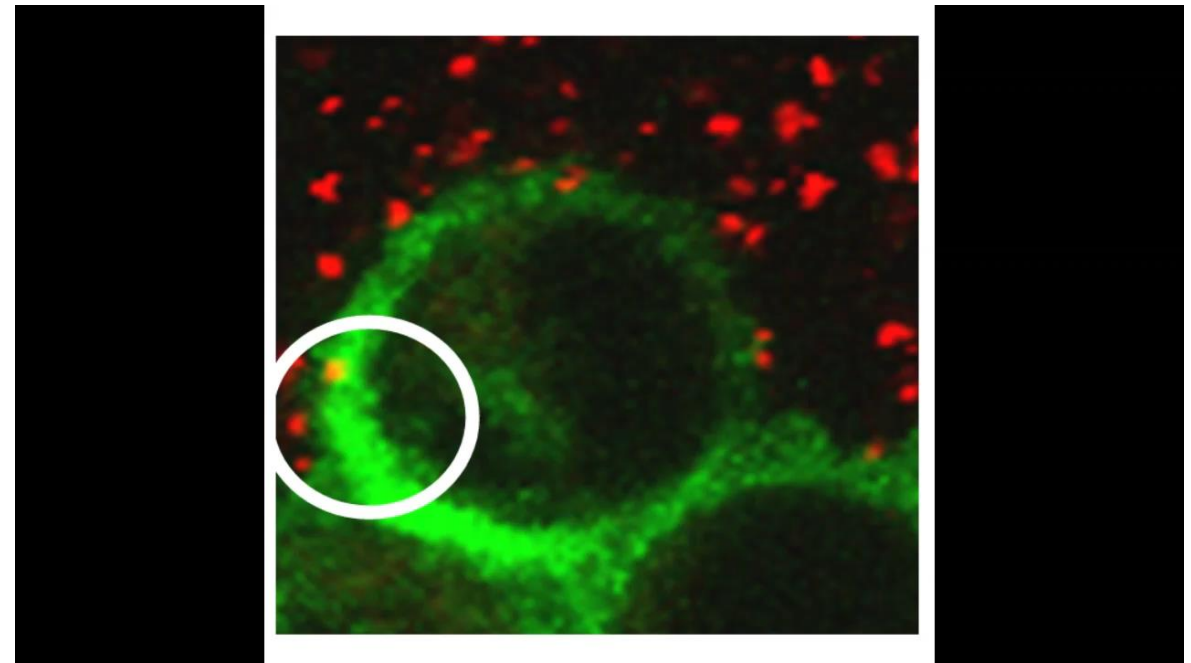


Cell-uptake studies

- Confocal microscopy

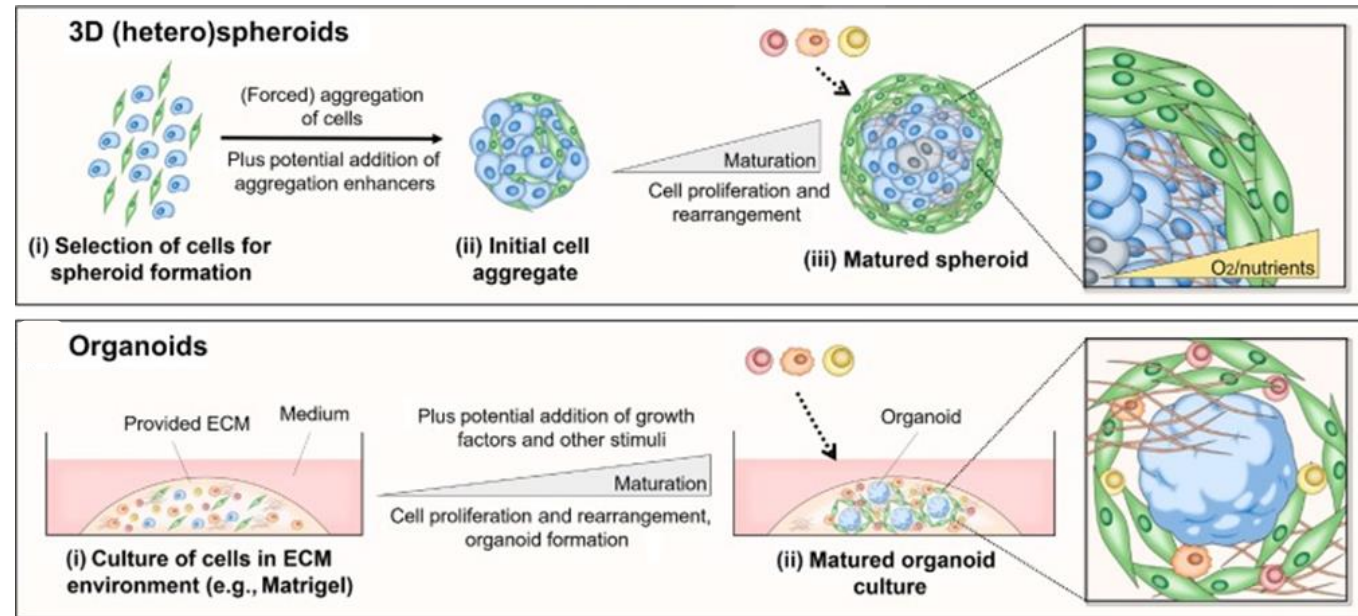


Uptake of fluorescently-labeled liposomes by macrophages (membrane labeled in green)



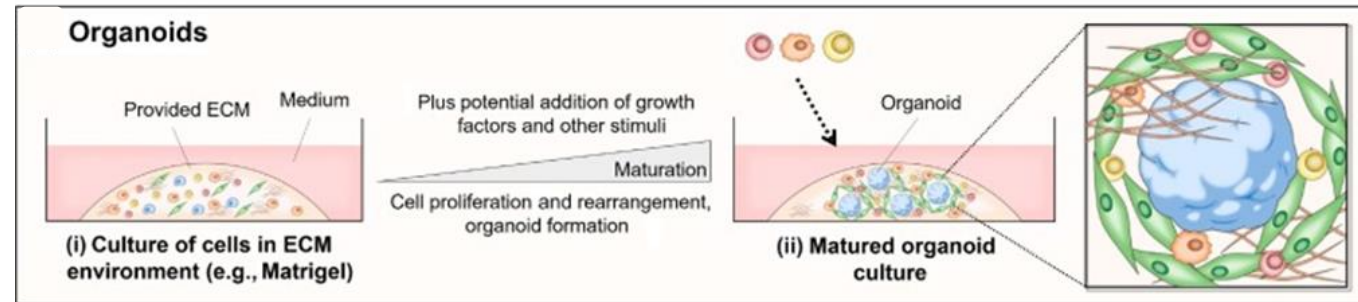
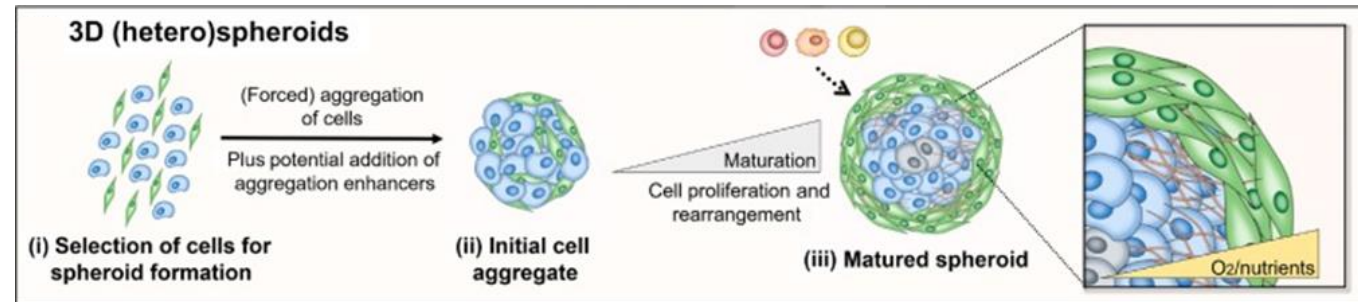
3D culture models

- Cell-Based

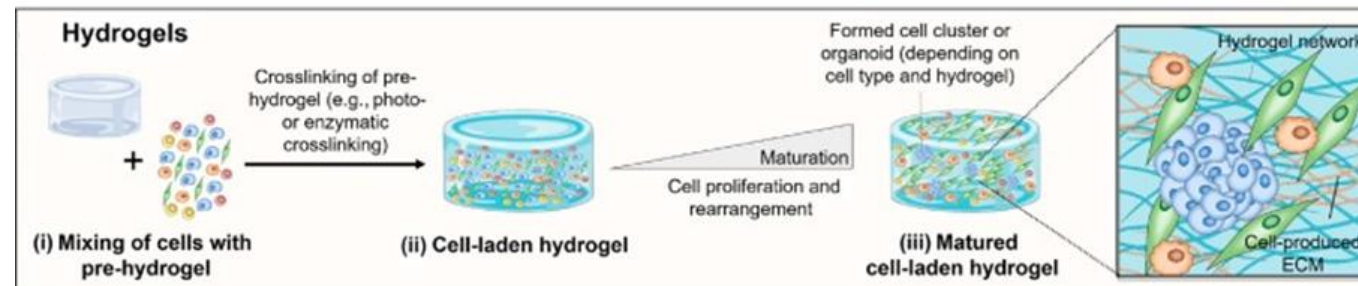
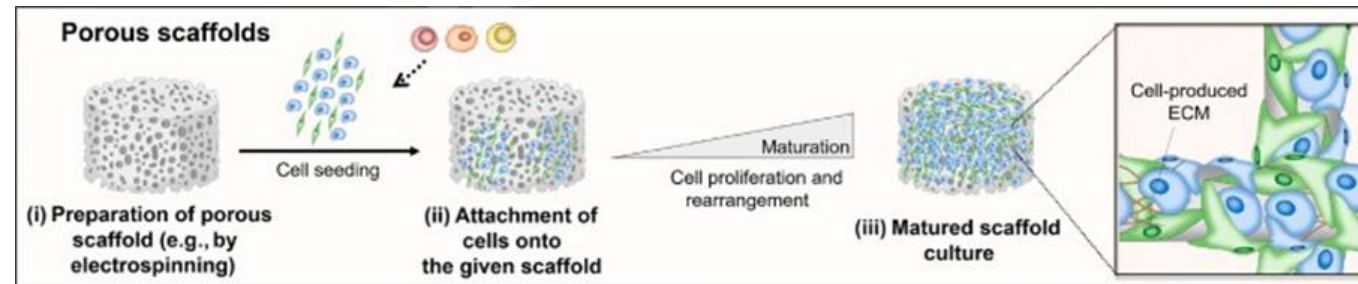


3D culture models

- Cell-Based

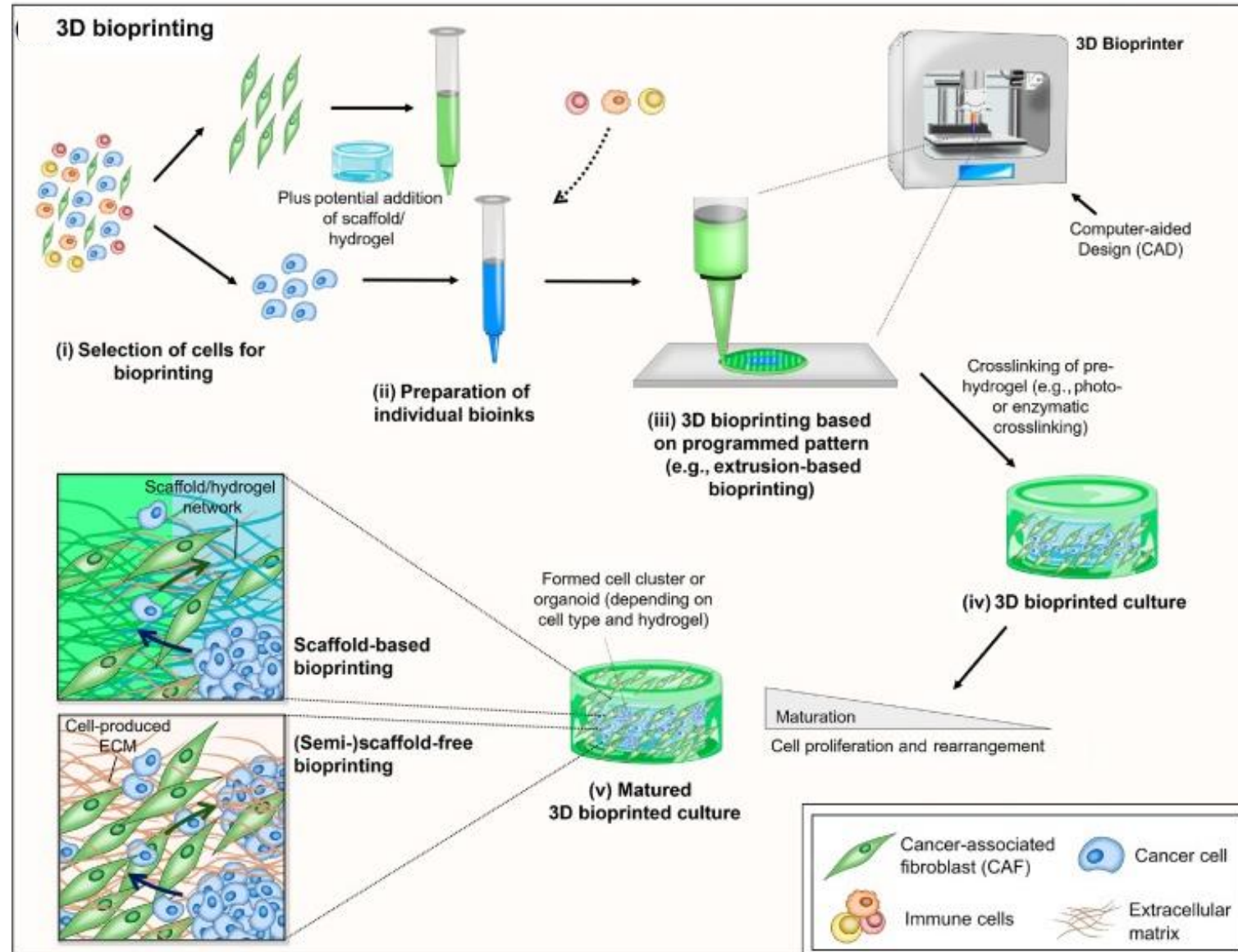


- Cell/Extracellular Matrix (ECM)-Based



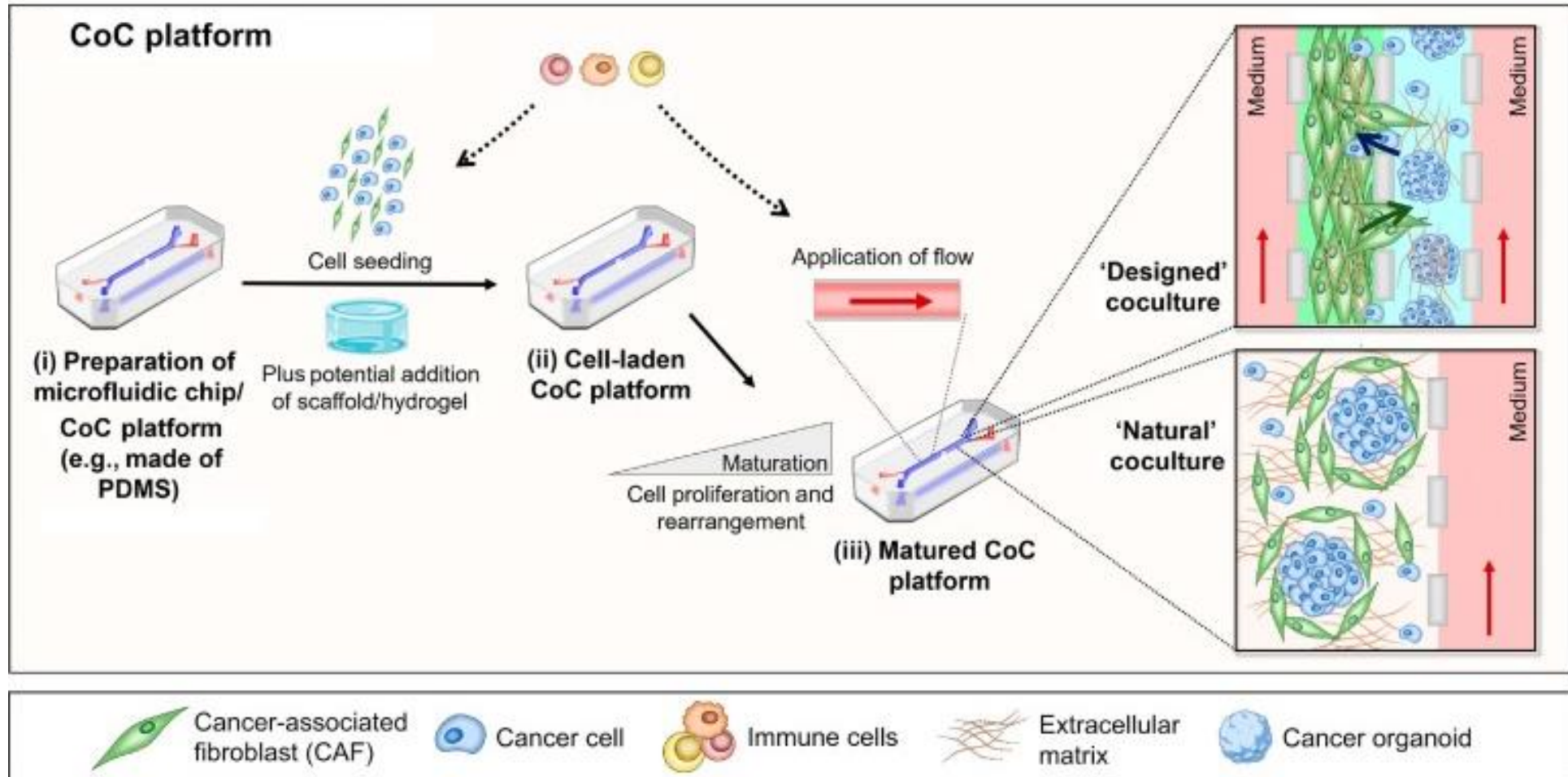
3D culture models

- Cell/Extracellular Matrix (ECM)-Based



3D culture models

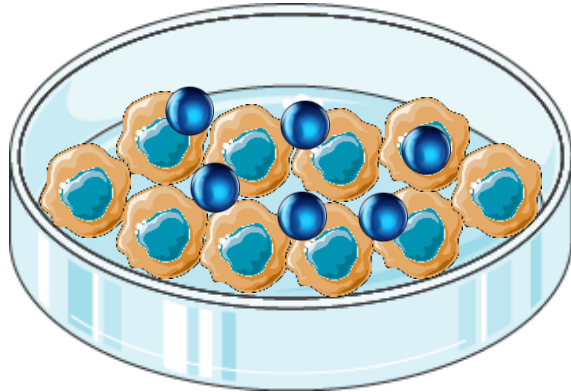
- Microfluidic Cancer-on-a-Chip (CoC)



Cell culture models

2D

 Drug / NPs

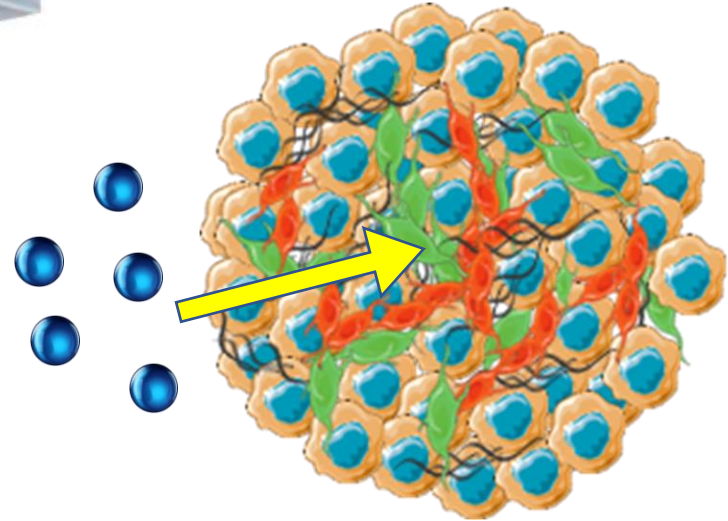


Cell-uptake studies

- Confocal microscopy



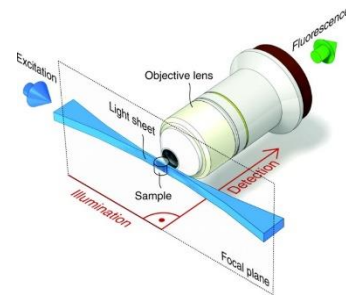
3D



Cell-uptake studies

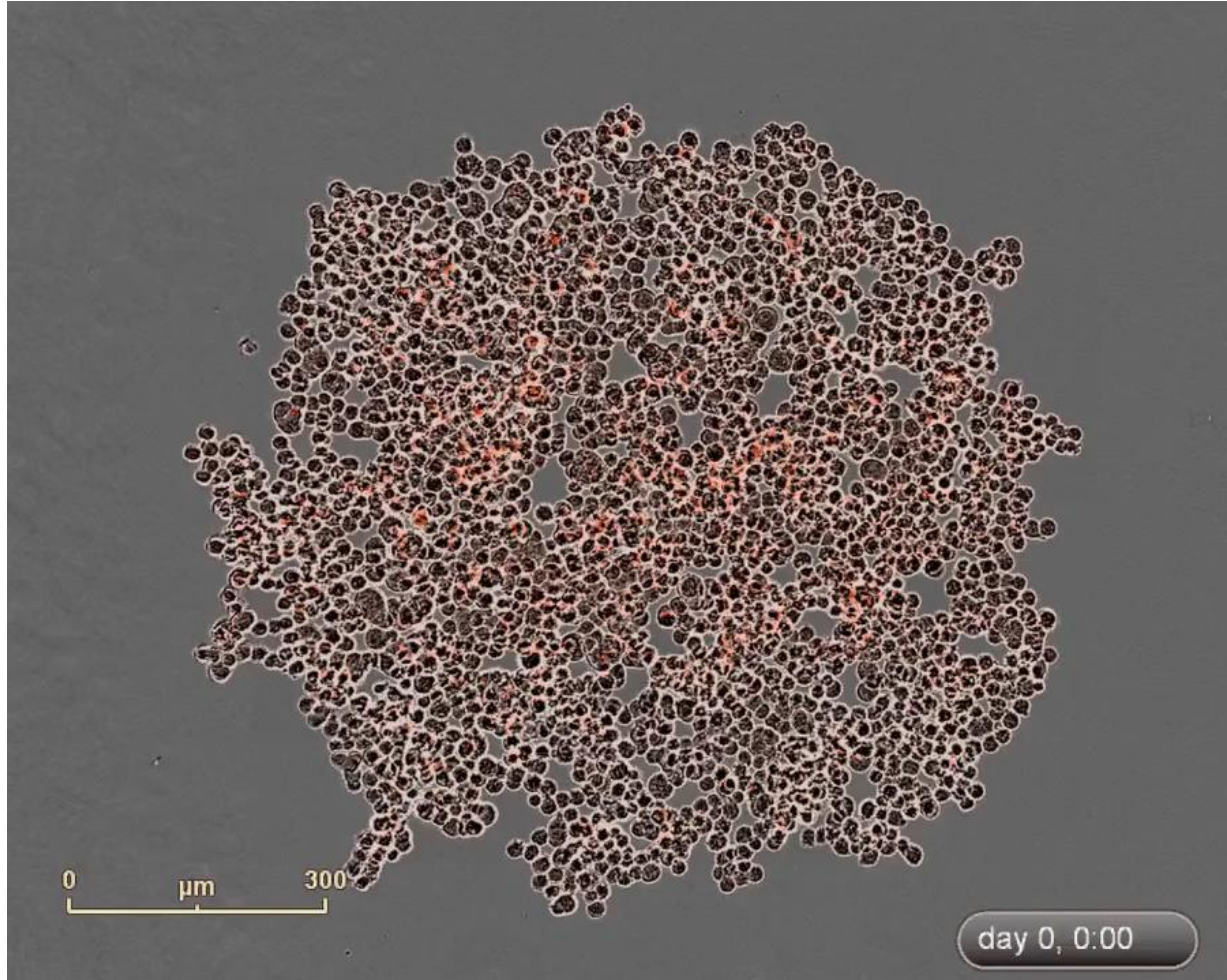
Penetration studies

- Light sheet Microscopy



Spheroids

- A549 human lung carcinoma cells stably expressing the red fluorescent protein



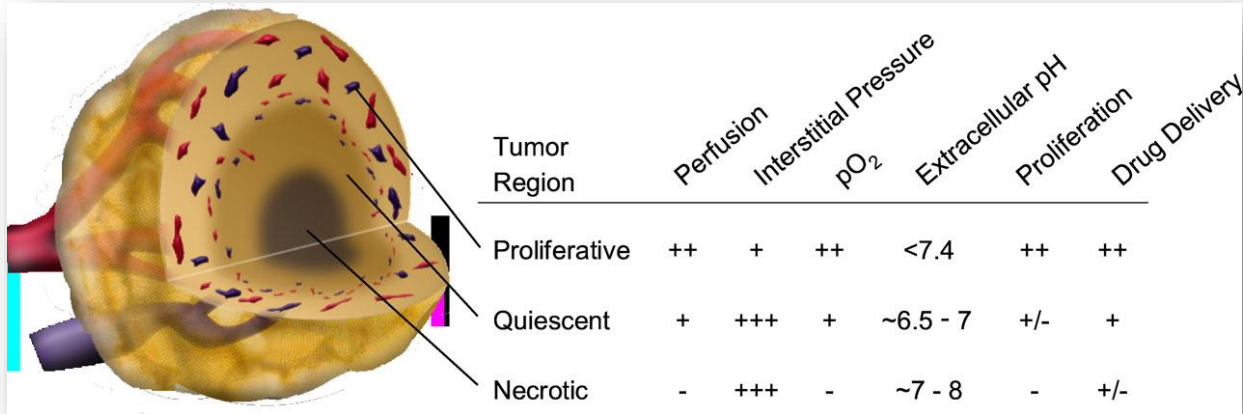
Cell aggregation and spheroid formation:

D3= 400 μm

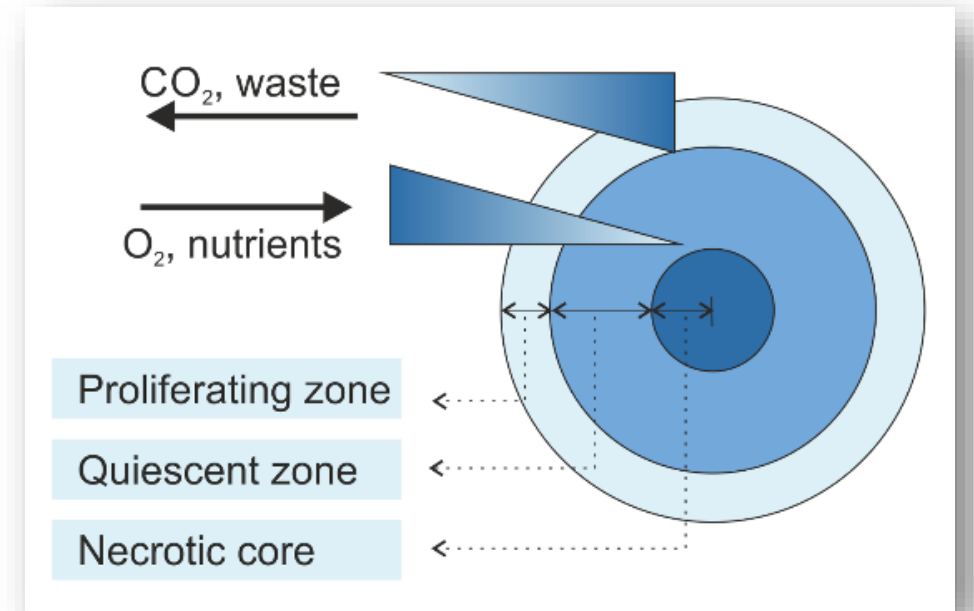
D10= 560 μm

Ancorage independent

- Common and versatile method for 3D cell culture
- Physico-chemical gradients



Tumor spheroids



Tumor spheroids

- Fabrication methods

- Liquid overlay

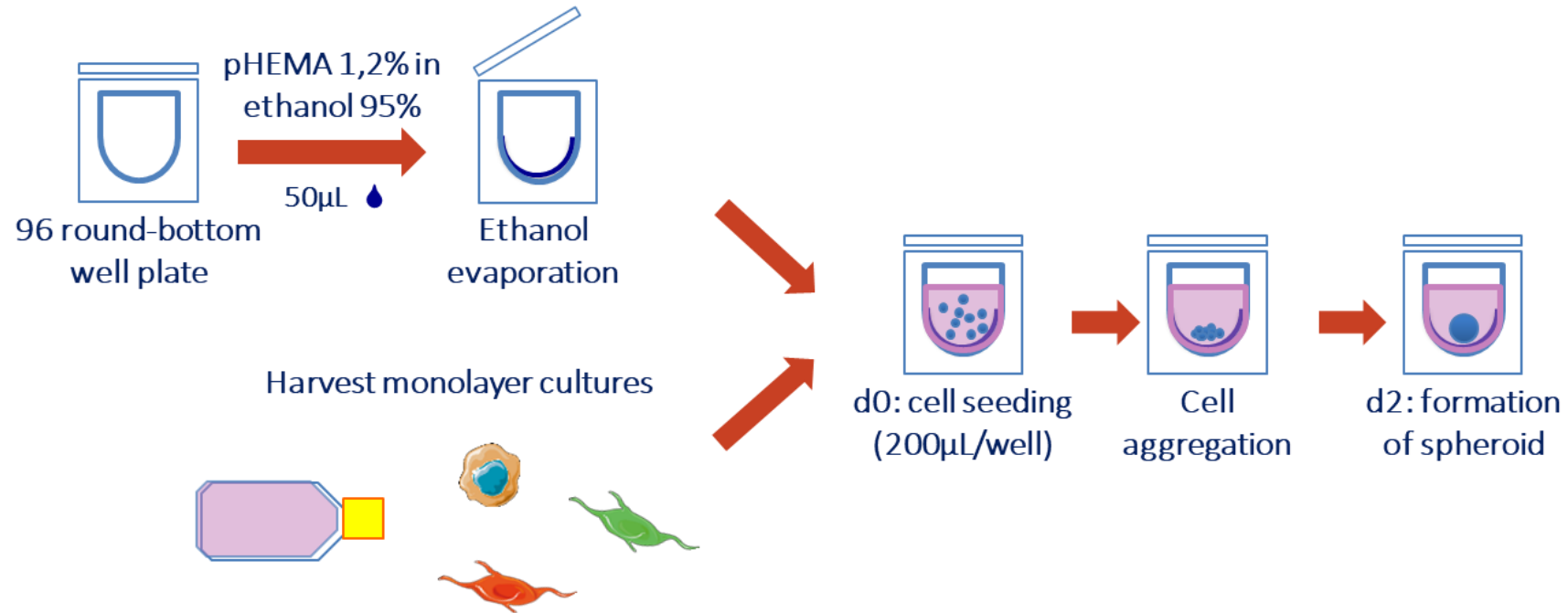
96 well plates



Flat bottom – Agarose coated (1.5% in DMEM) 50 μ l

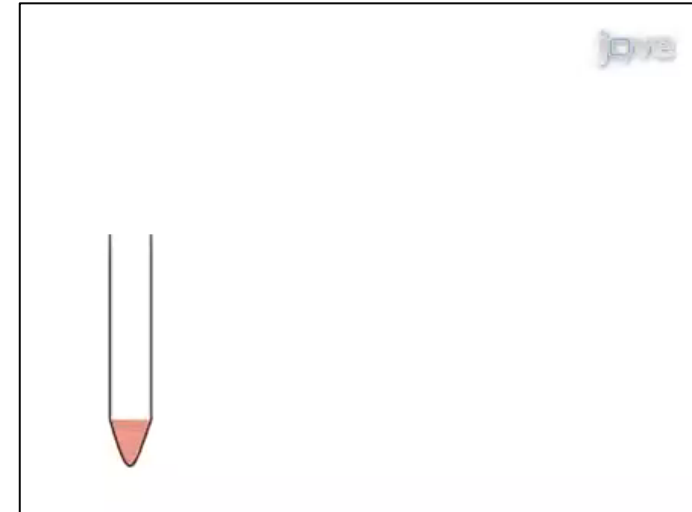
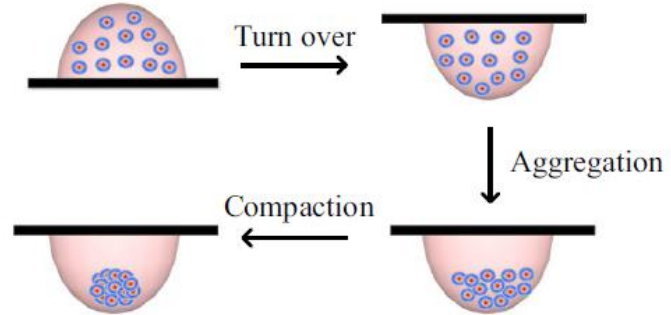
Round bottom – polyHEMA coated (1.2% in EtOH 95%) 2*50 μ L

Round bottom – ultralow attachment (ULA) plates

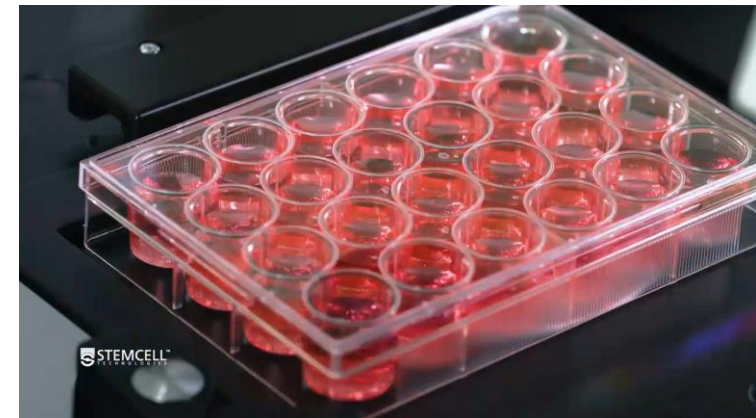


Tumor spheroids

- Fabrication methods
- Hanging drop

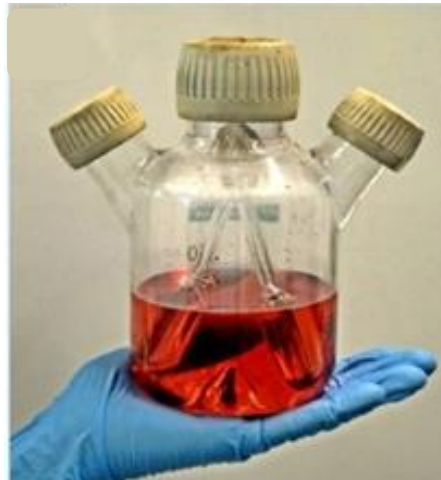
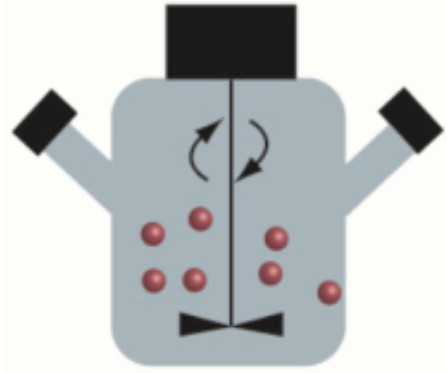


- AggreWell™



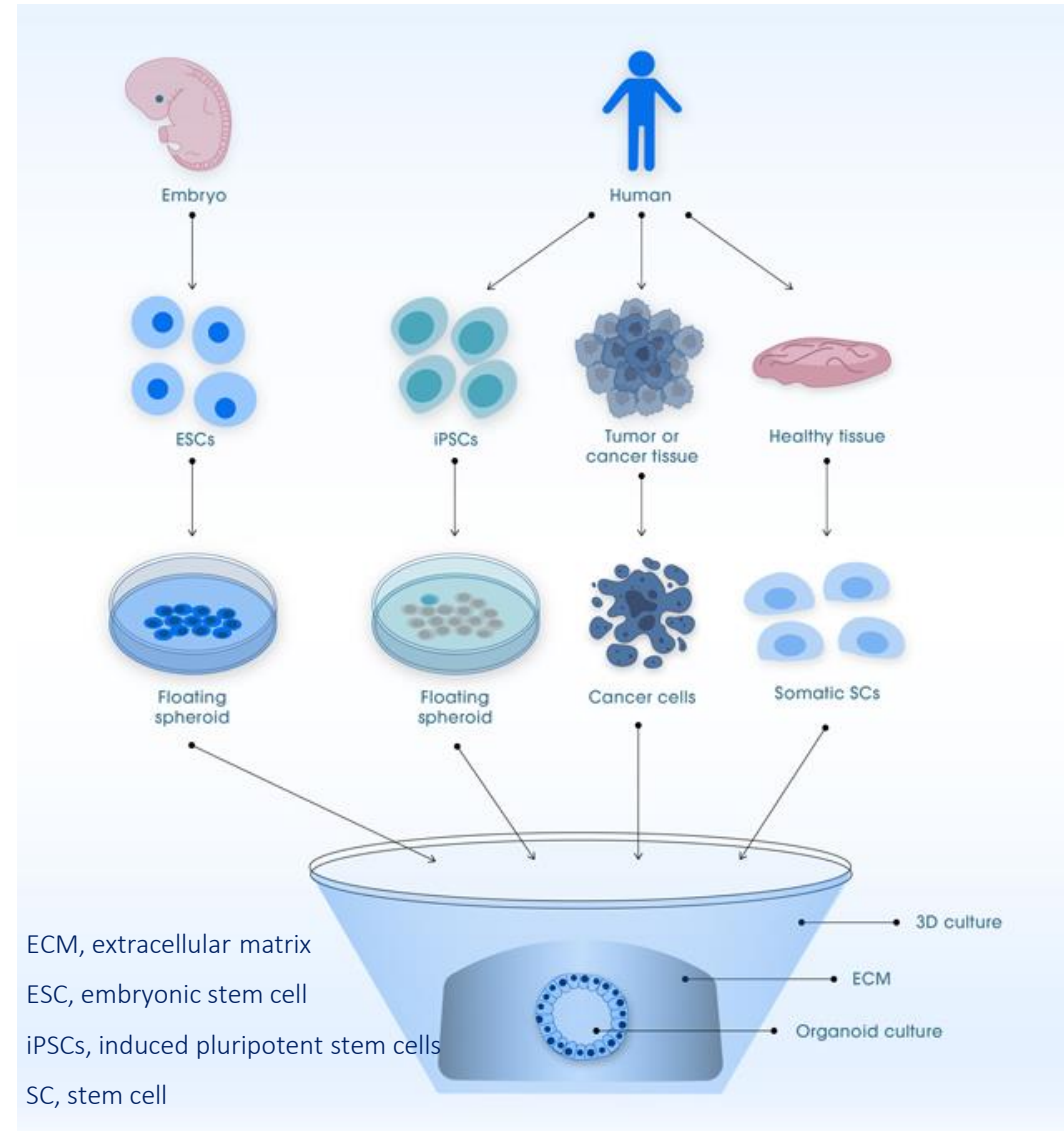
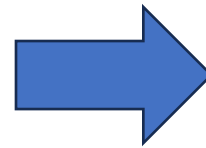
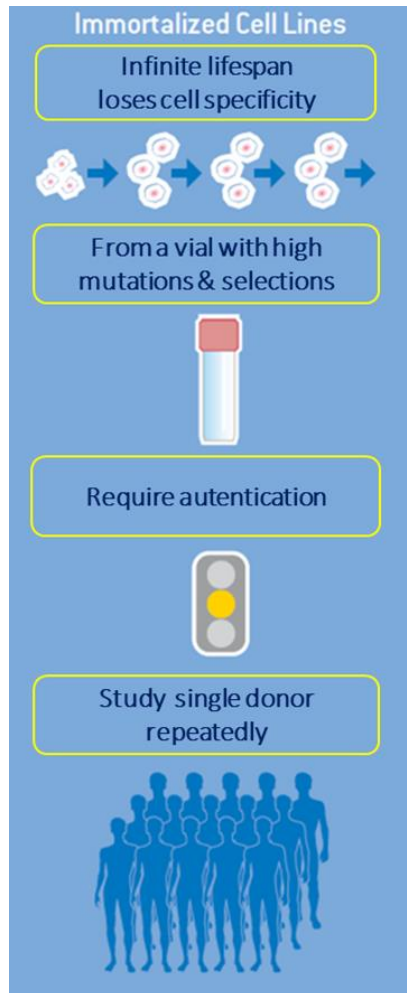
Tumor spheroids

- Fabrication methods
- Spinning Flask



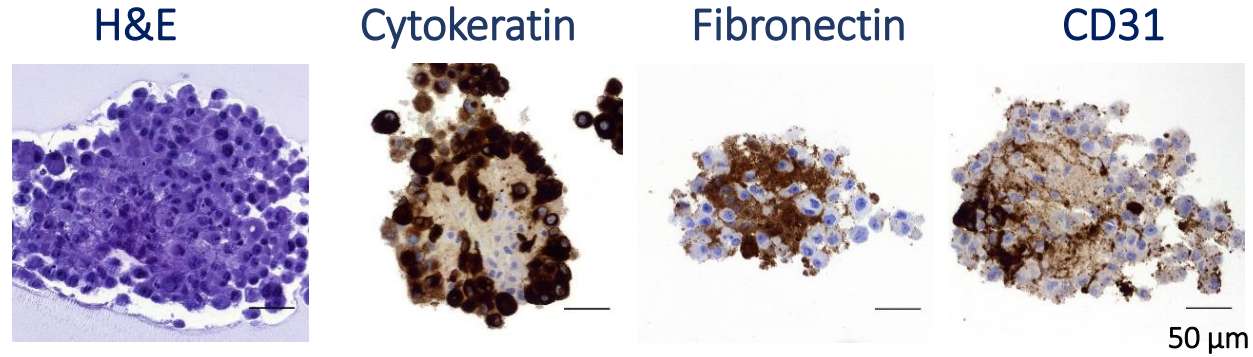
Spheroids vs Organoids

- Three-dimensional (3D) multi-cellular, microtissues derived from human embryos, organs or tumors.



Tumor spheroids

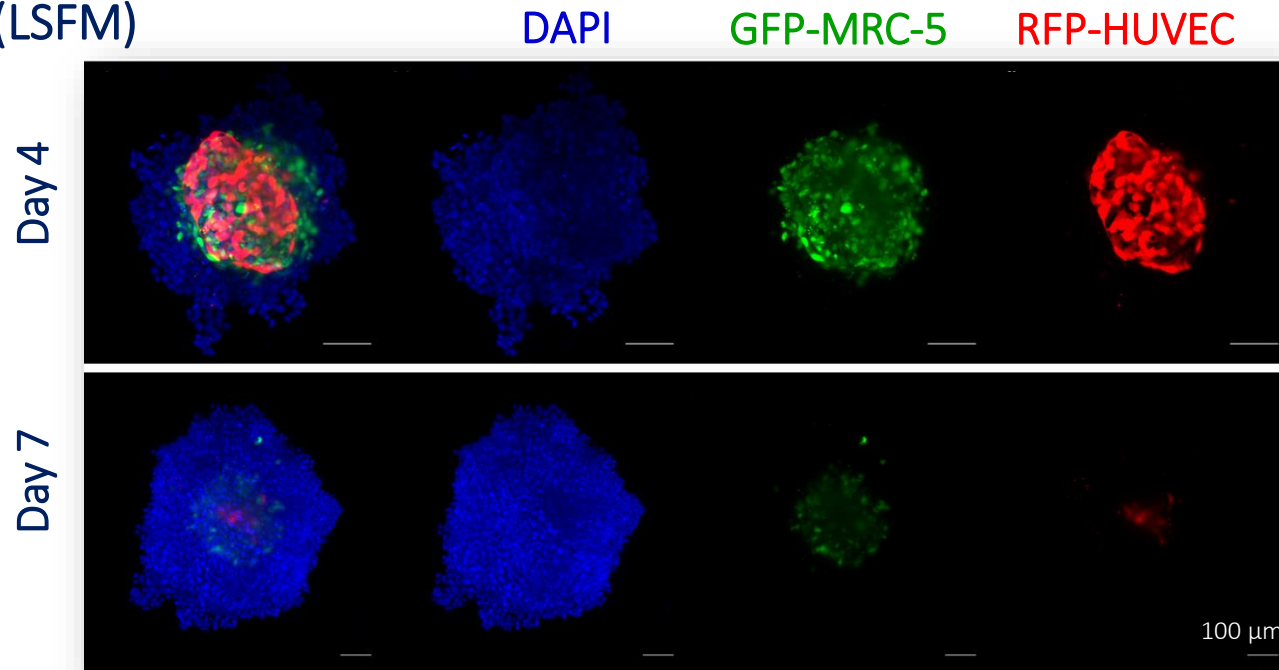
- Heterotype multicellular spheroids triple co-culture (PANC-1: MRC-5: HUVEC)
- Histology



- Liquid overlay
- LBL coating
- VEGF



- Light sheet fluorescence microscopy (LSFM)



First model of triple spheroid co-culture combining tumor cells, fibrotic tissue and a collapsed vessel-like structure

3D culture models

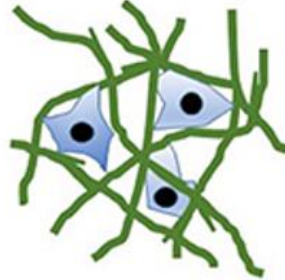
Natural hydrogels

Animal Derived

- Collagen
- Matrigel
- Gelatin

Plant Derived

- Alginate



Synthetic hydrogels

Non-natural

- Polyethylene Glycol (PEG)
- Polylactic Acid (PA)
- Polyglycolic Acid (PGA)

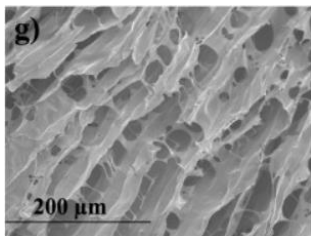
Natural

- Hyaluronic Acid (HA)
- Peptides

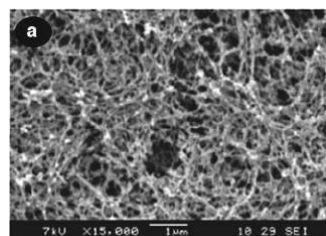
- + Biomimetic
- + Mimic physiological cell/material interactions
- Batch to batch variability
- Limited range of material properties
- Limited cell adhesion site number

- + Possibility to easily tune structural properties
- + Mimic specific microenvironment features
- Potential toxicity due to fabrication methods
- Limited bioactivity

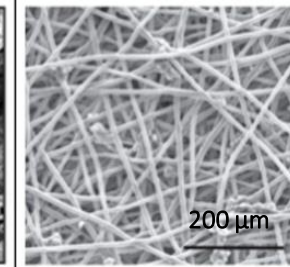
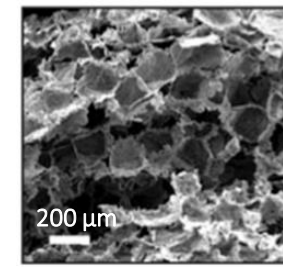
Collagen



Matrigel

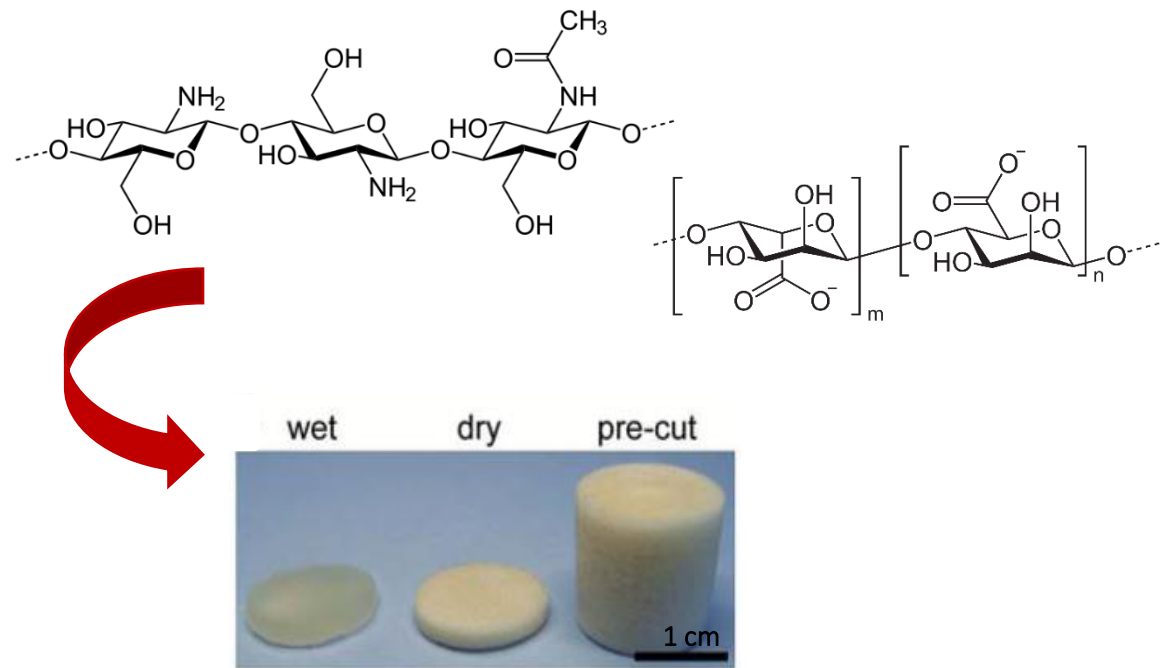


poly-lactic-glycolic acid polycaprolactone

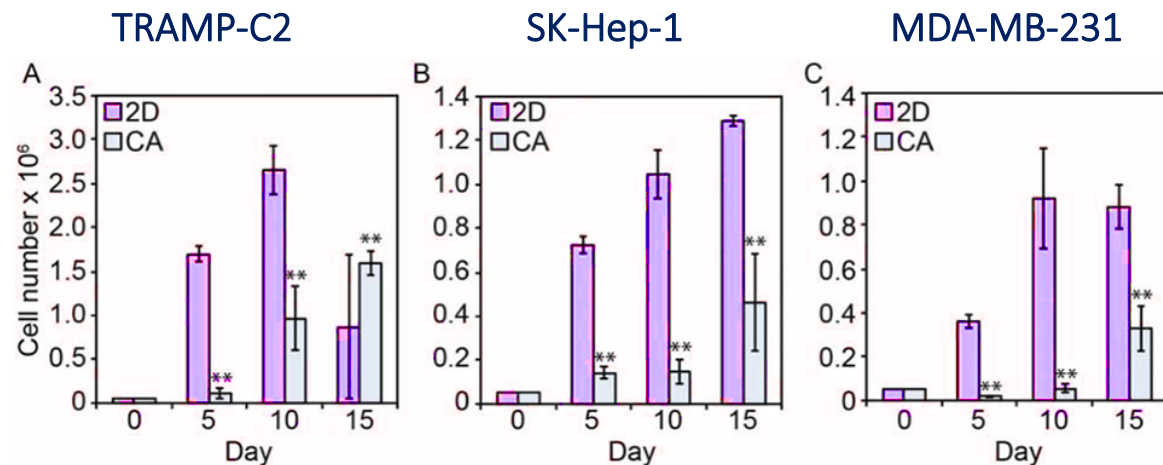


Anchorage dependent: natural hydrogels

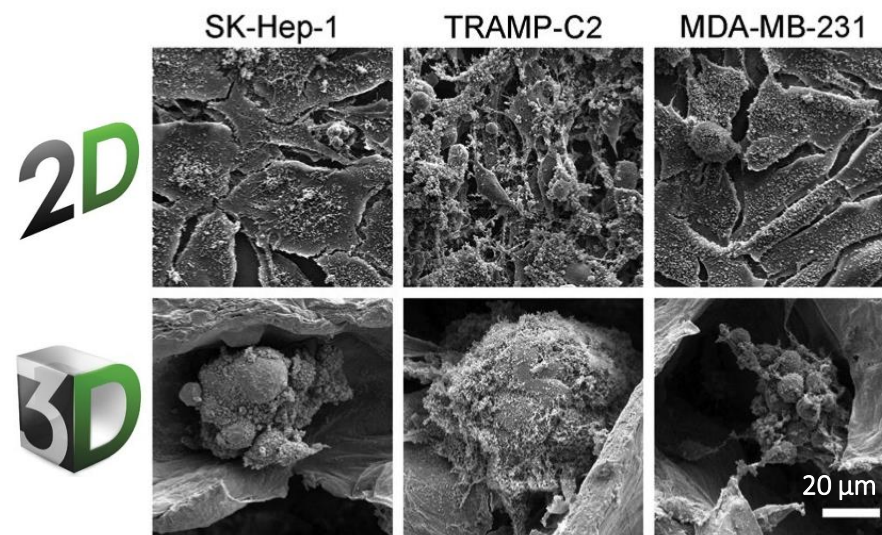
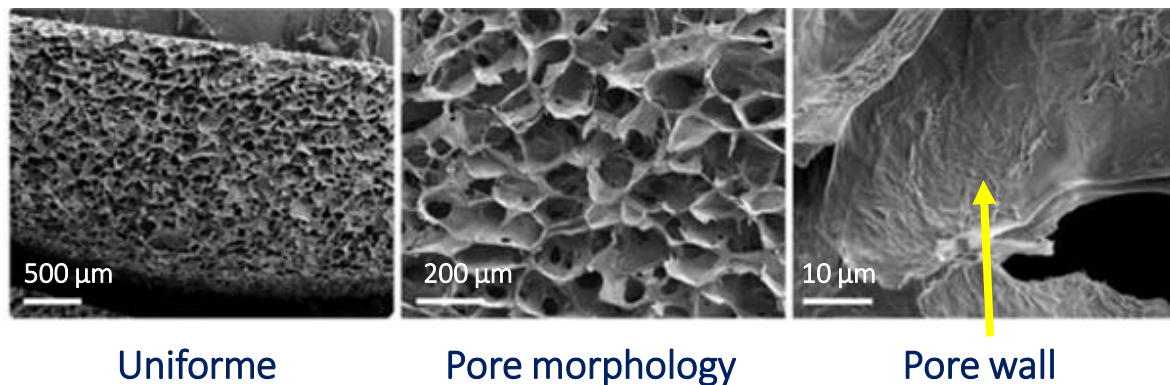
- Chitosan-alginate polyelectrolyte complex



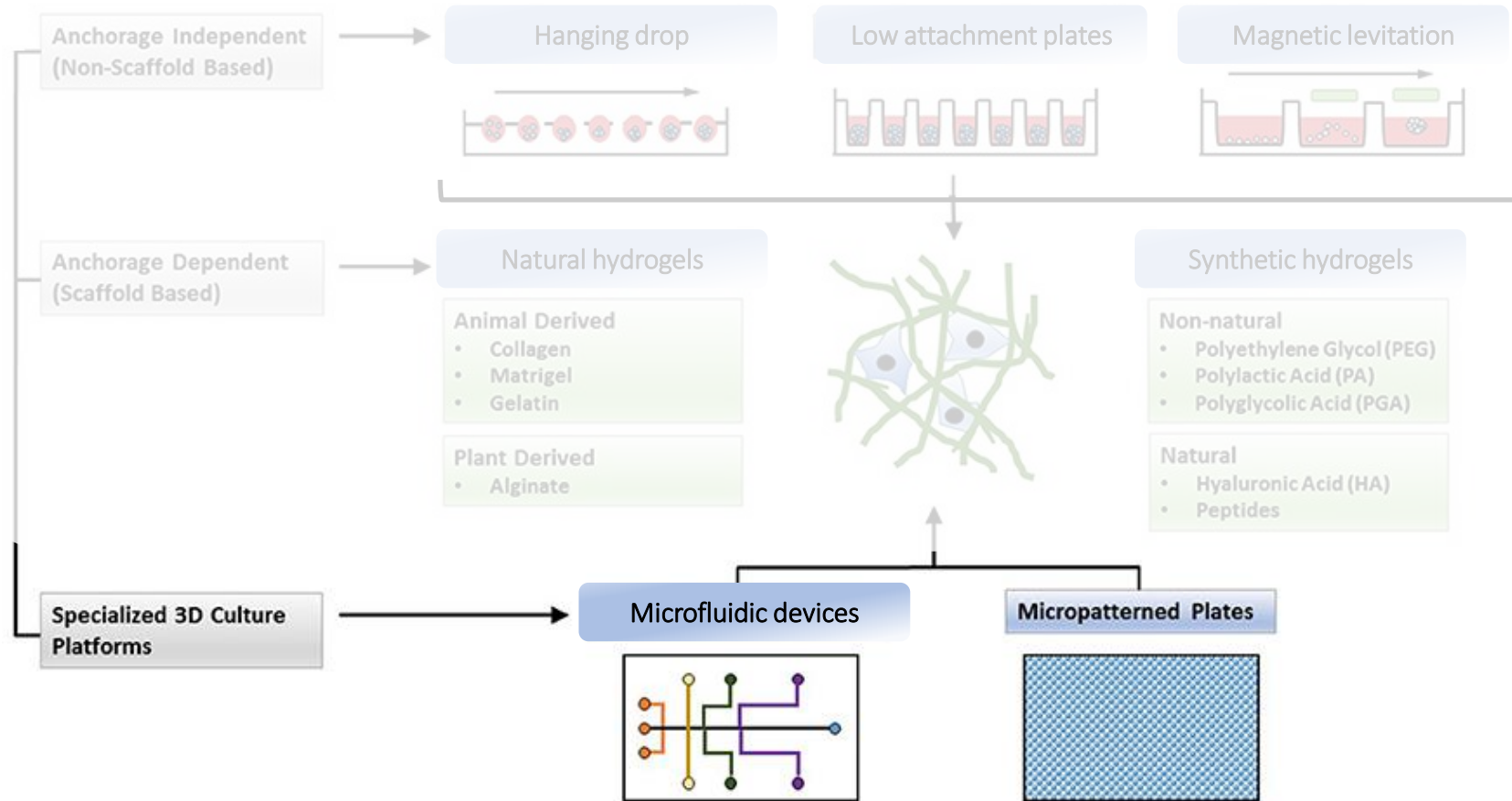
- Cell culture



- Scaffold porosity

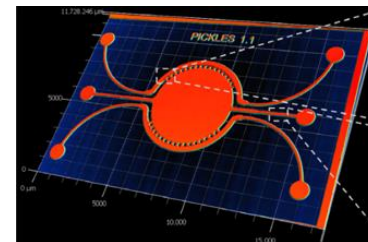
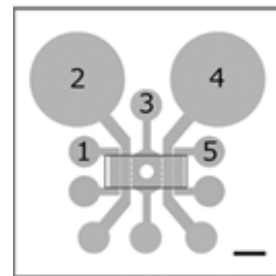
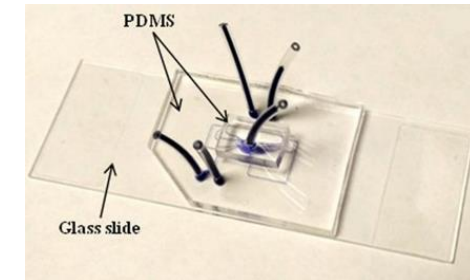
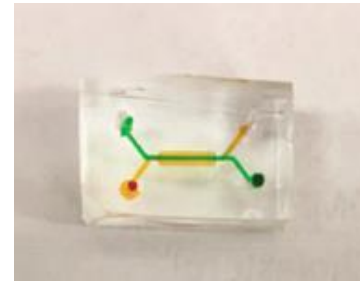
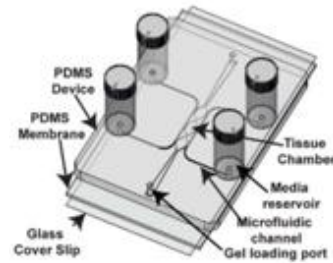


3D culture models



Microfluidic devices

- Culturing living cells in continuously-perfused, micrometer sized chambers
- Model physiological functions of tissues and organs
- Incorporate physical forces, fluid shear stress
- Strong control of culture parameters
- Evaluation of biological responses: cell recruitment, response to drug treatment



Organs-on-chips (OoCs) - microphysiological systems - tissue chips

- Integration of design, technology and biological science for more reliable models
- Provide insights into normal human organ function and disease pathophysiology
- Predict the safety and efficacy of promising new compounds and therapeutics

- NIH, FDA and DARPA funded programs

Tissue Chips for Drug Screening

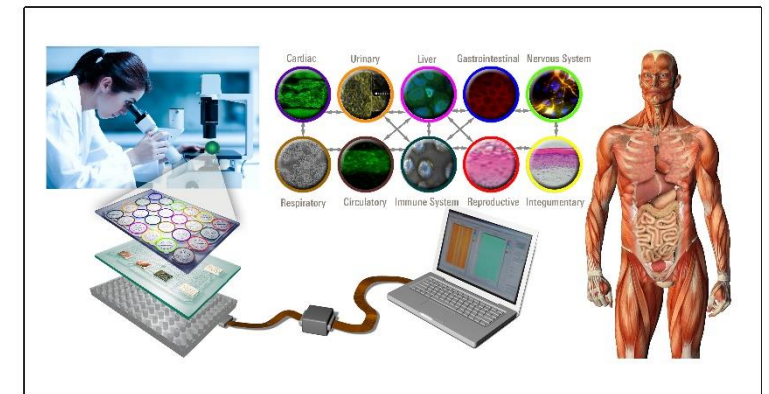
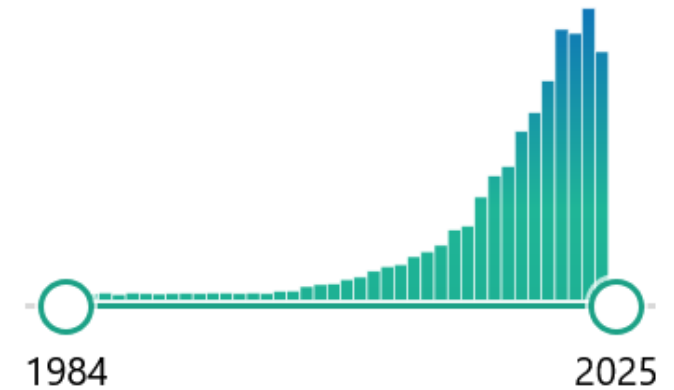
develop 3D microsystems to represent multiple tissue types

Microphysiological systems programme

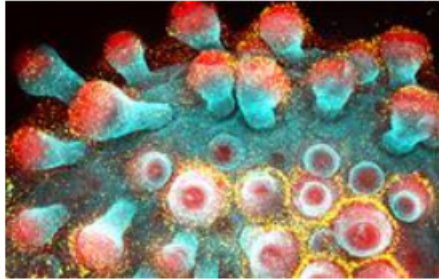
develop a system integrating at least 10 human organs/tissues to mimic and replicate biological crosstalk between tissues.

- Pubmed search « *organ on chip* »

5485 articles
@ 03/10/2024



Organs-on-chips (OoCs) - microphysiological systems - tissue chips



CEA IRIG

FRANCE 2030 - PEPR

MED-OOC : Organes et organoïdes sur puce



Le PEPR exploratoire MED-OOC vise à réunir organoïdes, microfluidique avancée et expertise clinique pour obtenir des organes sur une puce reproduisant fidèlement la situation *in vivo* afin d'accélérer la découverte de médicaments, de modéliser les processus de développement et de développer des systèmes expérimentaux personnalisés ou des « jumeaux cliniques ».

Ce PEPR a été retenu en 3ème vague en 2023 et se met en place. La DRF devrait y contribuer activement par le biais de ses instituts Irig et Jacob.

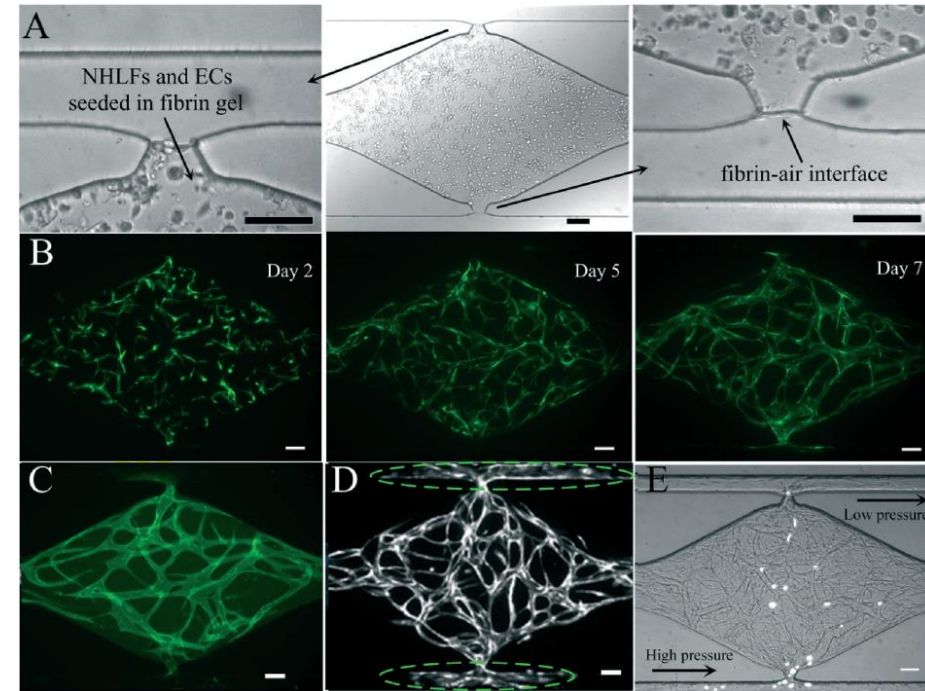
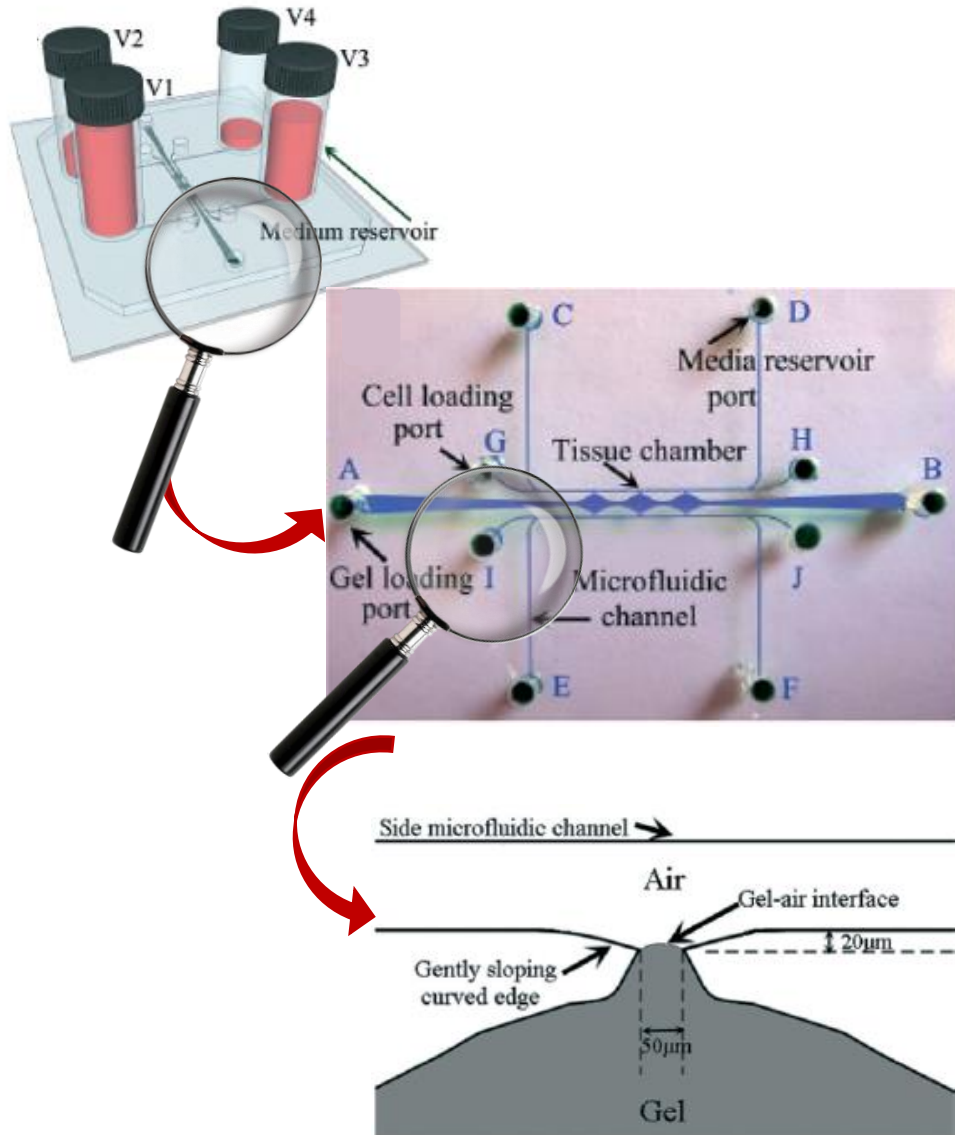
Co-pilotes : CEA, CNRS, Inserm
Budget : 48 M€
Durée : 6 ans

PEPR* exploratoires: *accompagner une transformation qui commence à émerger et en est à ses débuts voire à ses prémices, pour un montant prévu de 1 Md€*

Permettre la conduite d'une politique scientifique sur des domaines d'intérêts national et européen, aux retombées pouvant être multiples

Microfluidic devices

- Perfusable microvascular network

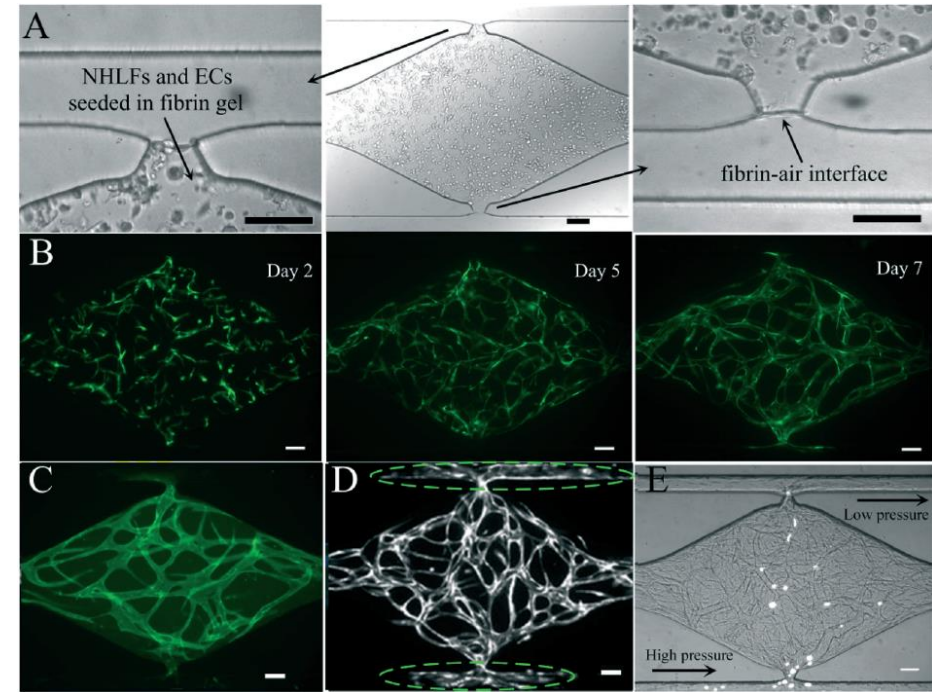
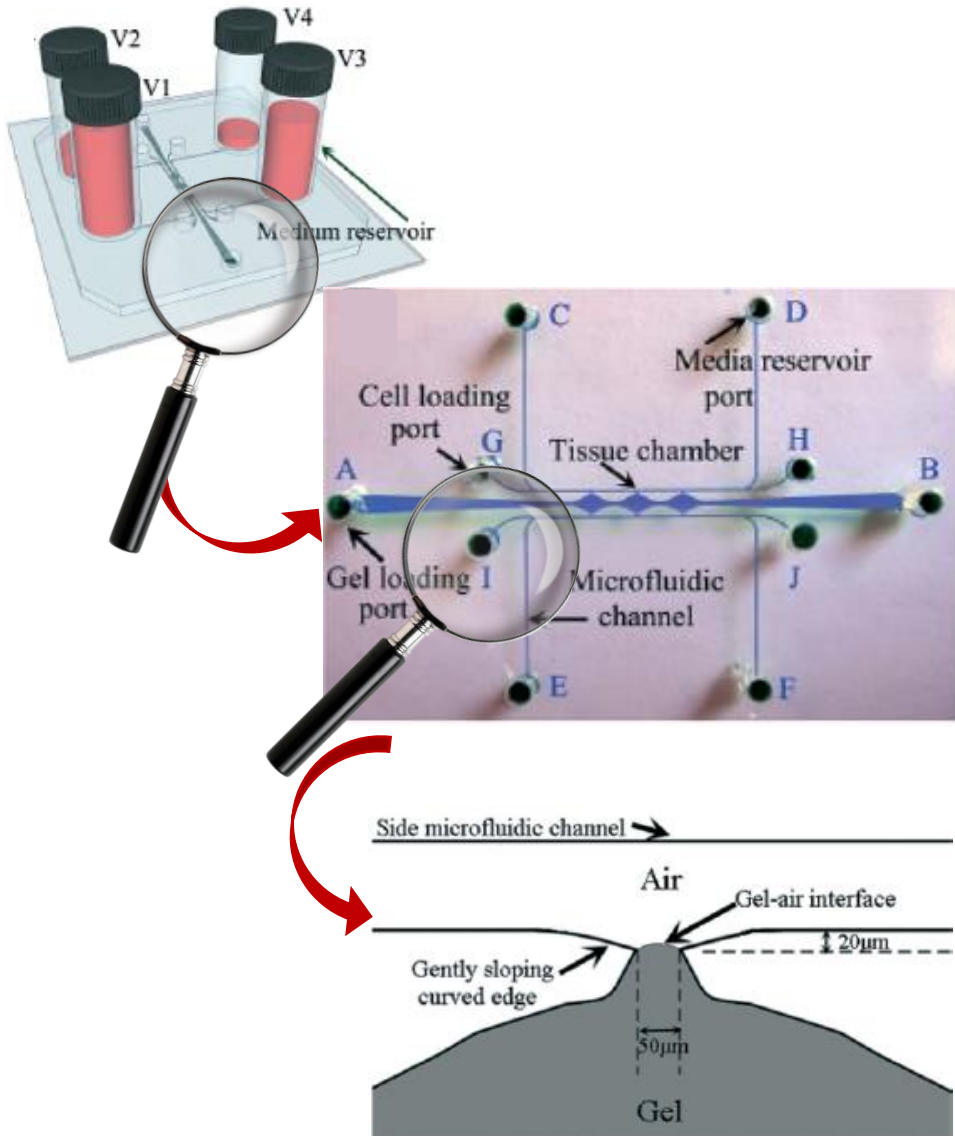


Optimised pore design

- NO gel leakage
- Vasculogenesis, Sprouting & Anastomosis

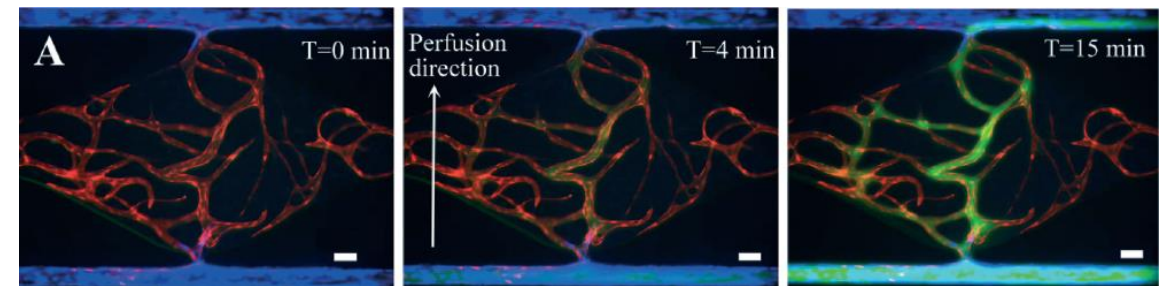
Microfluidic devices

- Perfusable microvascular network

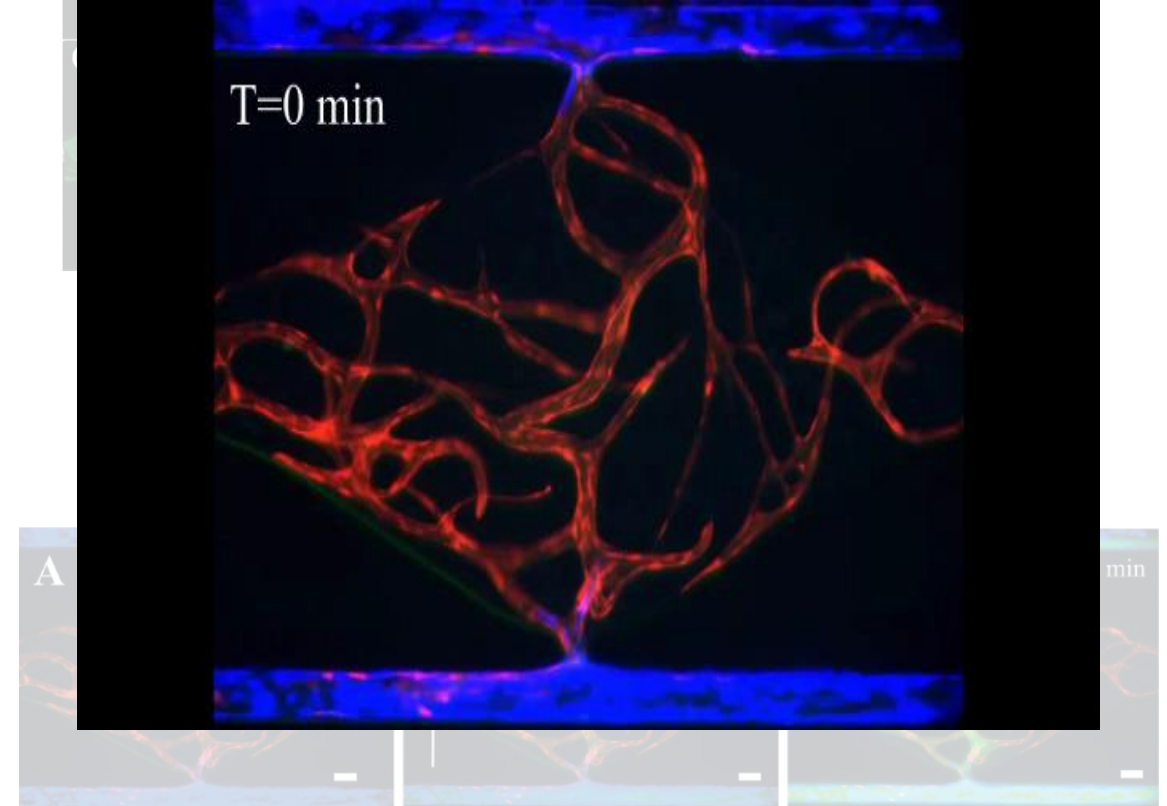
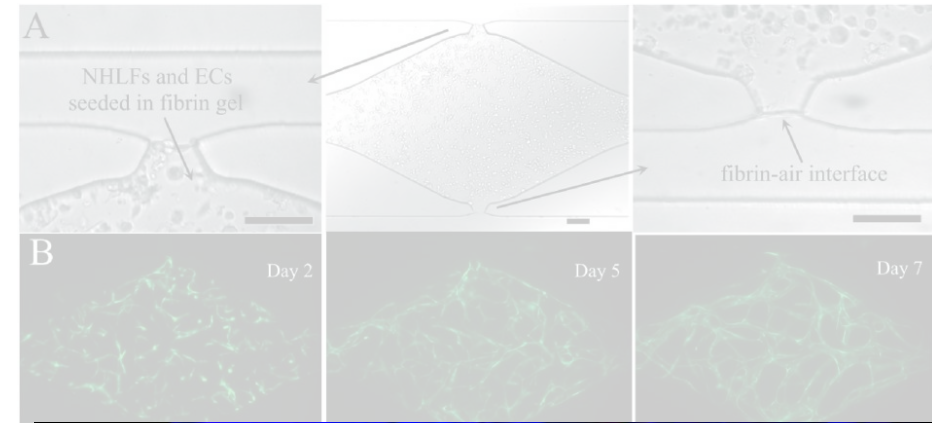
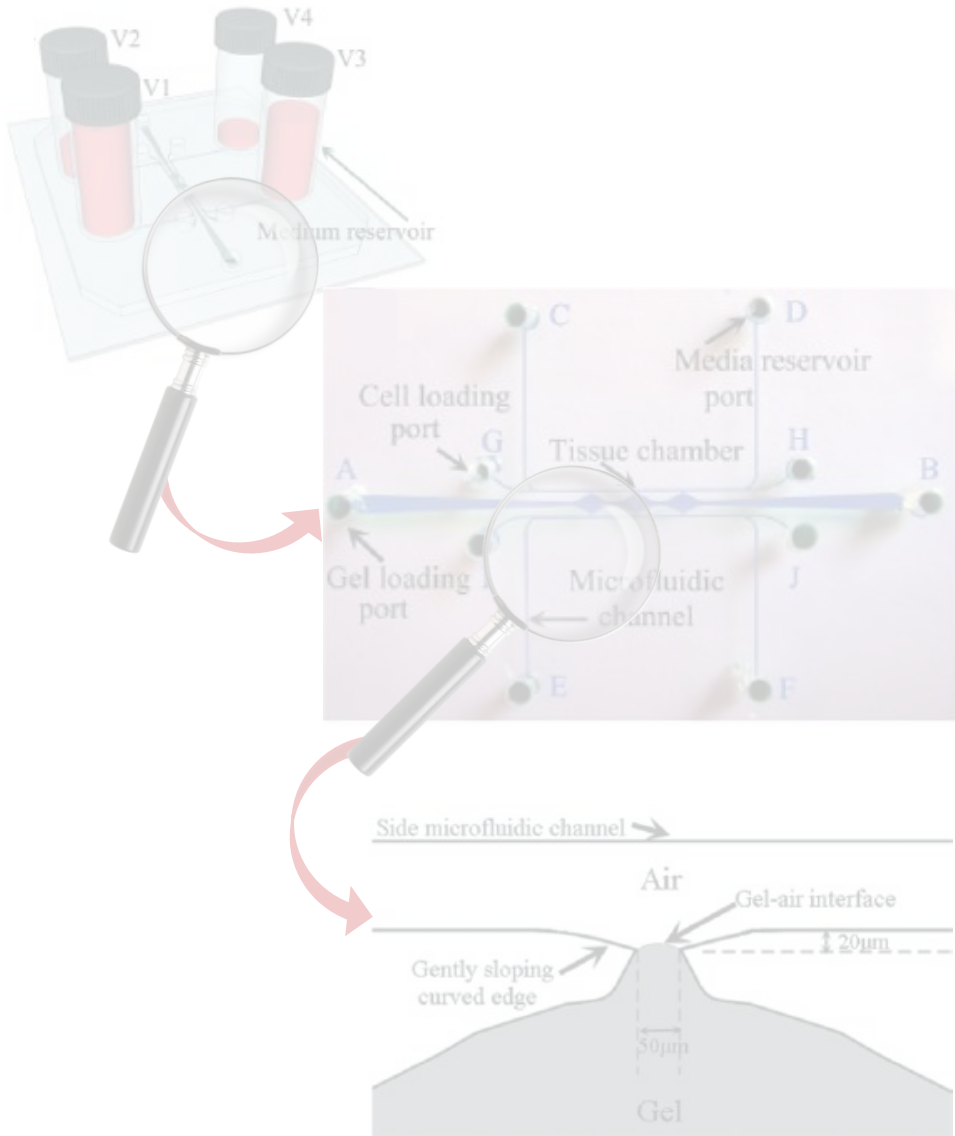


Optimised pore design

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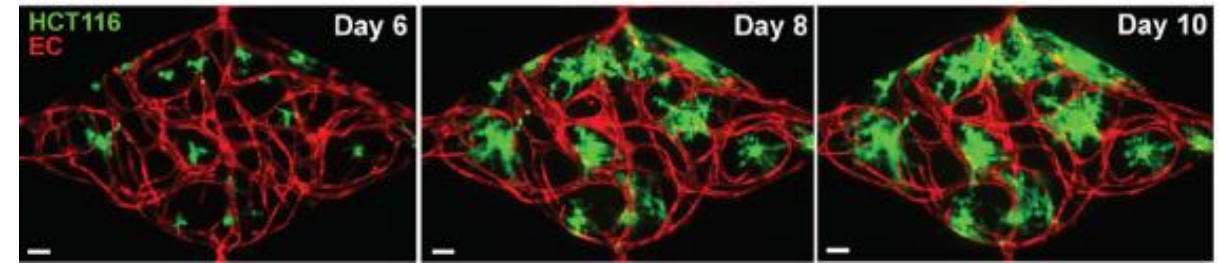
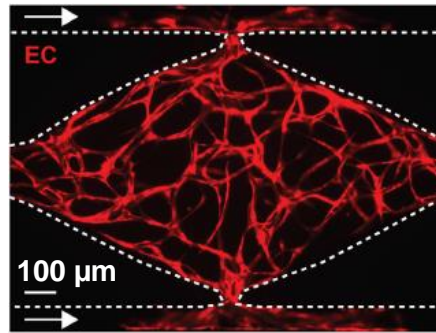
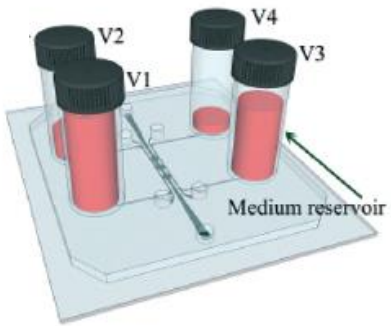


Microfluidic devices

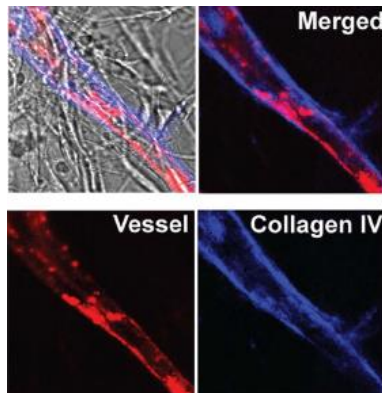
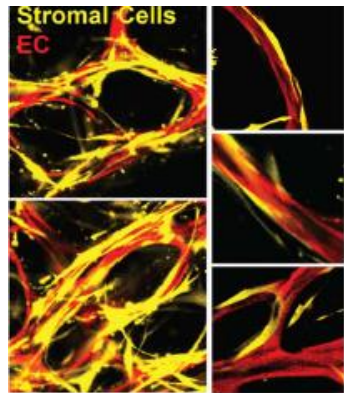


Microfluidic devices

- Perfusable microvascular network
- Coculture with cancer cells: Vascularized Micro-Tumors

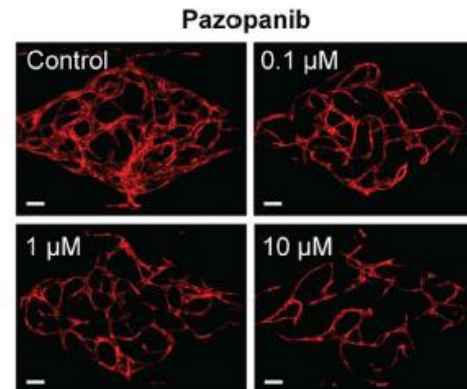
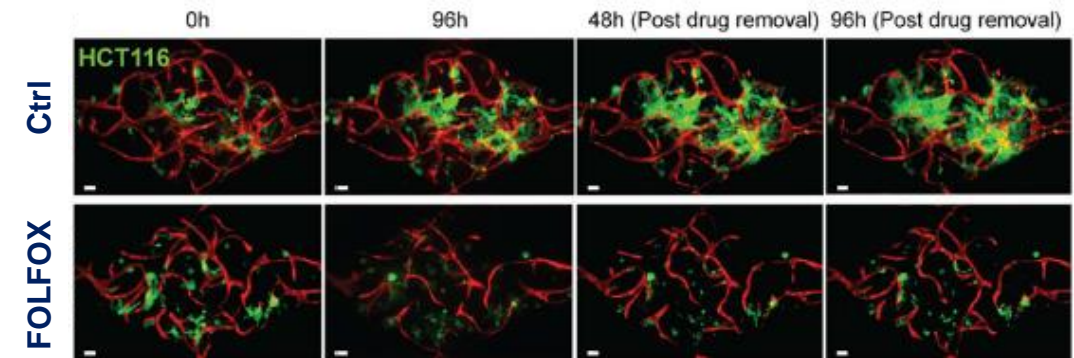


- Drug treatment: cancer or endothelial cell targeting



Stromal cells in perivascular position

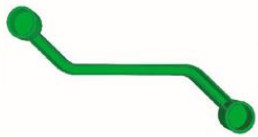
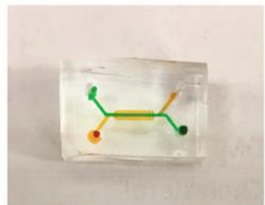
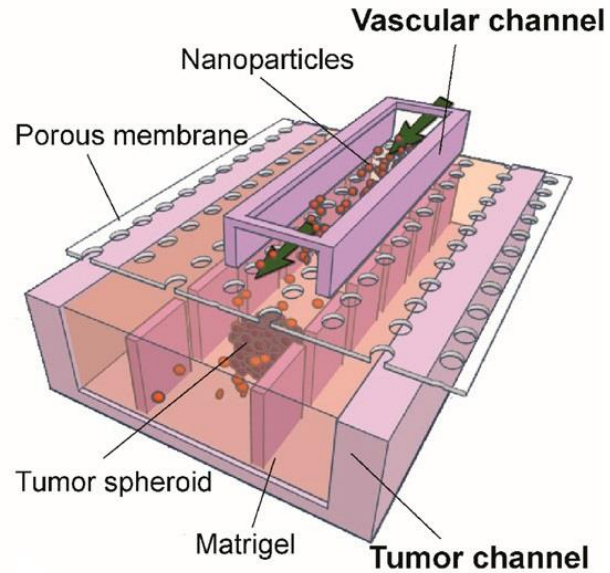
Basement membrane deposition



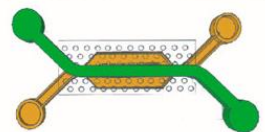
Suitable for the development of novel treatment with multiple targets

Microfluidic devices

- Open top device for nanomedicine screening
- Chip Design

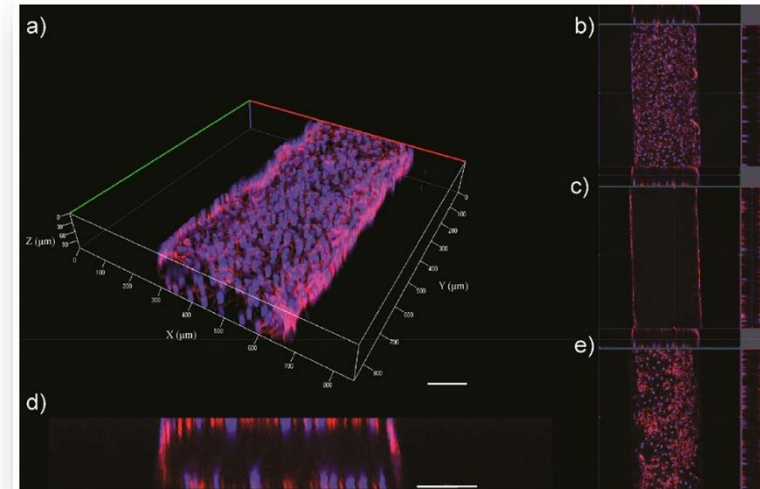


Steady medium perfusion for culturing endothelial cells

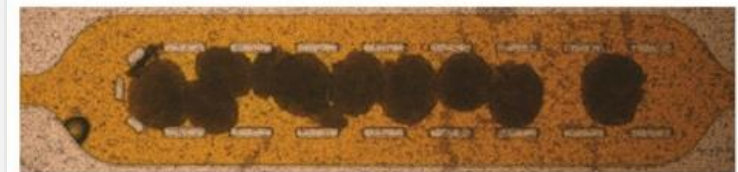


Central region for trapping tumor spheroids

- Confluent HUVEC monolayer

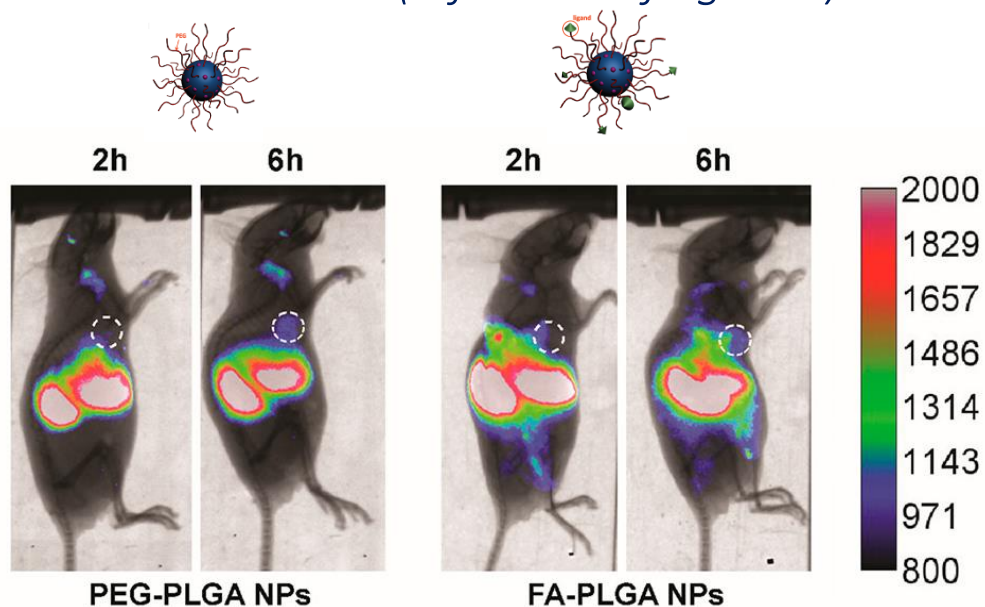


- Ovarian cancer cells (SKOV3) spheroids

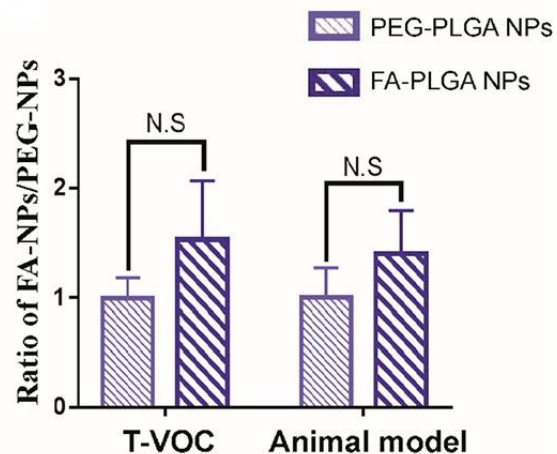
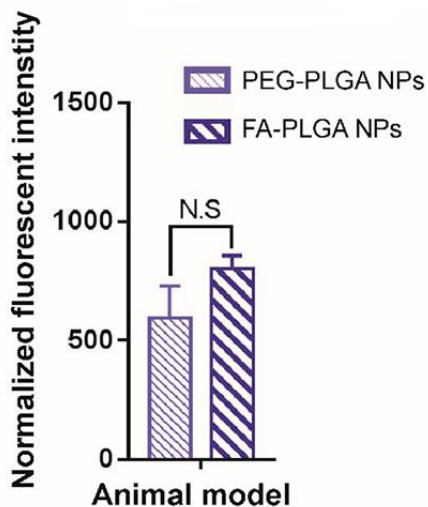
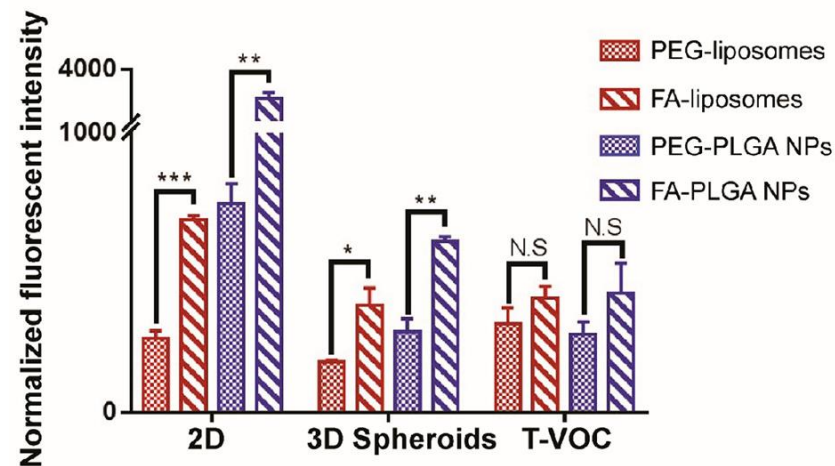


Microfluidic devices

- NP accumulation *in vivo* (influence of ligands)



Better mimicking the *in vivo* tumor microenvironment



- 2D monolayer: FA-modification promotes NP uptake
- 3D tumor spheroids: less significant
- Microchip & *in vivo*: non-significant

Better mimicking the *in vivo* tumor microenvironment

Conclusions



- Lack the organ function
- Lack structure and complexity



- Lower reproducibility
- Endpoint readouts to be optimized
- Challenge to study on a single cell level
- Often limited perfusion

- Very costly and complex
- Low availability
- Some engineering skills
- Not suitable for high-throughput screening



- In Vivo is not a human
- Very costly and time-consuming
- Extrapolate results to the human situation
- Limited mechanistic information



Conclusions

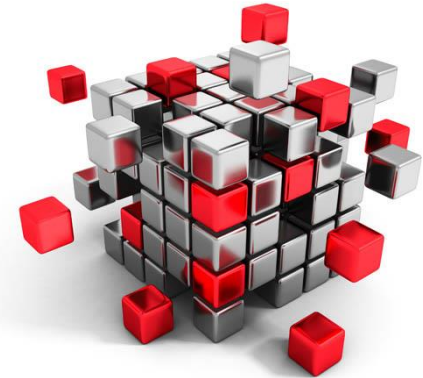
What is your question?



Simple question: use a simple model

**KEEP IT
SIMPLE**

Complex question: go to a more complex model



Conclusions

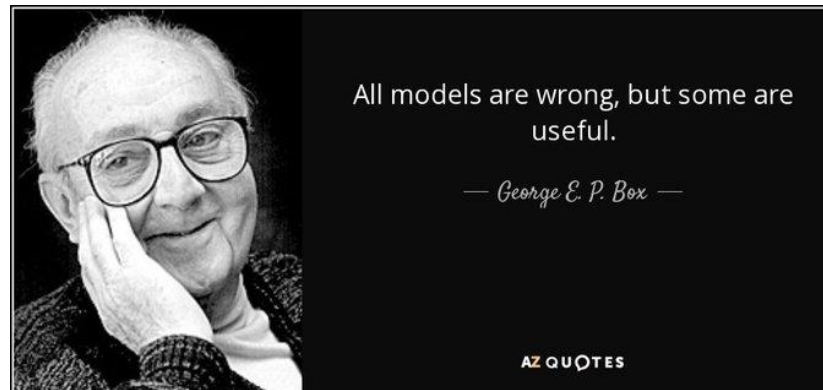
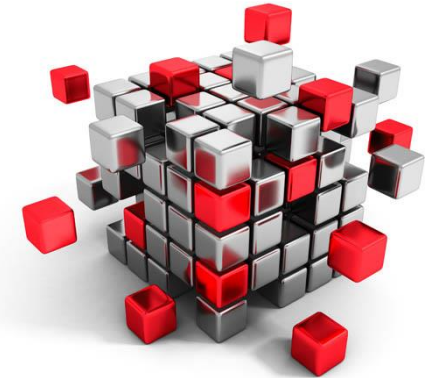
What is your question?



Simple question: use a simple model



Complex question: go to a more complex model



Conclusions

- Reduction of animal use in research



Ethical and economic benefits

- Proteins and molecules interaction at the surface of nanoparticles
- Perfusion and Flow pressure
- Control of the heterogeneity
- Characterization
- High throughput
- Automated techniques need to be adapted from 2D to 3D

